

# Modeling the radiobiological effects of gold nanoparticles in proton therapy of glioblastomas

#### MOTIVATION

The combination of high-Z nanoparticles (NP) and external radiotherapy leads to an increased radiation effect in tumoral cells without an increase of the patient dose (Figure 1).

However, it is not yet clear how the sequence of physical, chemical, and biological mechanisms contributes to the observed synergic effect.



Figure 1. Effect of NPs in tumoral cells [1].

# OBJECTIVE

Develop realistic simulations of the irradiation of monolayer (2D) and spheroid (3D) human glioblastomas multiforme (GBM) cell cultures, taking into consideration different concentrations cellular distributions of the gold and nanoparticles (GNPs).

# **TOol for PArticle Simulation**

The simulations will be implemented based on TOPAS [2] software more specifically the extension TOPAS-nBio [3] that includes models of the physical and chemical processes induced by radiation at the DNA scale.



Figure 2. a) TOPAS e b) TOPAS-nBio.

radiation:

reactive oxygen species (ROS).

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[1] S. Lacombe, et al., "Particle therapy and nanomedicine: state of art and research perspectives", *Cancer Nanotechnol*, 2017. [2] J. Perl, et al., "Topas: an innovative proton monte carlo platform for research and clinical applications," Med Phys, 2012. [3] J. Schuemann, et al., "Topas-nbio: An extension to the topas simulation toolkit for celular and sub-cellular radiobiology," Radiat

[4] H. Kim, et al., "Microdosimetric-Kinetic Model for Radio-enhancement of Gold Nanoparticles: comparison with LEM", Radiat

### **RADIOBIOLOGICAL MODELS**

The simulations outputs will be used to predict cell survival fractions (S), using standard mathematical models of the biological effects of radiation as Local Effect Model (LEM) and Microdosimetric Kinetic Model (MKM) [4]. Both models assume that the cell nucleus is the principal target, and it is divided into small independent domains. The application of this models to GNP radio-enhancement is done considering the probability of interaction (p) and the radial dose per ionization from single GNP  $(d_{GNP})$ .

#### LEM

 $\alpha d + \beta d^2$ ,

The number of lethal events  $(L_n)$  is a function of the absorbed dose in infinitesimally small volume in the nucleus (d):

 $(\alpha + 2\beta D_t)d - \beta D_t^2, d > D_t$ 

 $d \leq D_t$ 

 $S = \exp(-\langle L_n(d) \rangle)$ 

The number of lethal events  $(L_n)$  depends on the average absorbed dose in the nucleus  $(D_n)$  and on the dose-mean linear energy  $(\overline{y_D})$ :

$$\langle L_n(D_n) \rangle = \alpha^* D_n + \beta D_n$$

$$n = \frac{\sum_{i=1}^{n} D(i)}{\sum_{i=1}^{n} D(i)}$$

 $\nabla N$ 

# RESULTS

The results obtained in the simulations will be compared with the biological in vitro and in vivo experimental results, which will include evaluation of cell viability and survival. Moreover, the simulated ROS yields will be also compared with the experimentally determined values. So far, we did the definition of geometry on TOPAS, represented in figure 3c.

In the future, we will use this complex and realistic geometry to obtain more accurate results when compared to those obtained when using simple geometries.









$$\alpha^* = \alpha + \frac{\beta \overline{y_D}}{\rho \pi r_d^2}$$

 $D(1+p(d_{GNP})_i)$  $S = \exp(-\langle L_n(D_n) \rangle)$ 



