

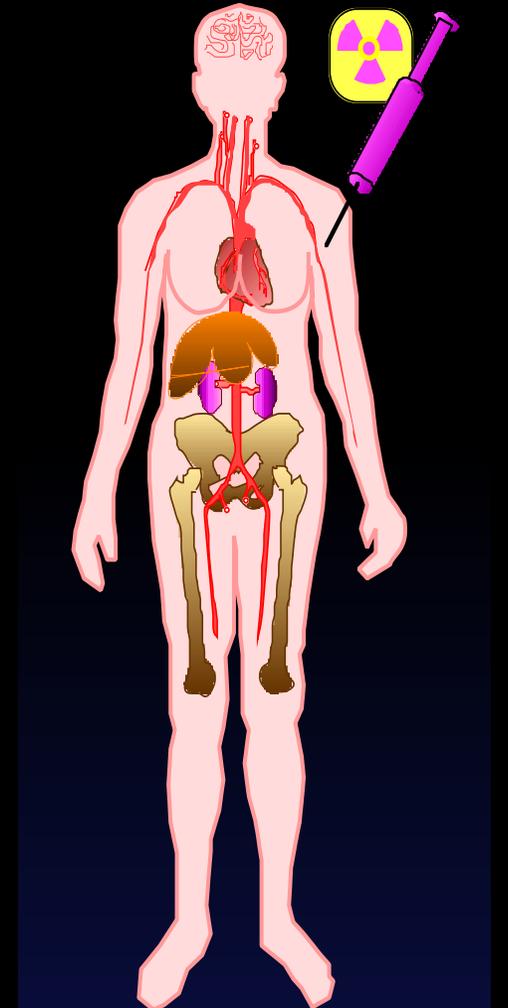


Activities at TagusLIP

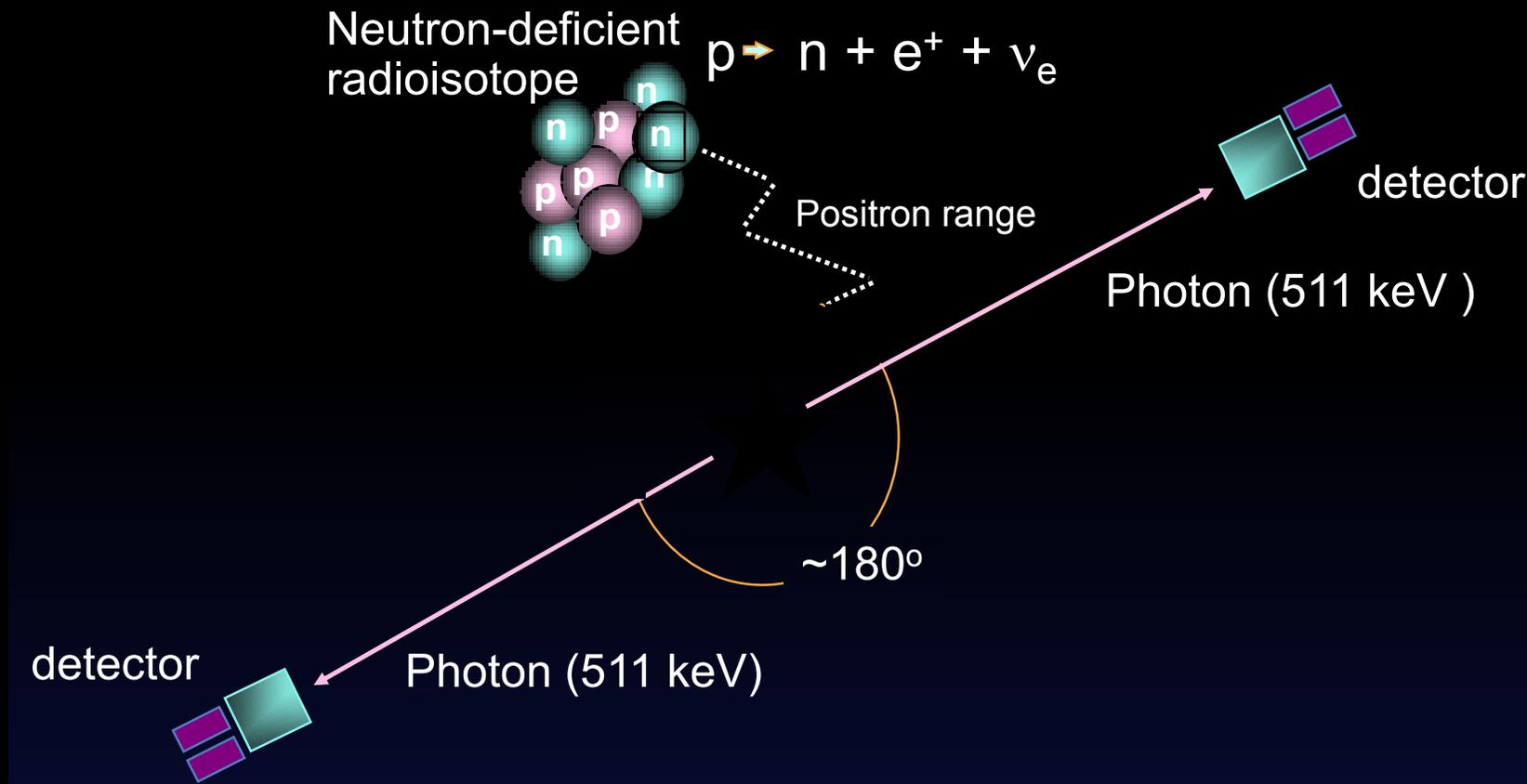
Tahereh Niknejad

PET: Positron Emission Tomography

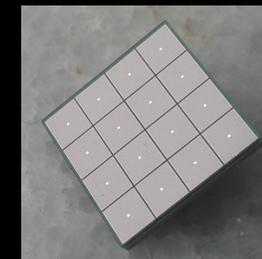
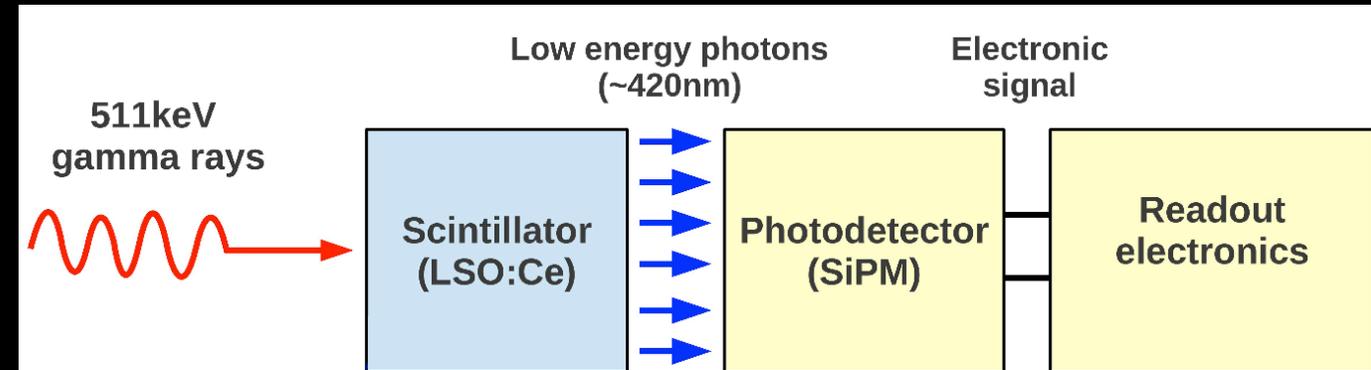
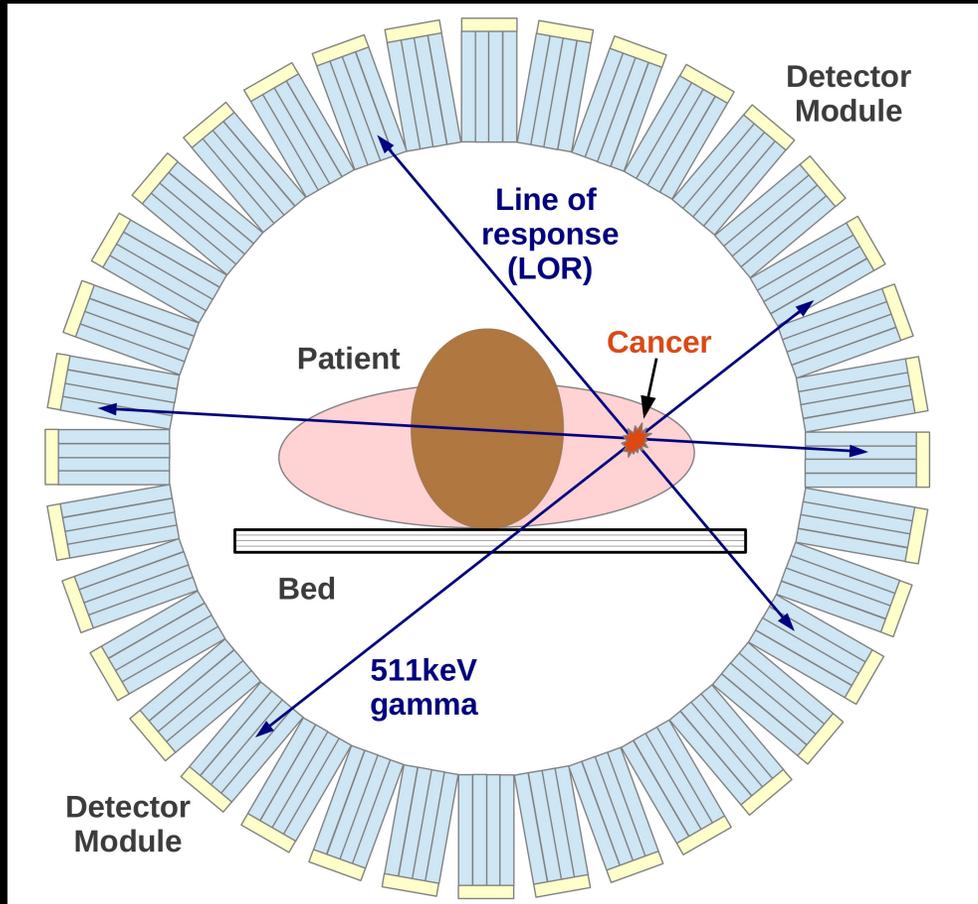
- How it works?
 - ✓ Drug (Glucose) is labeled with positron emitting radionuclide.
 - ✓ Glucose mainly concentrate in cancerous cells
 - ✓ Trace distribution of the drug in body
 - ✓ Radiation dose fairly small



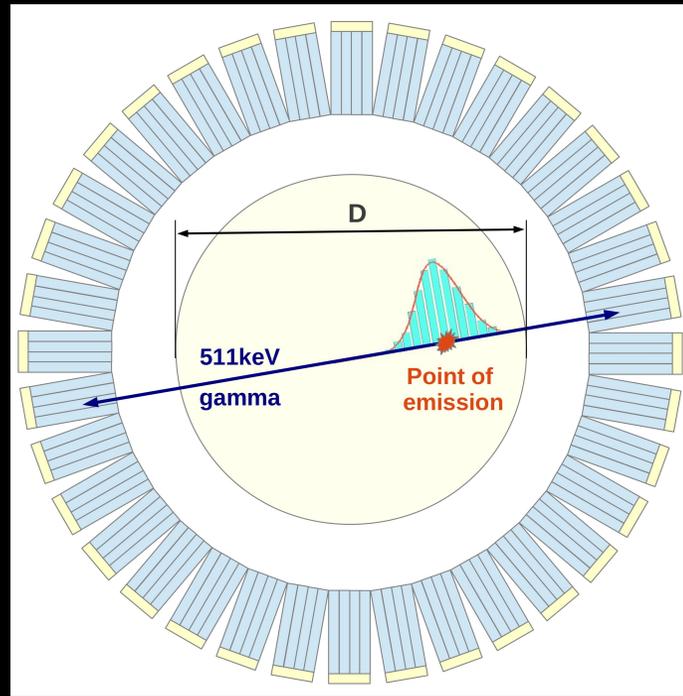
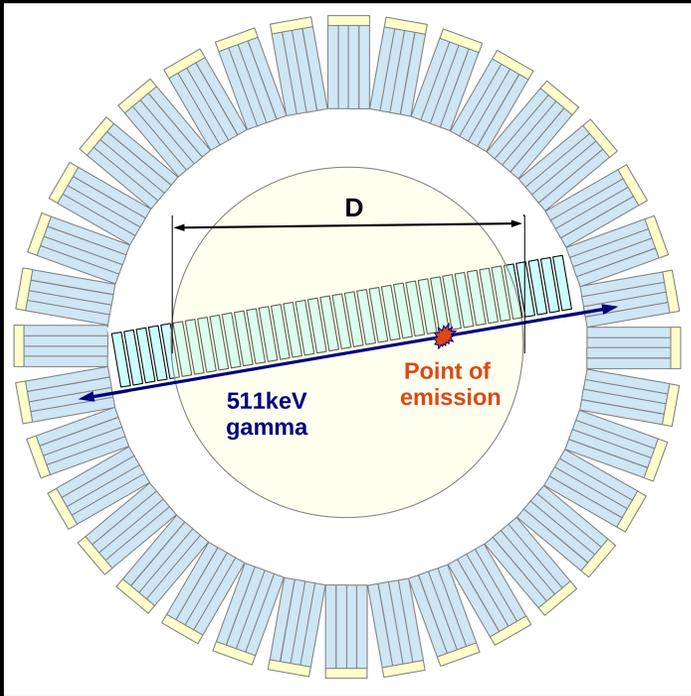
PET: detection



PET: Camera



PET: Time of Flight (TOF)

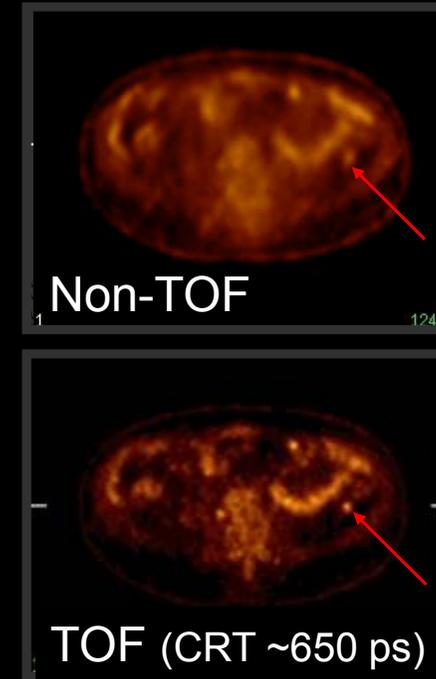


→ Without timing the positron emission could have happened anywhere along the line of response (LOR).

→ Time of flight can effectively confine the positron emission point.

→ Timing is determined by the full width at half maximum (FWHM) of the coincidence time resolution (CTR).

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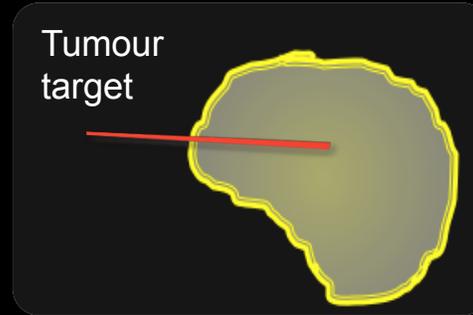
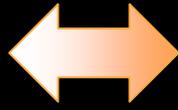
Colon cancer, left upper quadrant peritoneal node
13.4 mCi; 2 hr post-injection

$$G = \frac{SNR_{TOF}}{SNR_{nonTOF}} = \sqrt{\frac{2 * D}{c * CTR}}$$

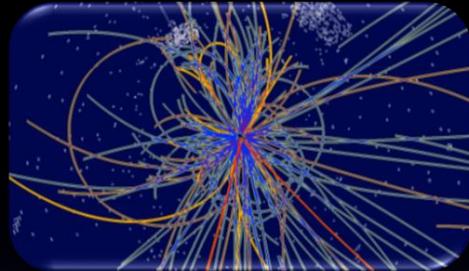
CERN Technology transfer



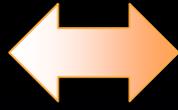
Accelerate particle beams



Hadron therapy



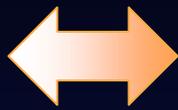
Detect particles



Medical imaging

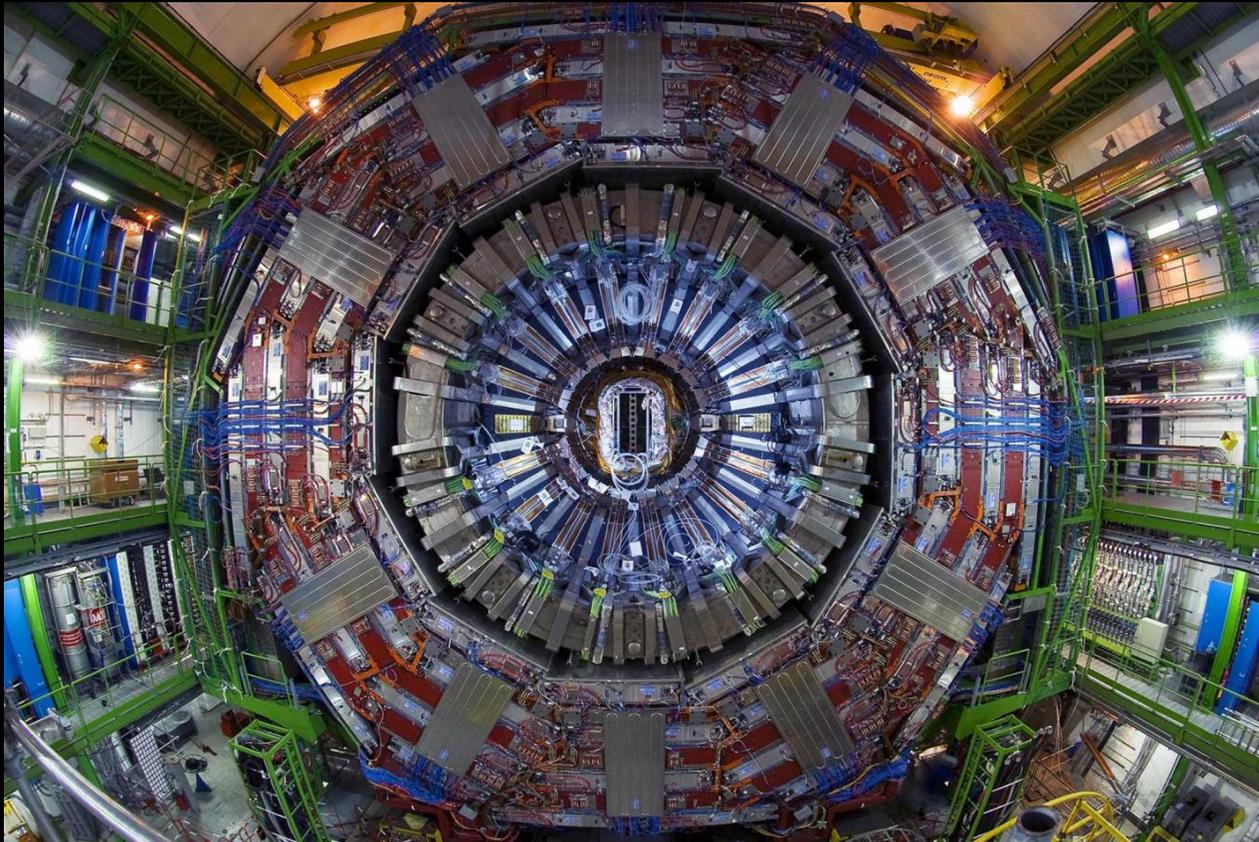


Large scale Computing (Grid)

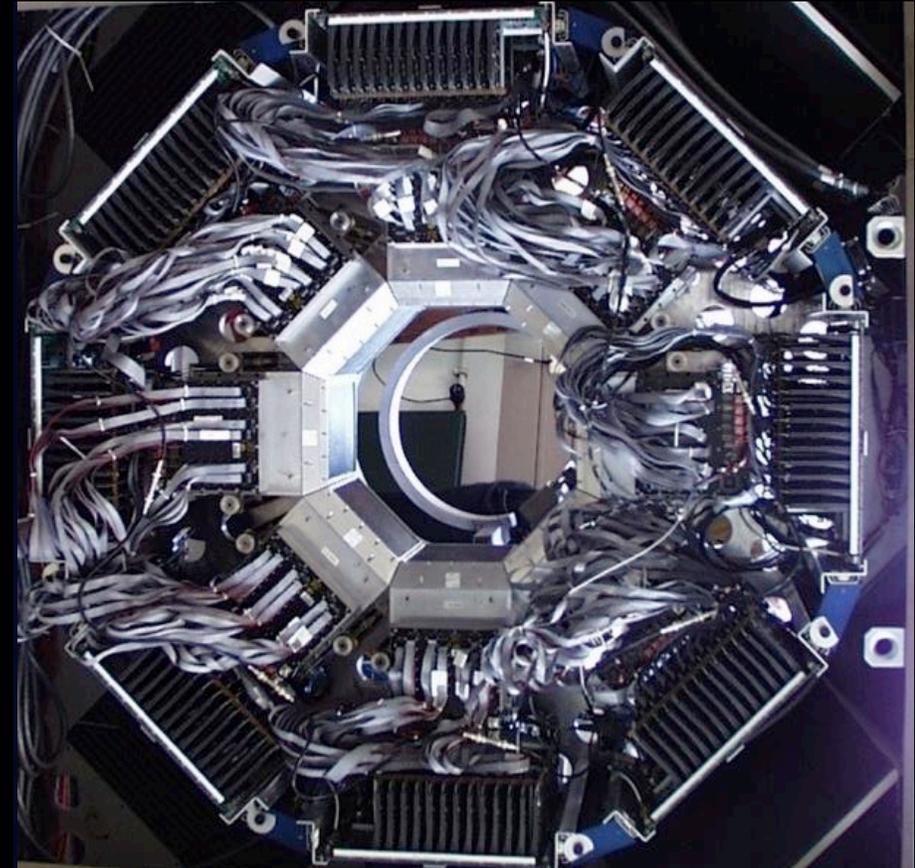


Grid computing for medical data management and analysis

PET vs photon detection in High Energy Physics (HEP): same challenges



CMS



PET camera

From HEP to PET

Requirements for HEP crystal calorimeters

❖ Crystals

- High density ($>6\text{gr/cm}^3$)
- Fast emission ($<100\text{ ns}$, visible spectrum)
- Moderate to high light yield
- High radiation resistance

❖ Photodetectors

- Compact
- High quantum efficiency
- High stability

❖ Readout electronics

- Fast shaping
- Low noise

❖ Software

- Handling of high quality data

❖ General design

- Compact integration of a large number of channels ($>>10'000$)

Requirements for PET scanners

❖ Crystals

- High density ($>7\text{gr/cm}^3$)
- Fast emission ($<100\text{ ns}$, visible spectrum)
- Moderate to high light yield
- High radiation resistance

❖ Photodetectors

- Compact
- High quantum efficiency
- High stability

❖ Readout electronics

- Fast shaping
- Low noise

❖ Software

- Handling of high quality data

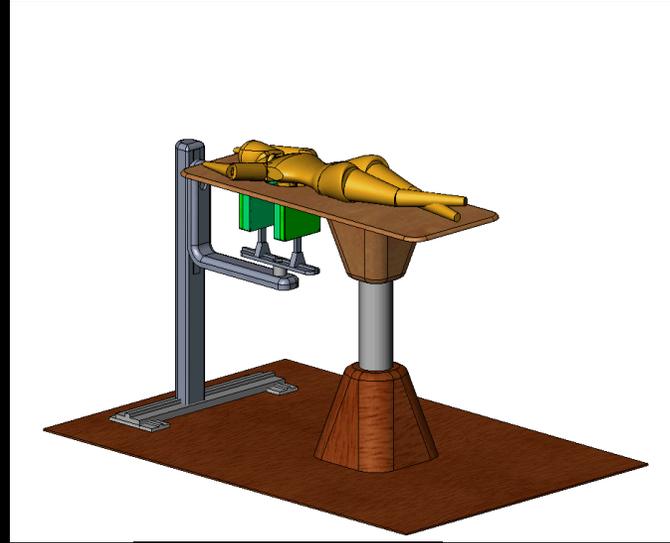
❖ General design

- Compact integration of a large number of channels ($>>10'000$)

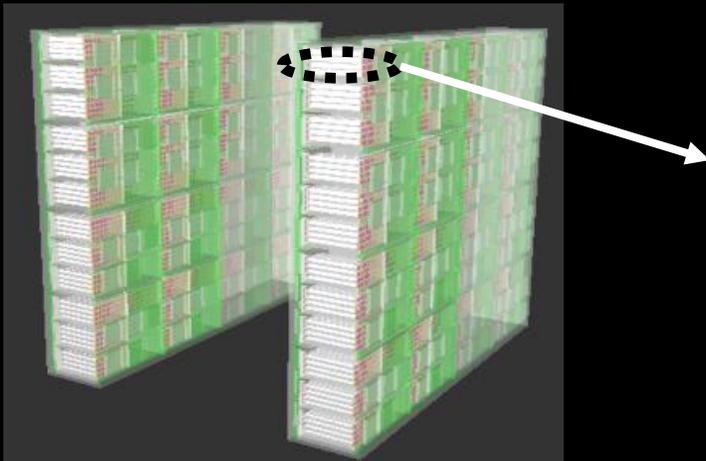
Technology transfer

- Development and validation of medical imaging technologies (readout electronics and detector modules)
- Design, produce and test/validate prototype imaging equipment.
- Design of new ASICs and front-end boards for the CMS upgrade

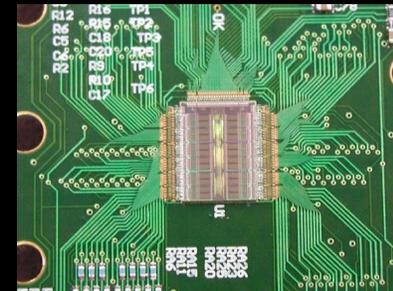
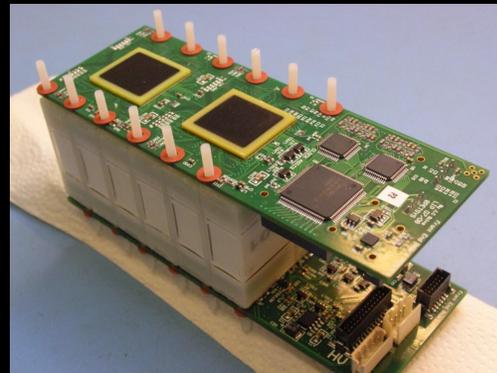
ClearPEM (2010)



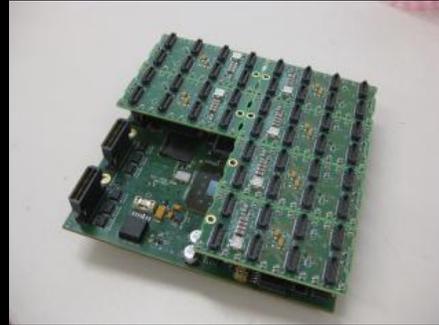
- PET detector dedicated to breast cancer screening
- Extremely sensitive to small tumor masses
- Spatial resolution 1-2 mm
- High counting sensitivity



LYSO+APD



EndoTOFPET (2013)



LYSO+SiPM

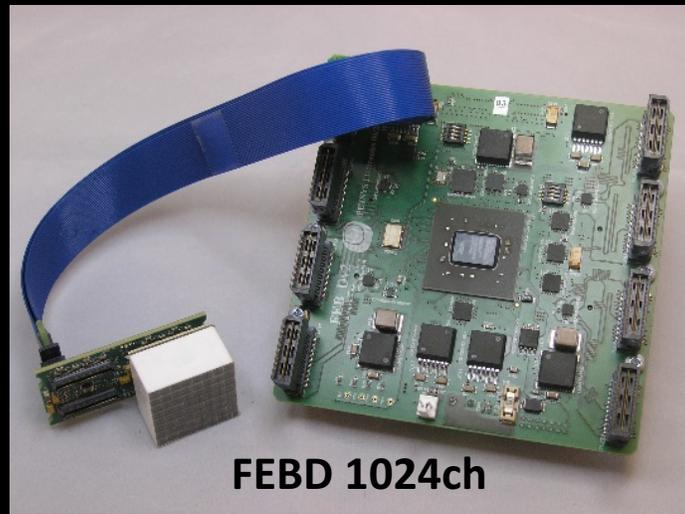
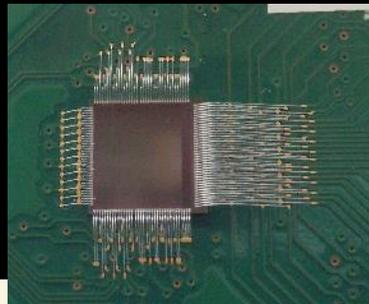
- PET detector dedicated to pancreatic cancer screening
- Spatial resolution ~ 1 mm
- Timing resolution ~ 350 ps FWHM
- High counting sensitivity



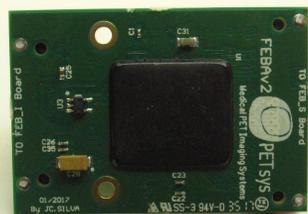
TOF ASIC for PET and HEP

- Highly integrated readout electronics scalable to several hundreds of channels

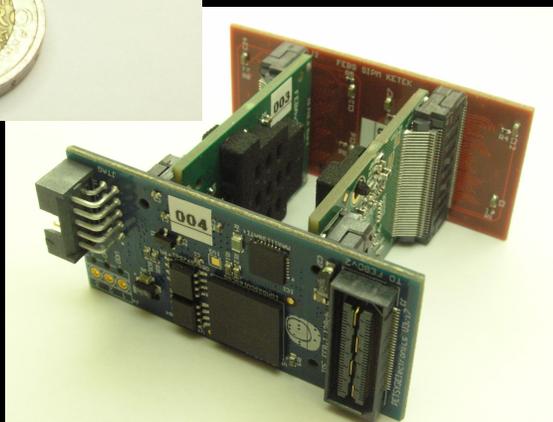
64chASIC
(5x5mm)



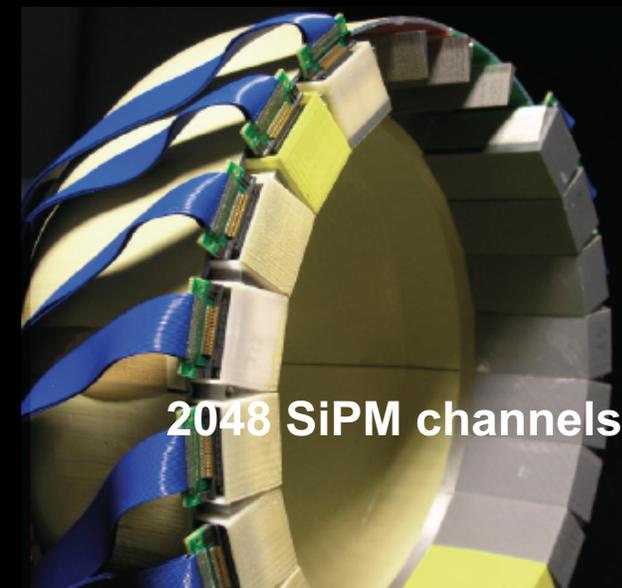
FEBD 1024ch



Front end
module
128ch



BIAS and DAQ mezz
Farshad Niknejad (f.niknejad@lip.pt)



2048 SiPM channels

ASIC for TOF applications



	PET	HEP
TOFPET1	✓	✓
TOFPET2	✓	✓
TOFEE (CT-PPS)		✓
TIGER (BES III)		✓
TOFHiR (CMS: BTL)		✓

Thank you for you attention

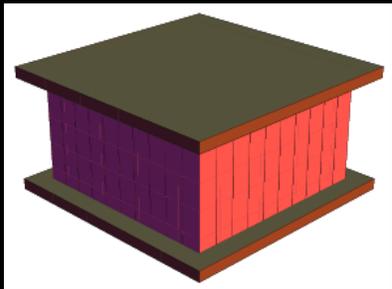
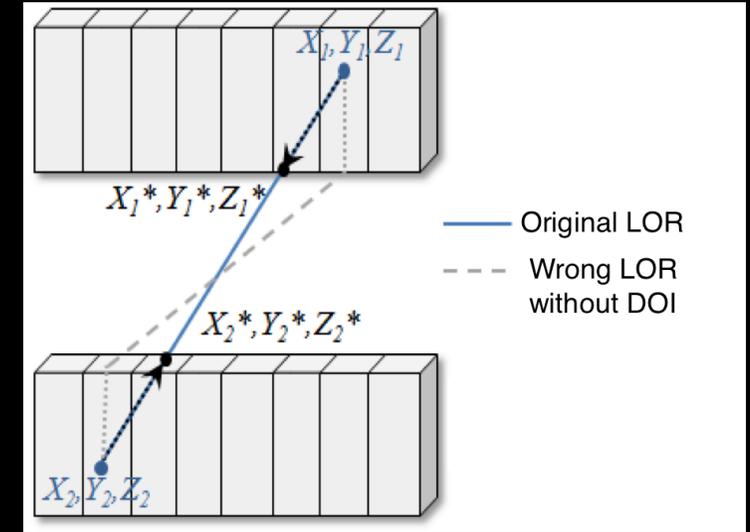
Any question?

Backup slides

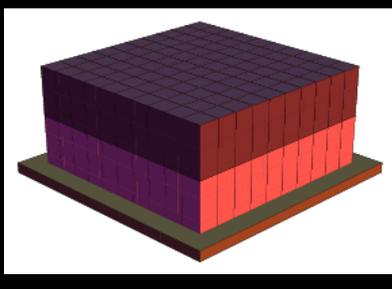
Depth of interaction

→ Without DOI wrong LORs are assigned to the events

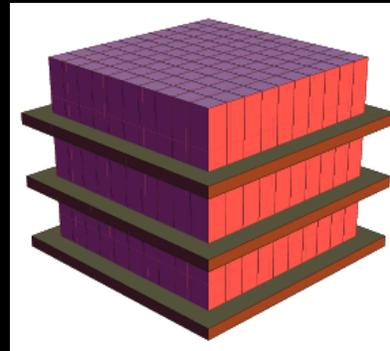
→ Depth-of-interaction determination



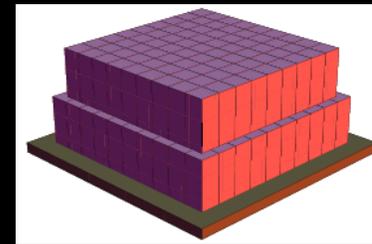
Dual Ended Readout



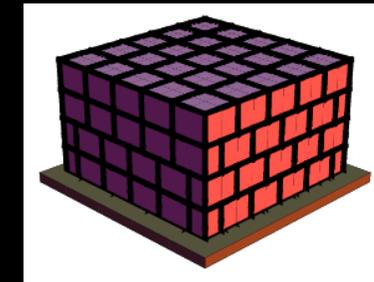
Phoswich



Stacked Detector



dual Layer with Offset



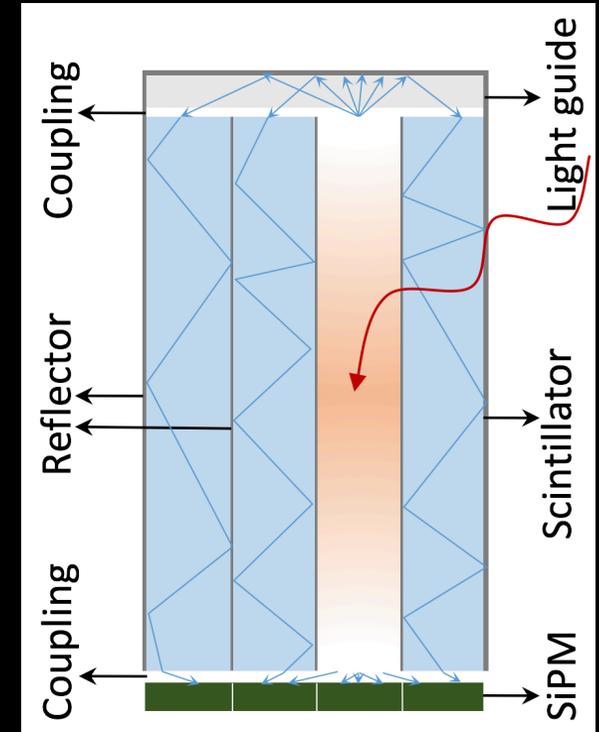
Multiple layer with offset

PhD Thesis Defense

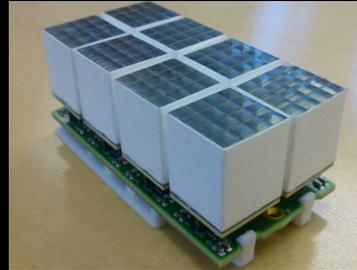
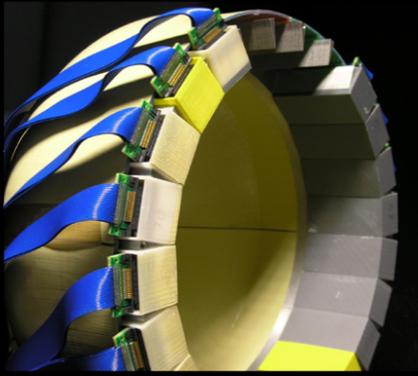
→ Drawbacks: Complexity and costs

New method for DOI

- Only one side readout
- A light guide is placed on the top of the module (same dimension of the matrix).
- The reflector recirculates the light and redirects it to the MPPC array.
- Optical treatment of the lateral surfaces of the crystals: depolished



Design and fabrication of TOF-PET demonstrator



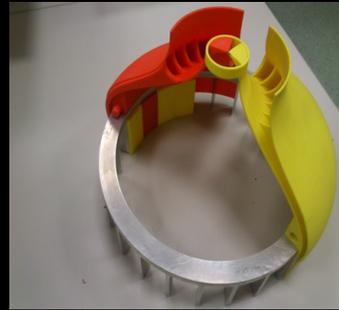
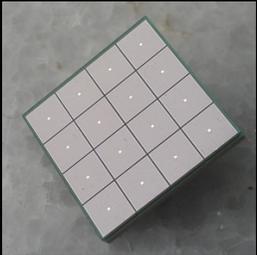
→ 16 Detector Modules (8 on each side)

- Ring diameter: 235 mm

→ Each module 2x4 array of crystal

→ LYSO crystal block

- Array of 4x4 LYSO
- Pixel size 3x3x15 mm³
- Separated by Vikuiti foils
- Pitch 3.2 mm



→ SiPM from Hamamatsu

- Active area 3x3 mm²
- Array of 4x4

→ Using cooling system: ~19°C

