

Particle Physics Techniques Applied to Health

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LIP training internship

LIP – July 6th, 2023

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Outline

I – Advances in Nuclear Medicine

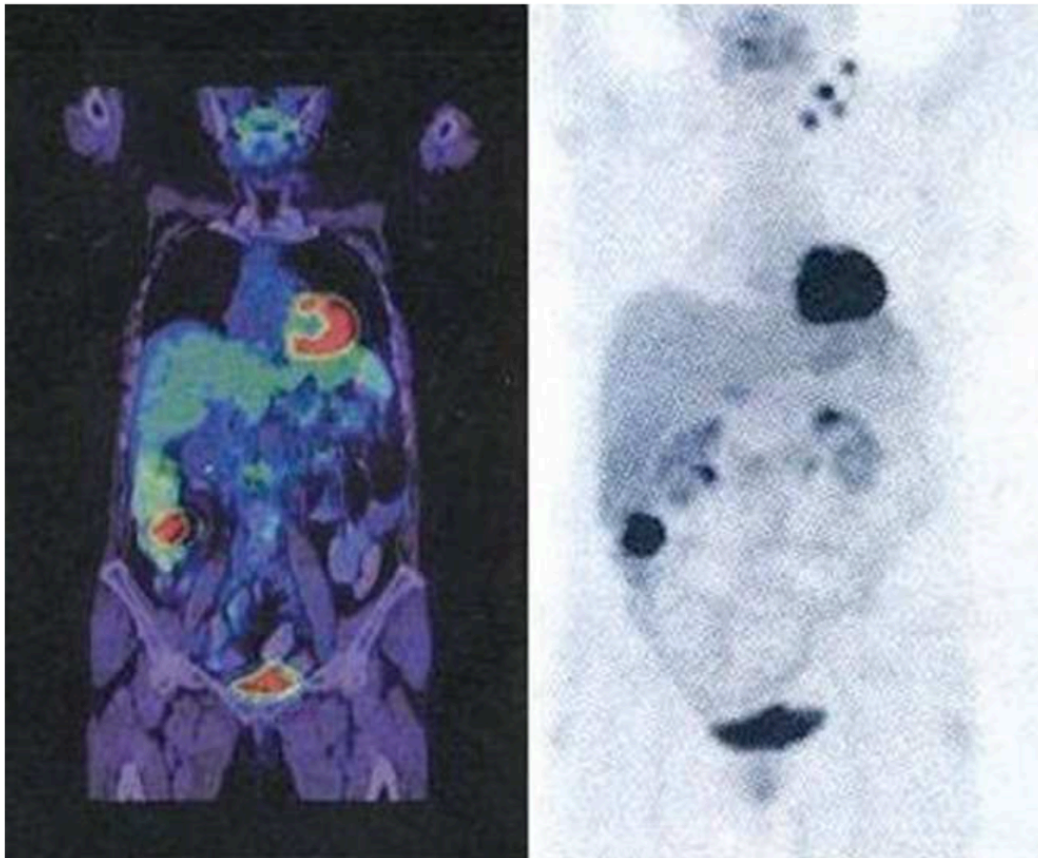
1. RPC-based TOF-PET
2. Development of New Gamma Cameras

II – Advances in Imaging in Proton Radiotherapy

1. Motivation
2. Rationale for in-vivo imaging in proton radiotherapy (RT)
3. The multi-slat concept for prompt-gamma imaging in proton RT
4. In-beam time-of-flight PET for proton RT

Rationale is based on state-of-the-art of PET (positron emission tomography):

- Technique experiences growing utilization in nuclear medicine, e.g. for diagnostic/screening/staging of oncologic, neurologic, and cardiac disease.

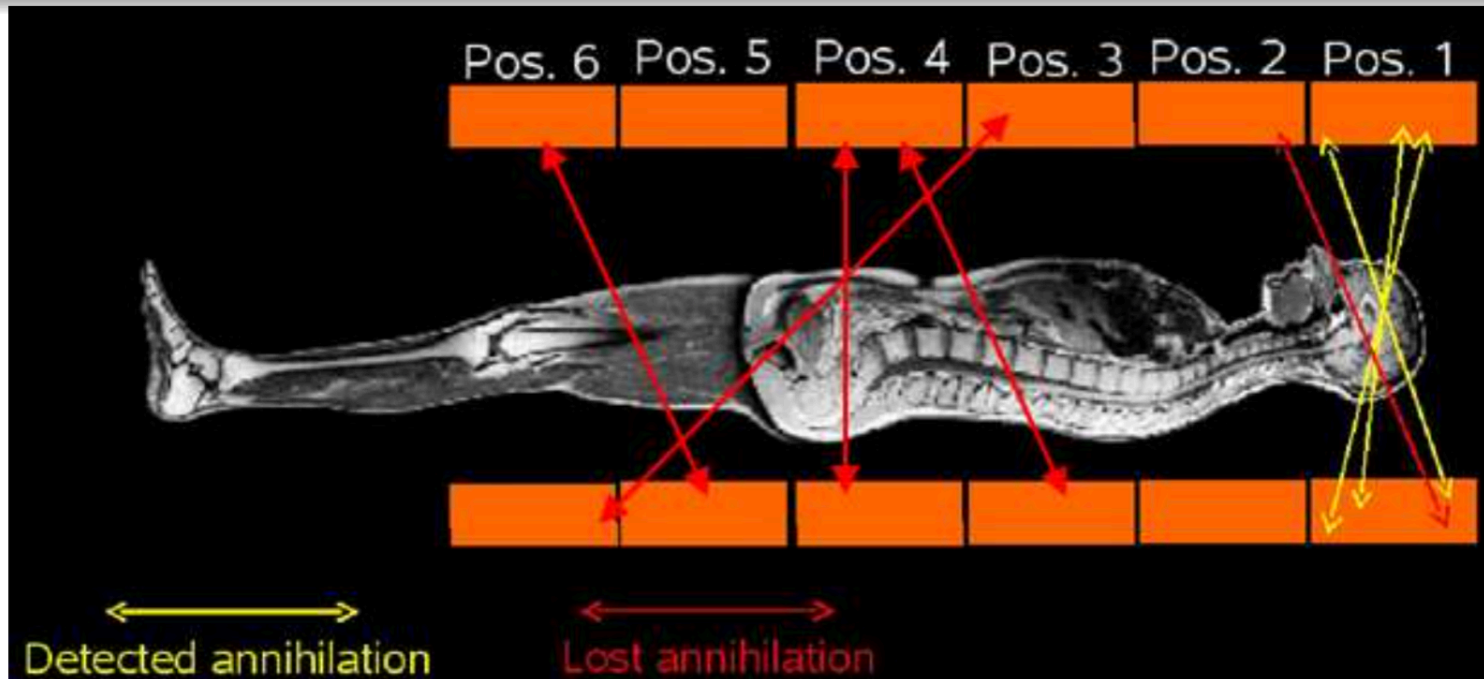


- E.g. **Palmisano et al. Saudi J Gastroenterol 2011**
- F, 64 a., symptoms: palpable supracavicular, ganglionic adenopathies, asthenia, anorexia.
- PET-based diagnostic: adenocarcinoma of the ascendent colon.

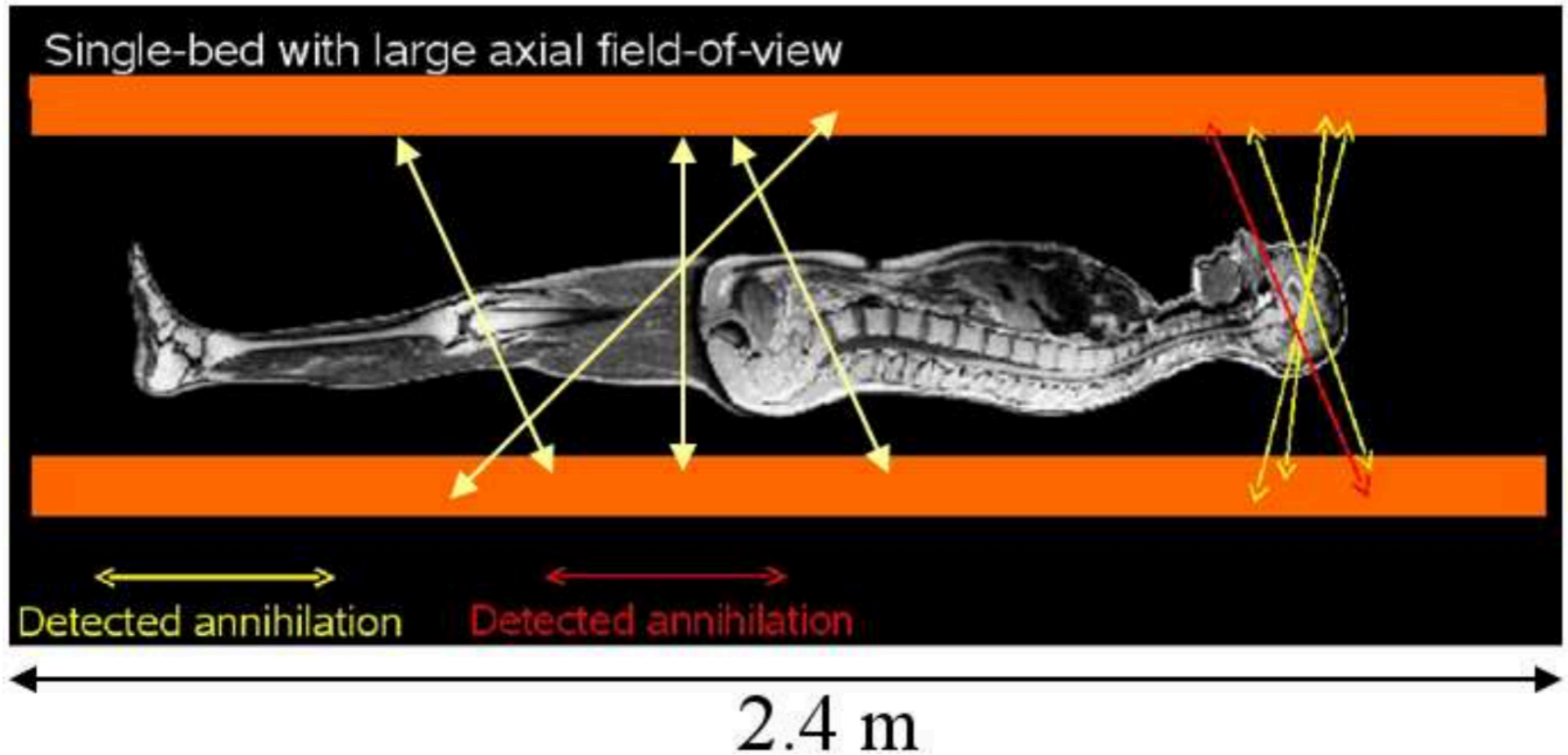
I - 1. RPC-based TOF-PET

Rationale:

- PET technology is extremely costly (millions of €); patient examinations are equally costly (ca. 4000 €), lengthy in time, morphologically imprecise, often inconclusive when imaging small lesions (detectability, sensitivity, and specificity); and the patient bears a non-negligible amount of radiation dose.



I - 1. RPC-based TOF-PET



I - 1. RPC-based TOF-PET



Electrónica de aquisição cedida pelo grupo de DAQ de HADES (GSI, Alemanha)

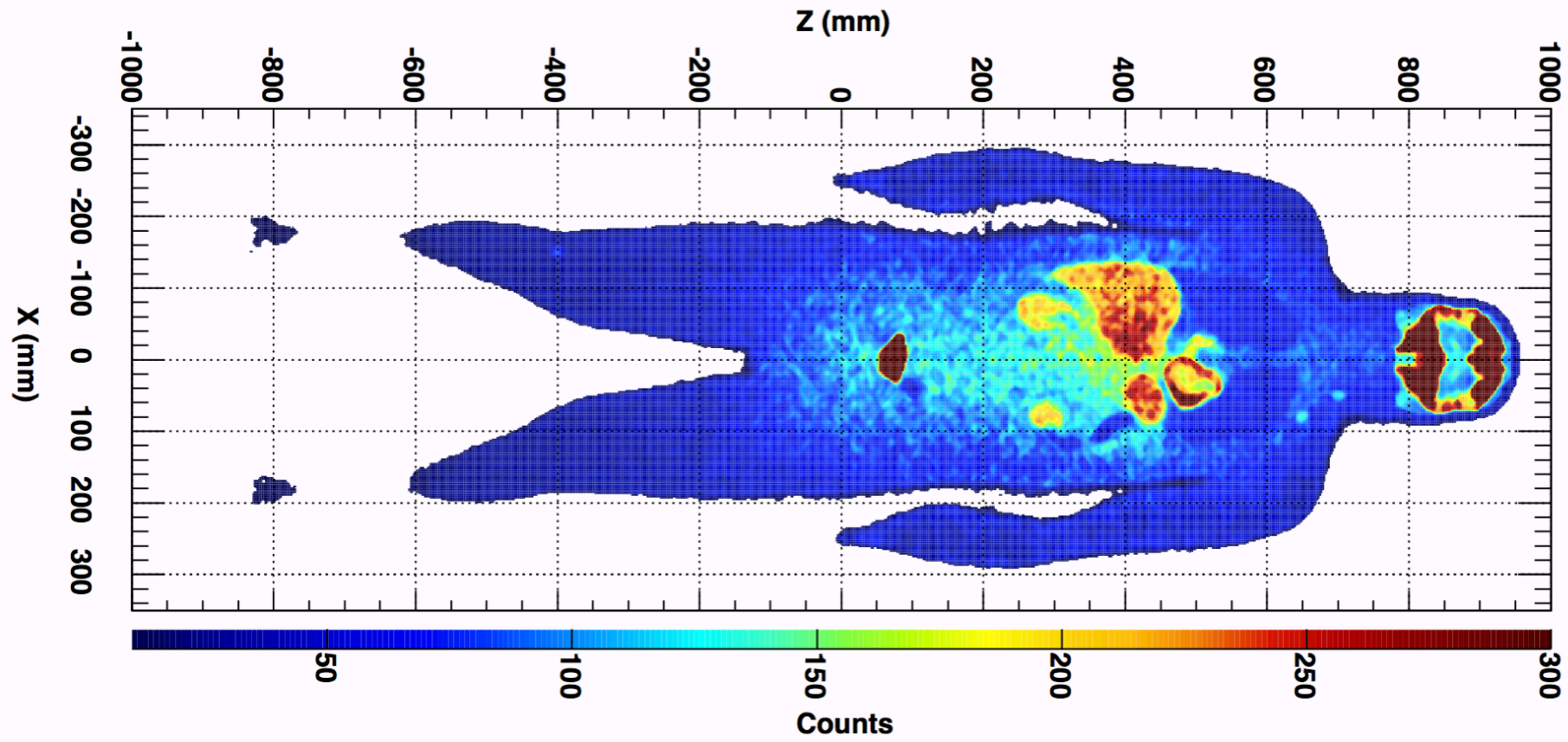
Electrónica de coincidências

Detectores RPC-PET (uma cabeça)

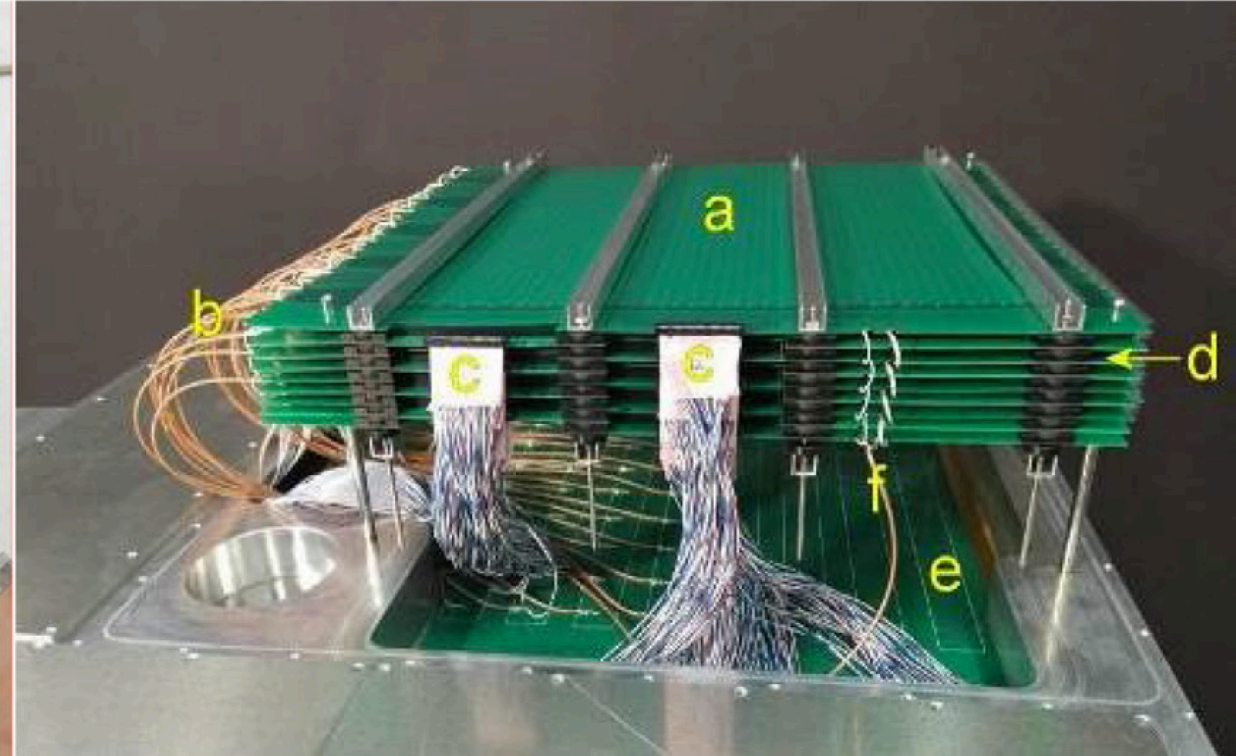
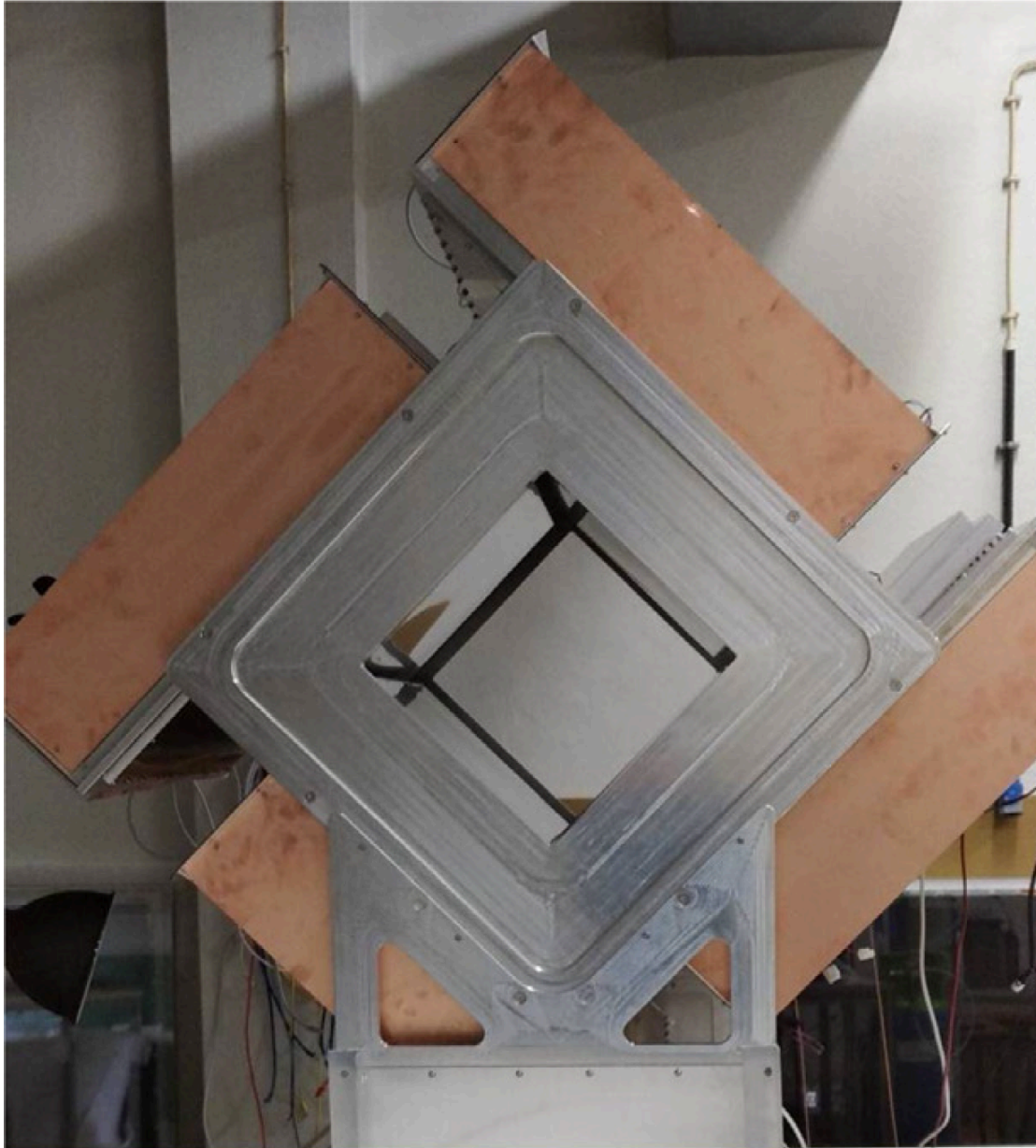
I - 1. RPC-based TOF-PET

Implementation (software):

- R&D in simulation and reconstruction

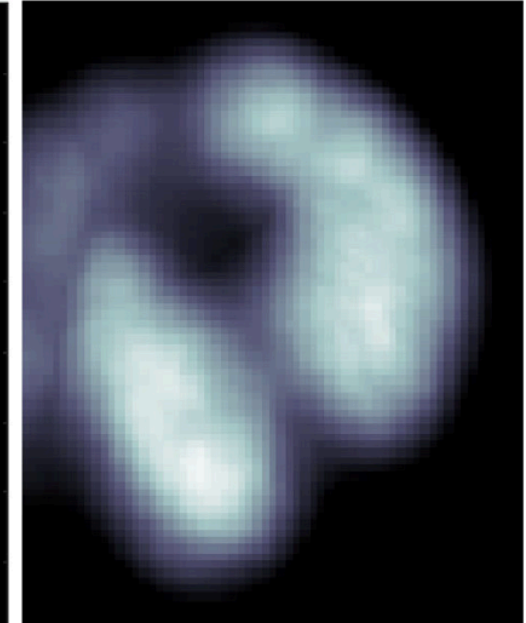
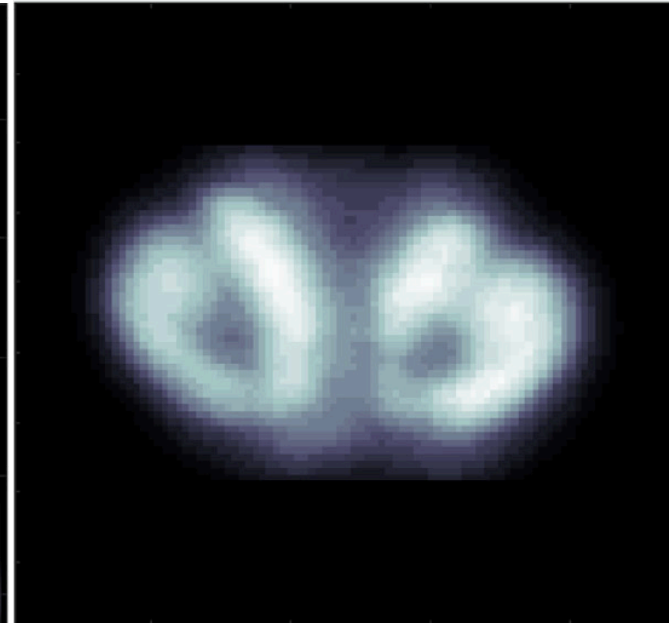
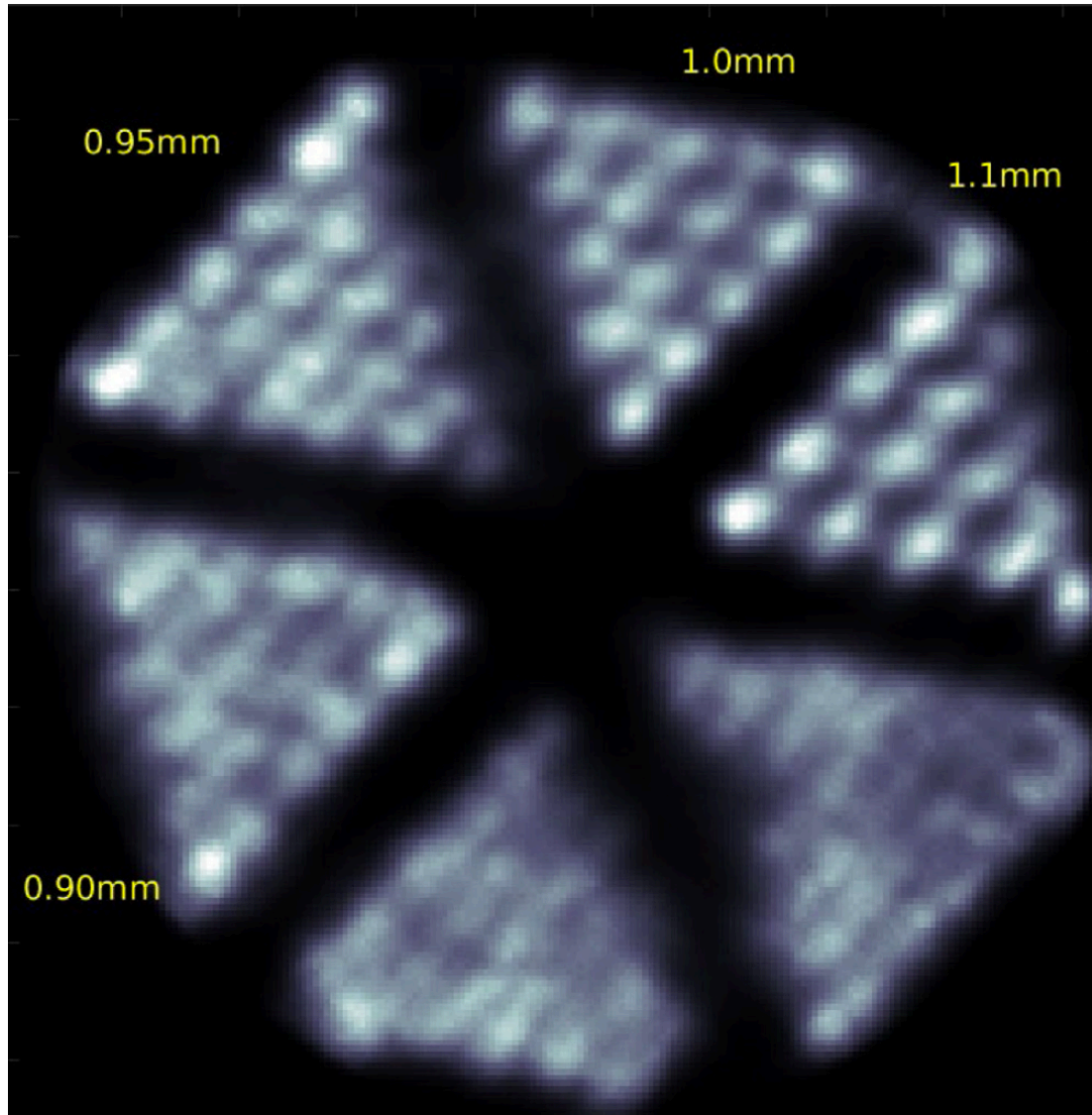


I - 1. Brain HiRez RPC-PET



(Fonte at al NIMA 2023)

I - 1. Brain HiRez RPC-PET



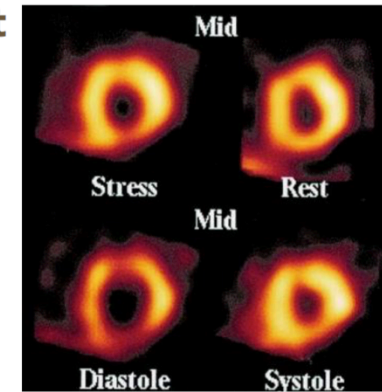
(Fonte at al NIMA 2023)

I - 2. Development of New Gamma Cameras

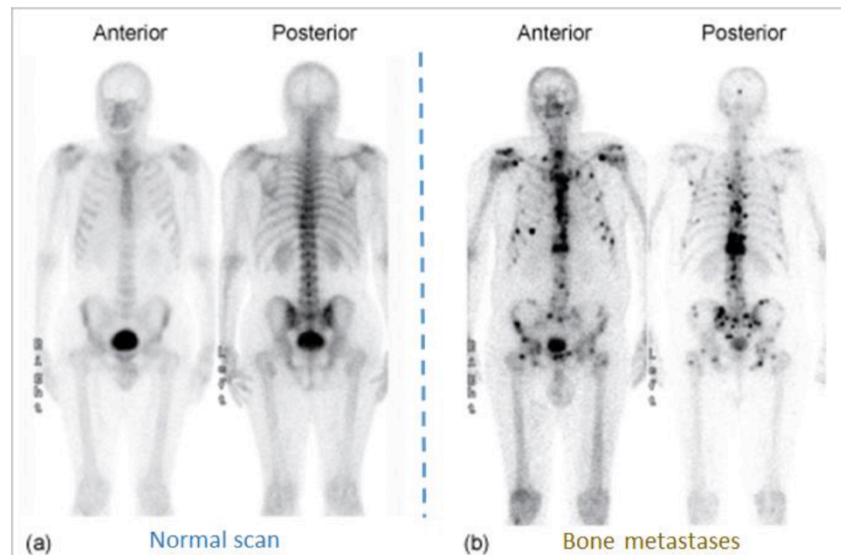
- Collaboration between Laboratório de Instrumentação e Física Experimental de Partículas, **LIP** and the University Hospital of Coimbra – **Nuclear Medicine Department**
- Gamma cameras are used to perform **scintigraphy**: a medical imaging modality used to obtain functional images. E.g. cardiology, pneumology, oncology (staging of tumors, evaluate therapeutic response)



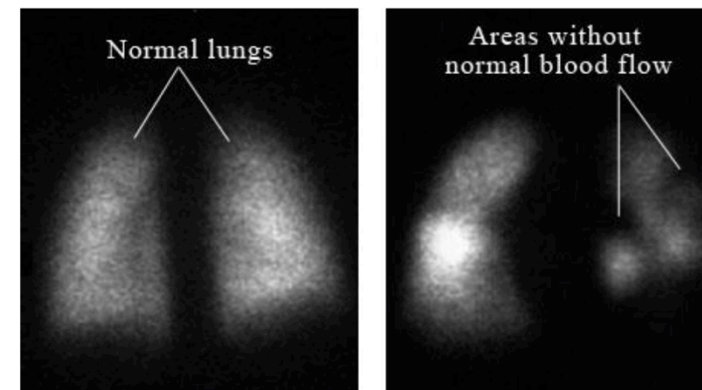
Heart
study



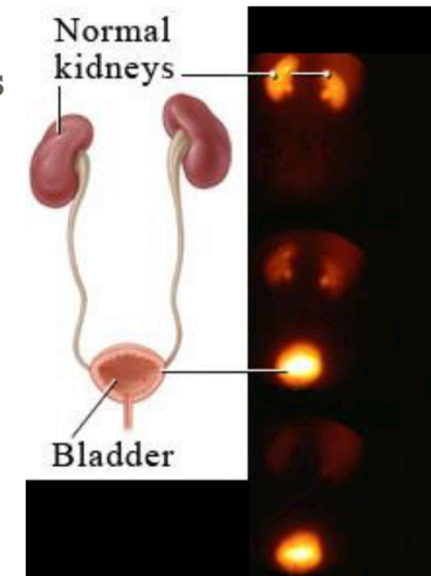
Bone scans



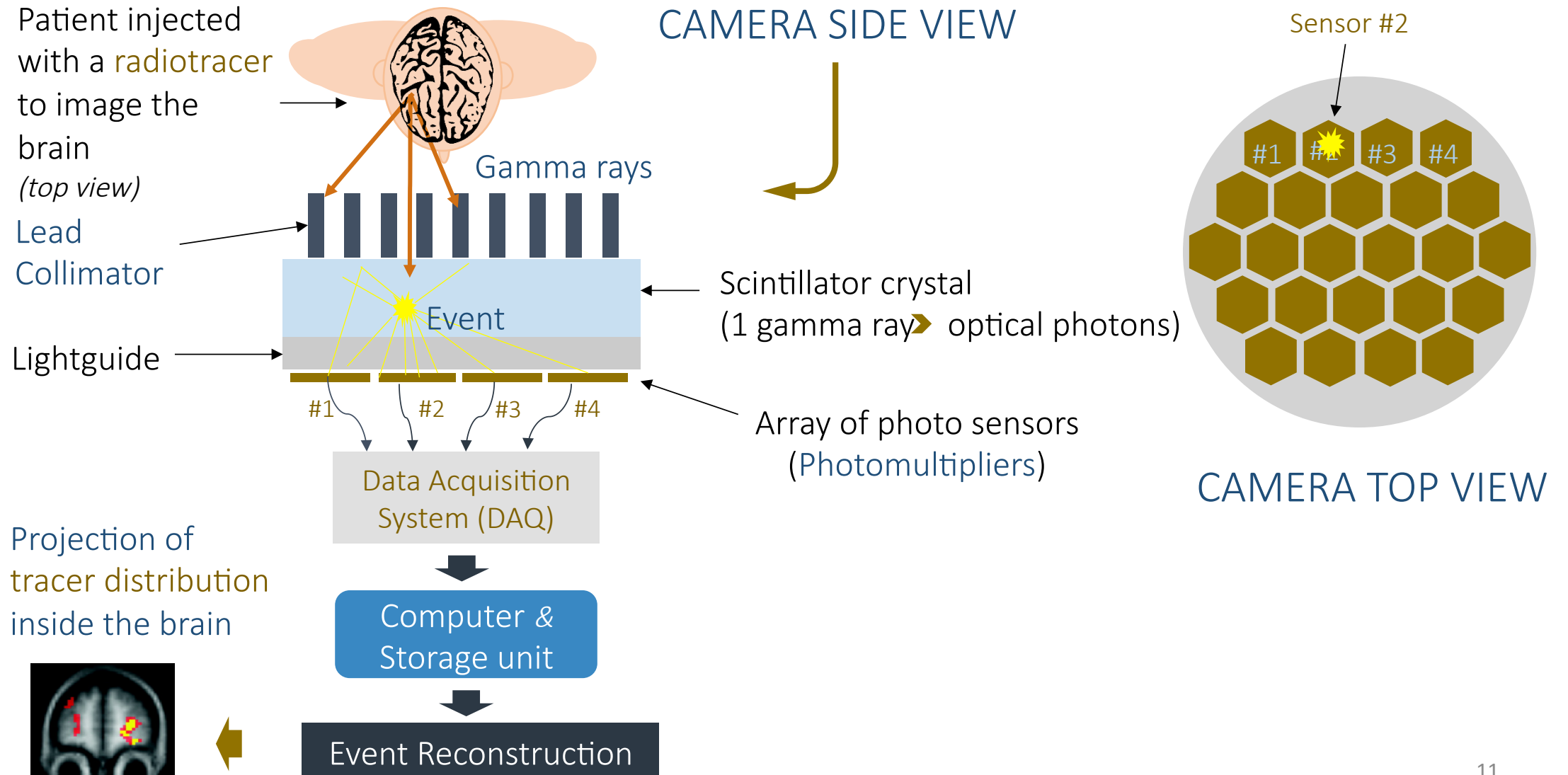
Lung
scintigraphy



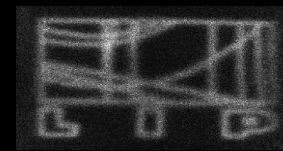
Kidneys
study



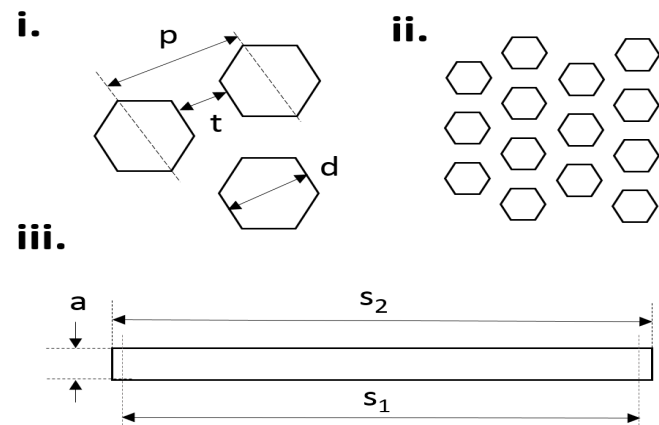
Gamma camera working principle



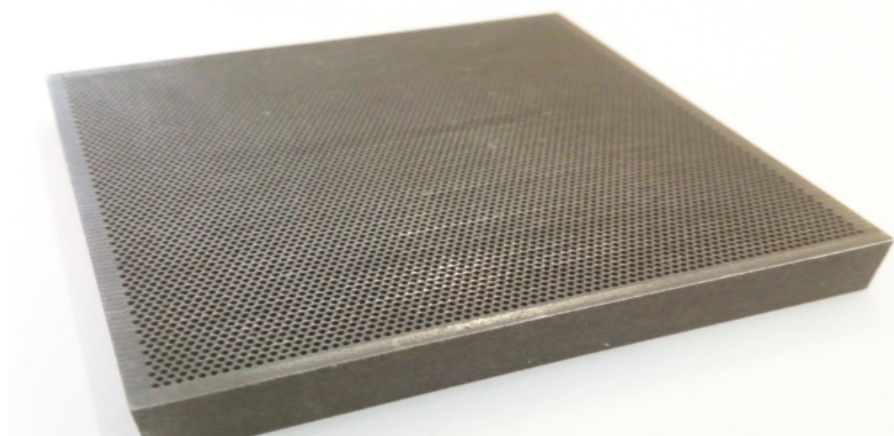
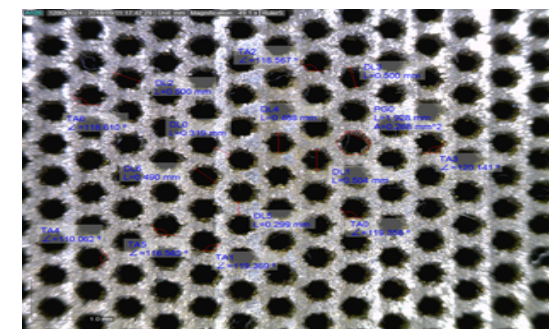
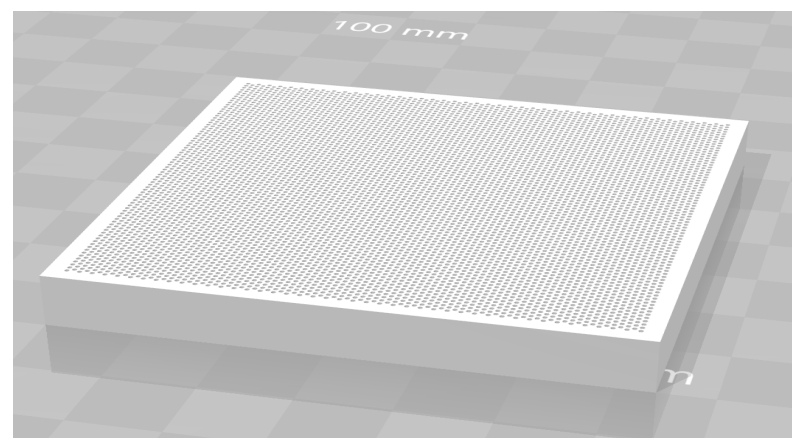
Collimators prototypes



Parallel-holes collimator (hexagones 0.5 mm "diameter)

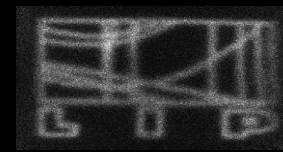


Made of tungsten using Selective laser melting



- **Specification** by João Marcos
- **Designed** by Eng. Rui Alves (LIP mechanical workshop)
- **Manufactured** by M&I Materials

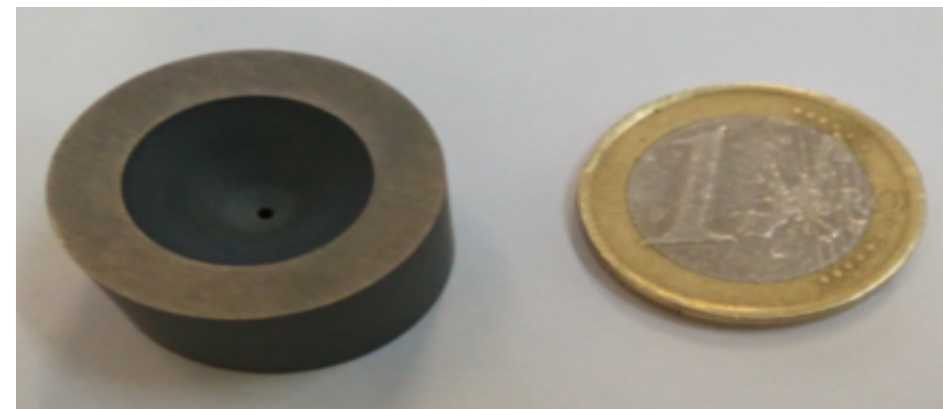
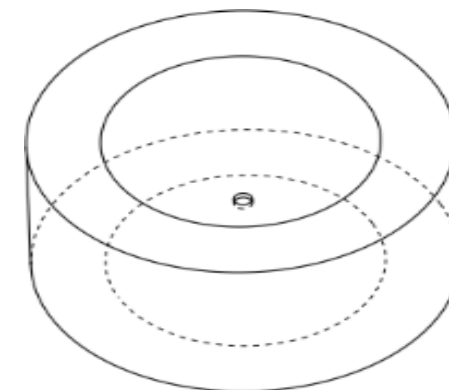
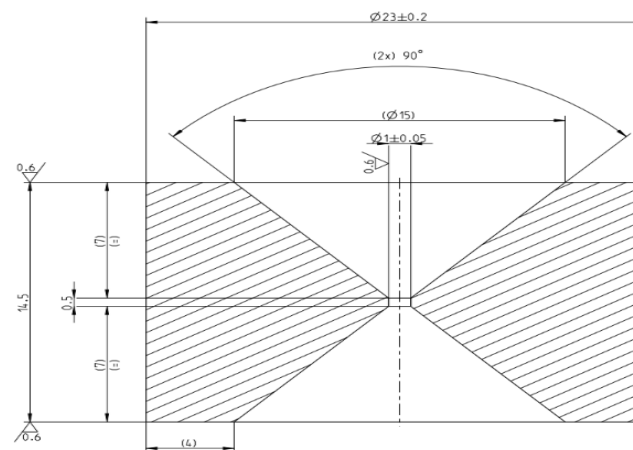
Collimators prototypes



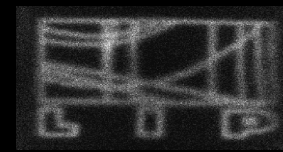
Pinhole collimator (1 mm hole, 0.5 mm channel edge height)

Made of Tungsten alloy (95.5% W, 4.5% Co)

- **Specification** by João Marcos
- **Designed** by DURIT (Albergaria-a-Velha)
- **Manufactured** by DURIT



Phantom imaging



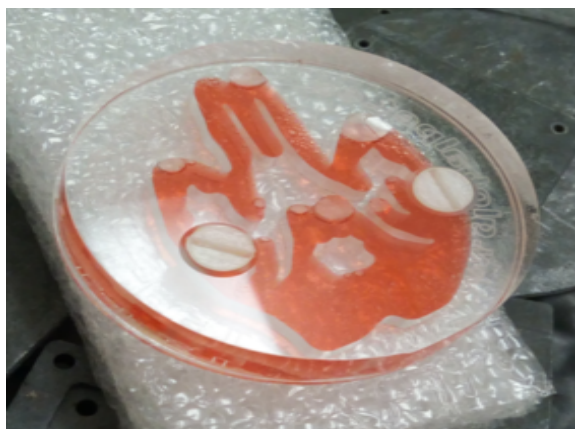
1 2



9 0

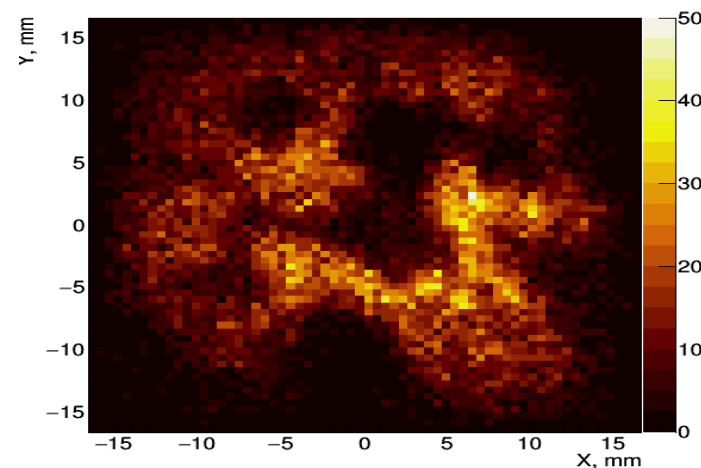
UNIVERSIDADE DE
COIMBRA

Brain slice phantom



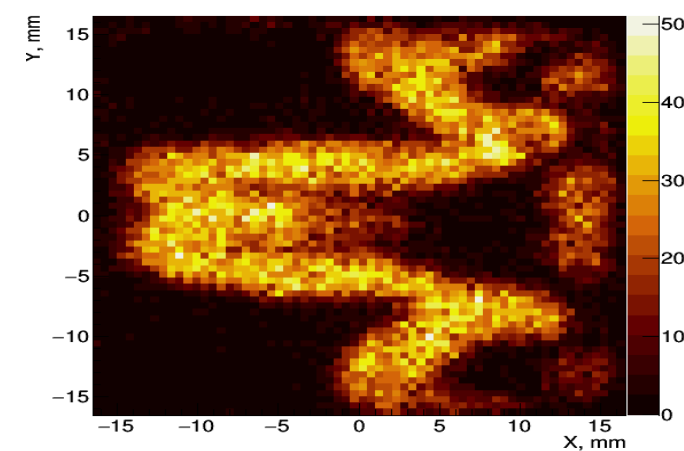
Pinhole collimator

Event density vs XY

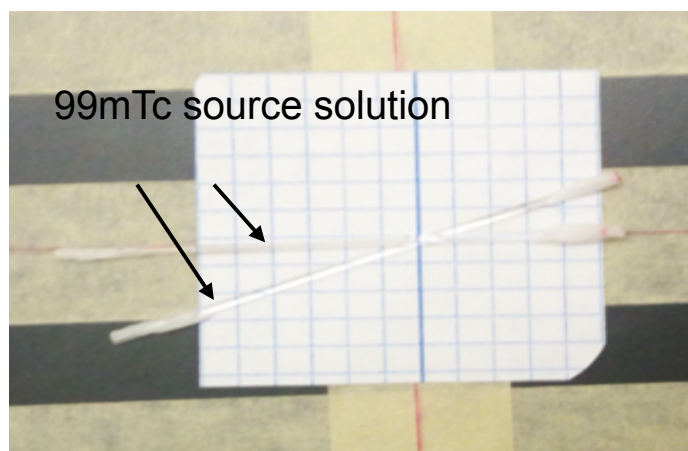


Parallel-hole collimator

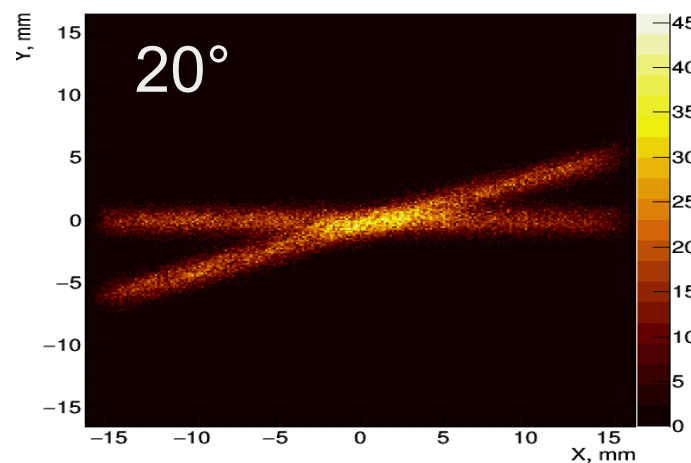
Event density vs XY



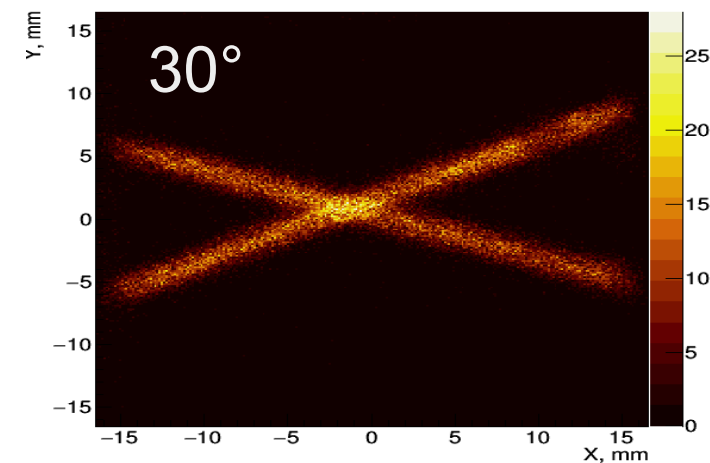
Crossed capillary tubes phantom



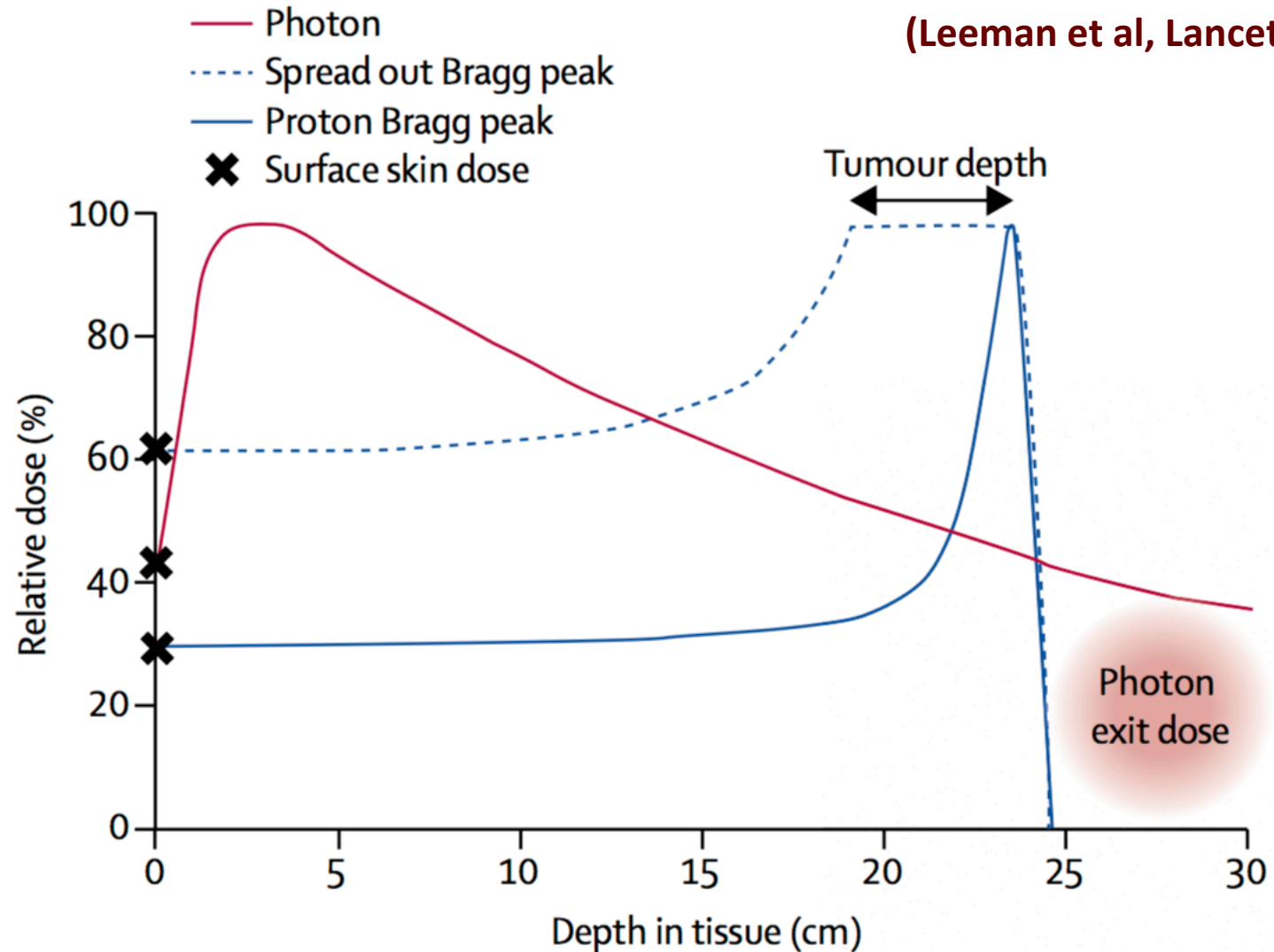
Event density vs XY



Event density vs XY



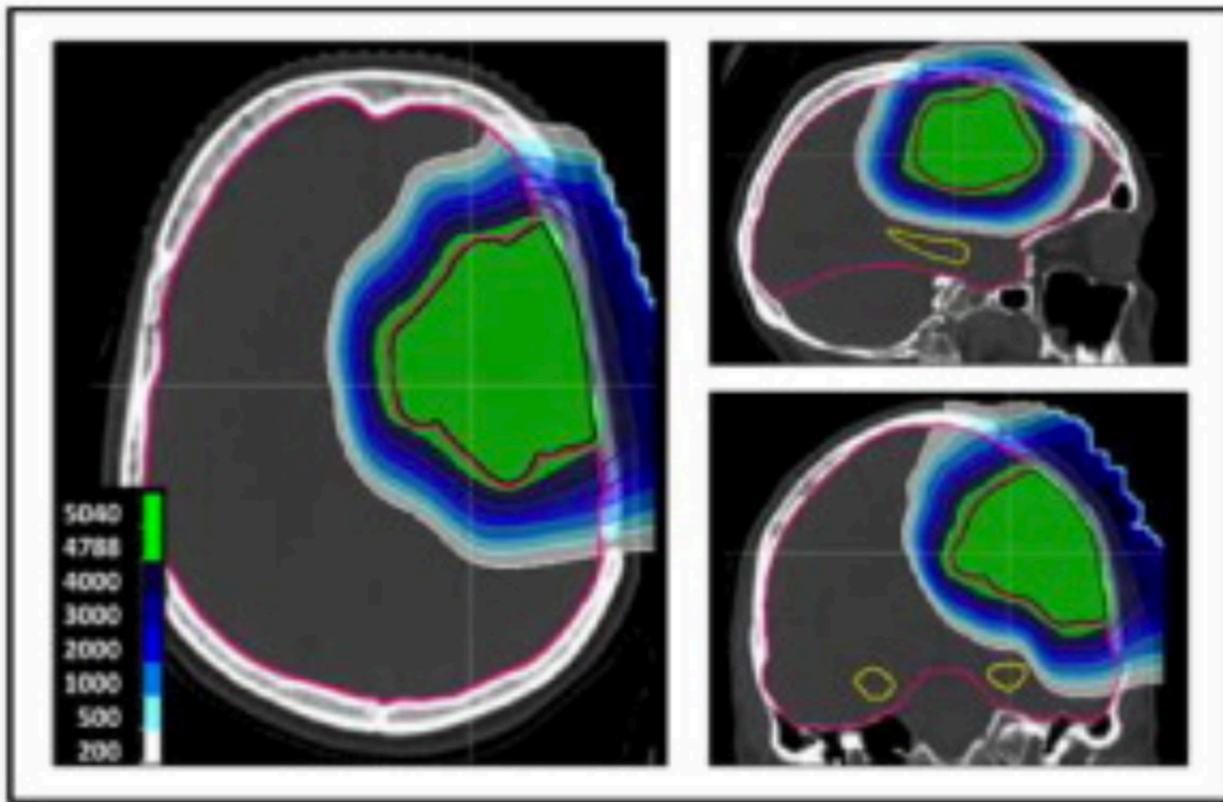
II - 1. Motivation: Proton therapy physical advantage over photons



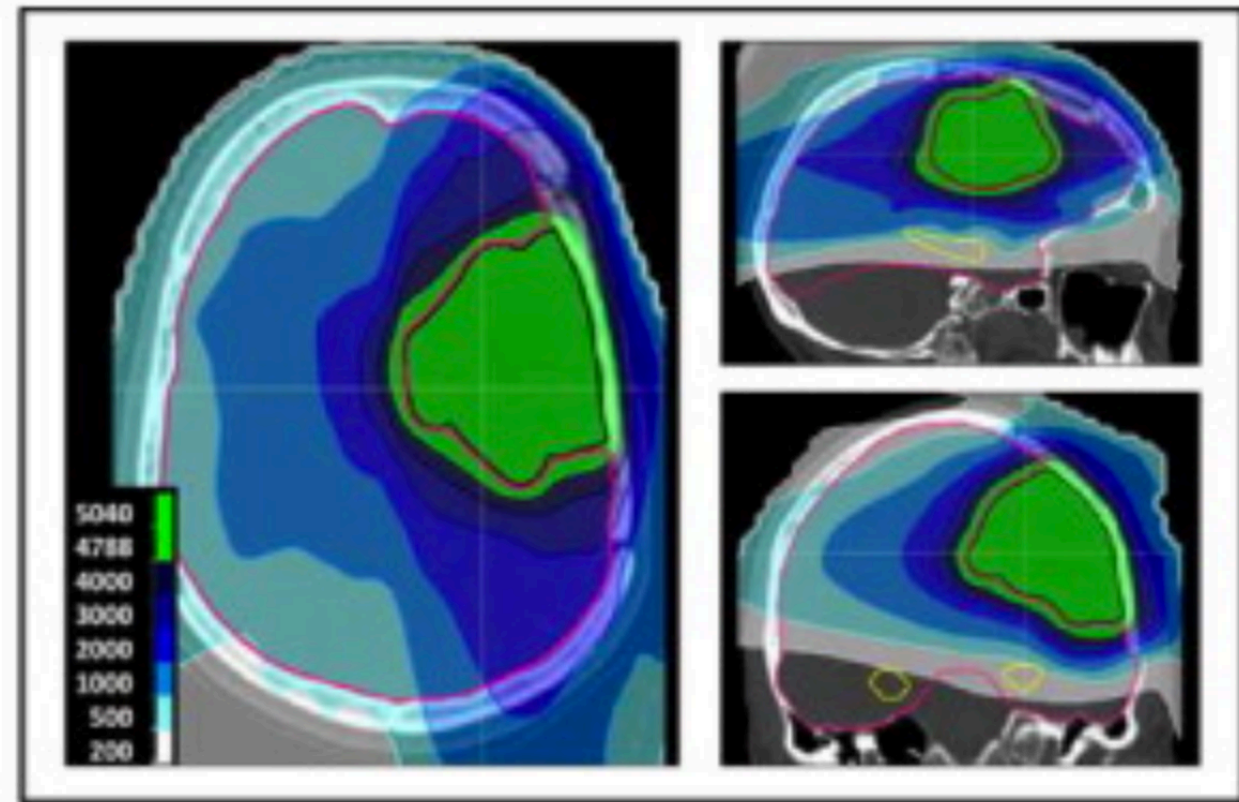
Some evidence of advantages of PT over state-of-the-art X-rays

Low-grade glioma, female, 38 y.o.: **dose reduction accepted as being clinically relevant**

Two-field intensity modulated PT



Volumetric intensity modulated arc therapy

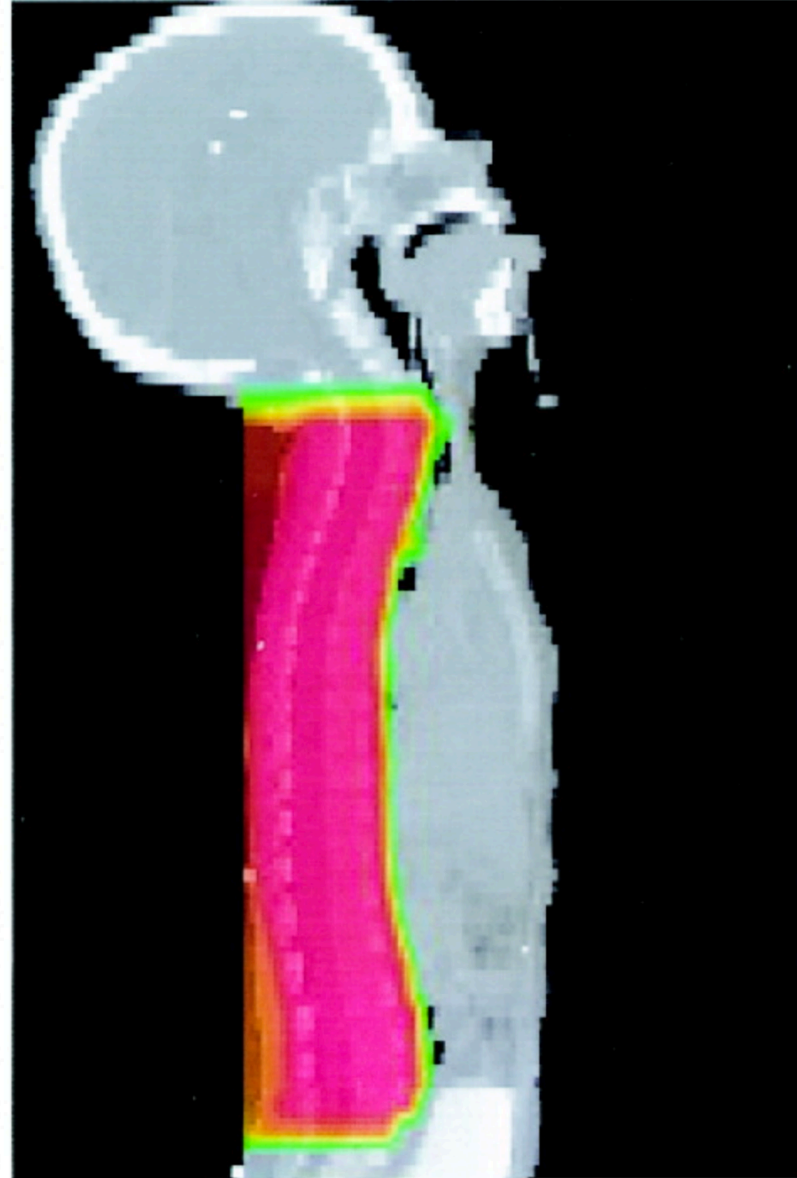
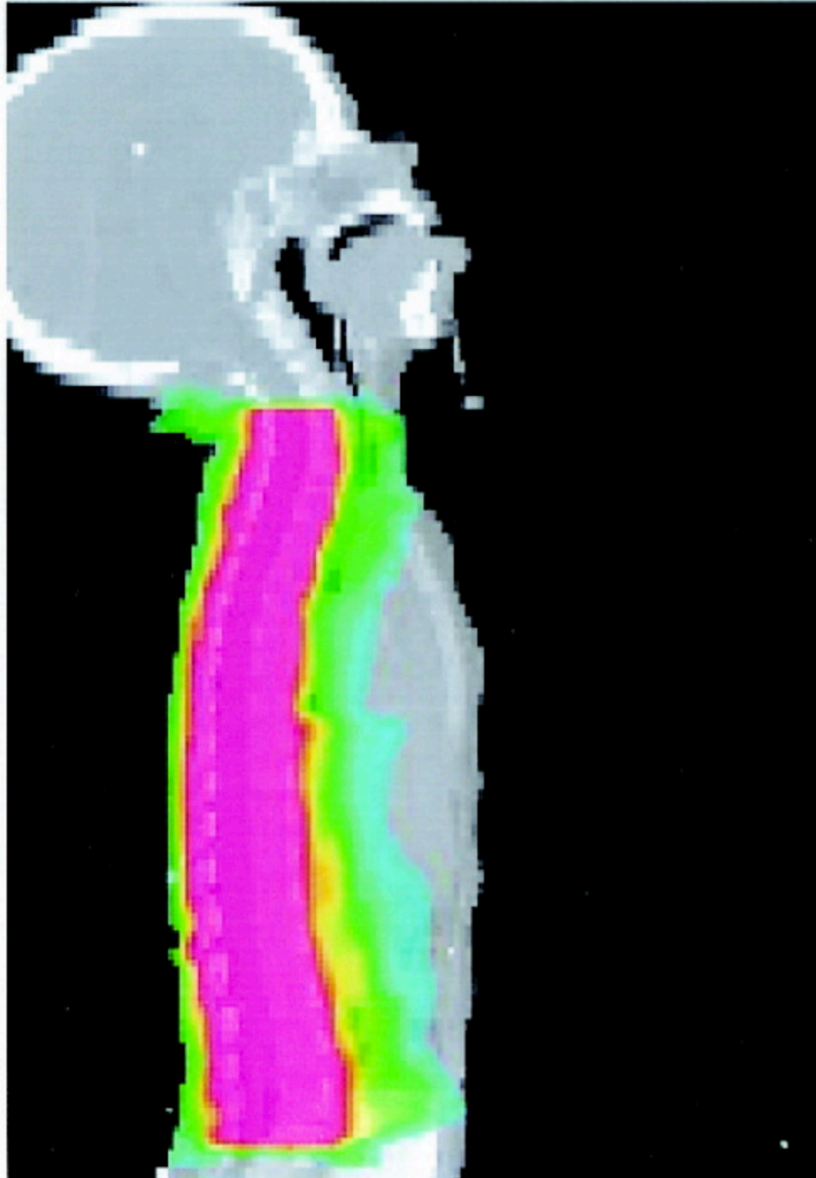


van der Weide et al., Radiother Oncol (2020)

Some evidence of advantages of PT over state-of-the-art X-ray therapy

Pediatric medulloblastoma: **Dose to 50% of the heart volume was reduced from 29.5% for IMRT to 0.5% for protons**

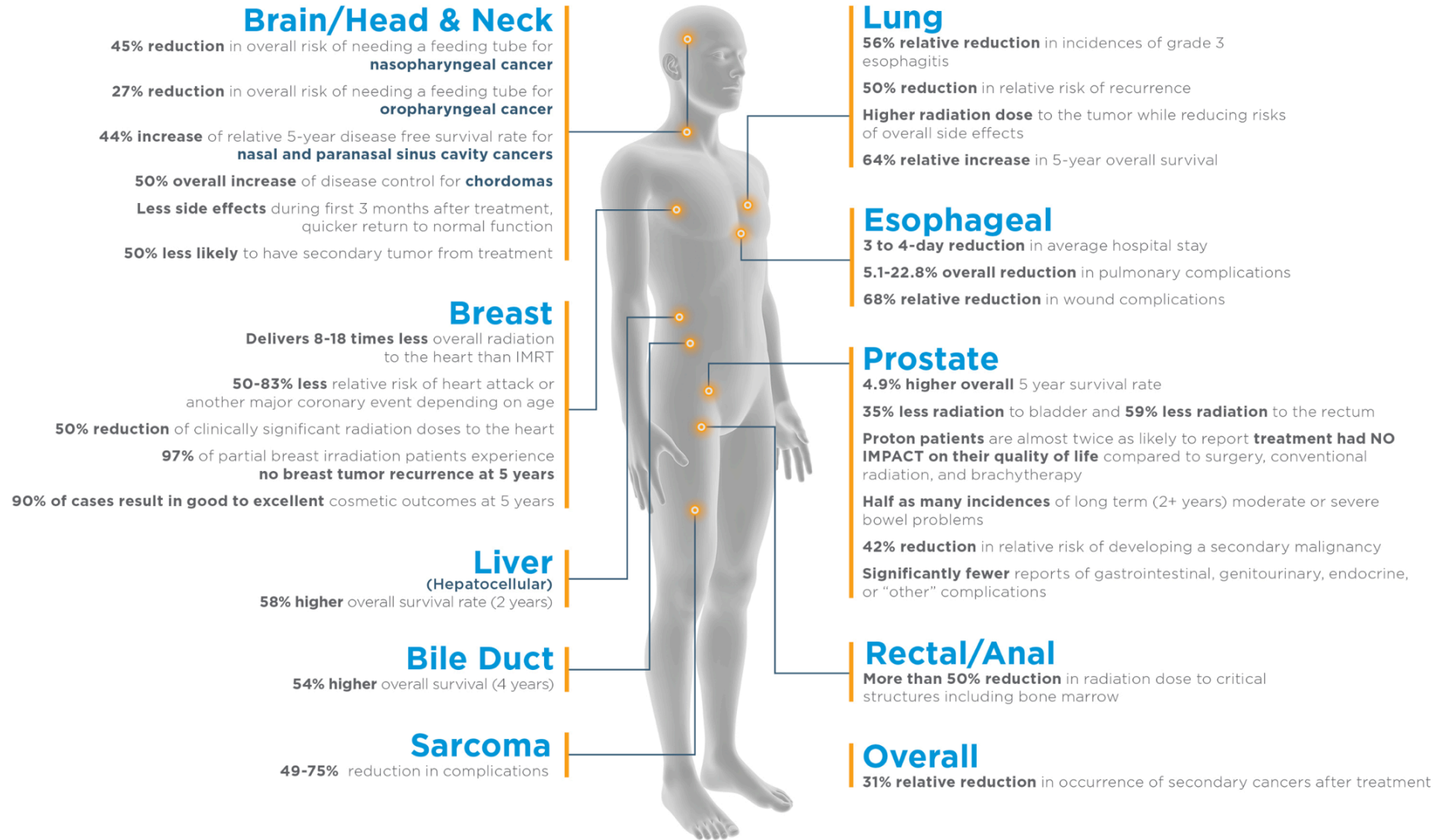
IMRT –
intensity
modulated
radiation
therapy



PT

Clair et al., IJROBP
(2004)

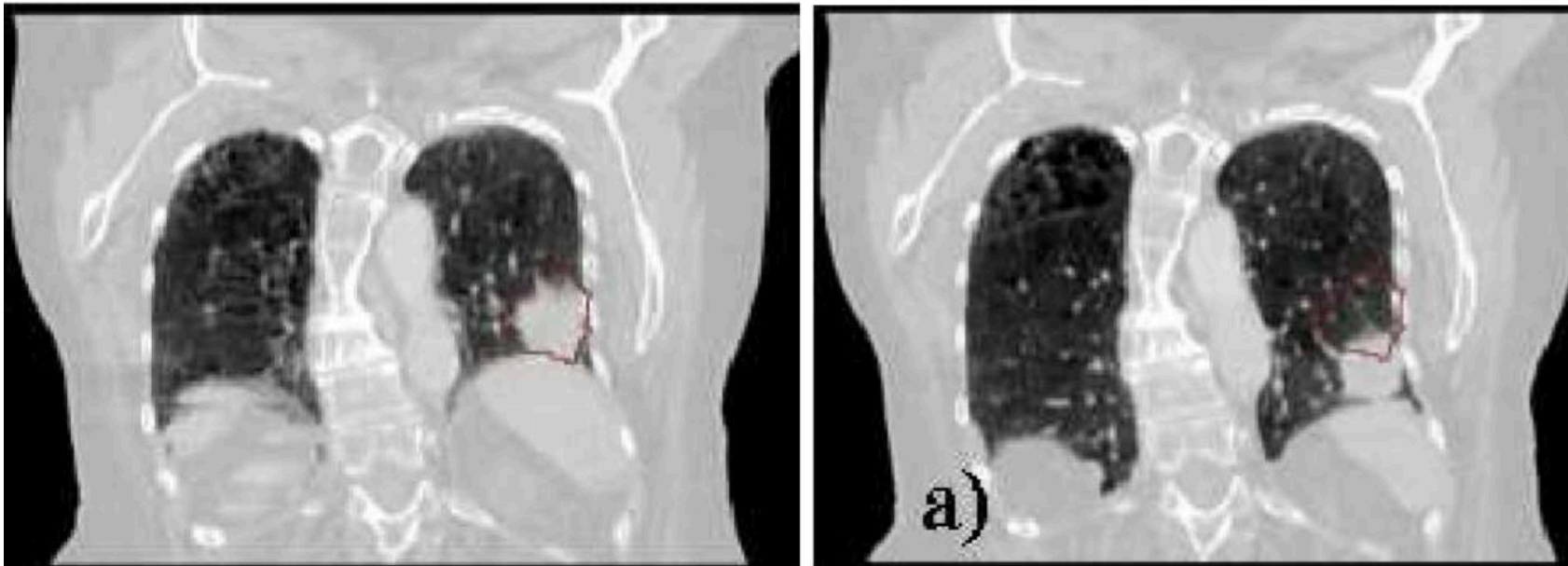
II - 1. Motivation: Proton therapy clinical benefits



II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: tumor displacement

- Breathing (intrafraction)

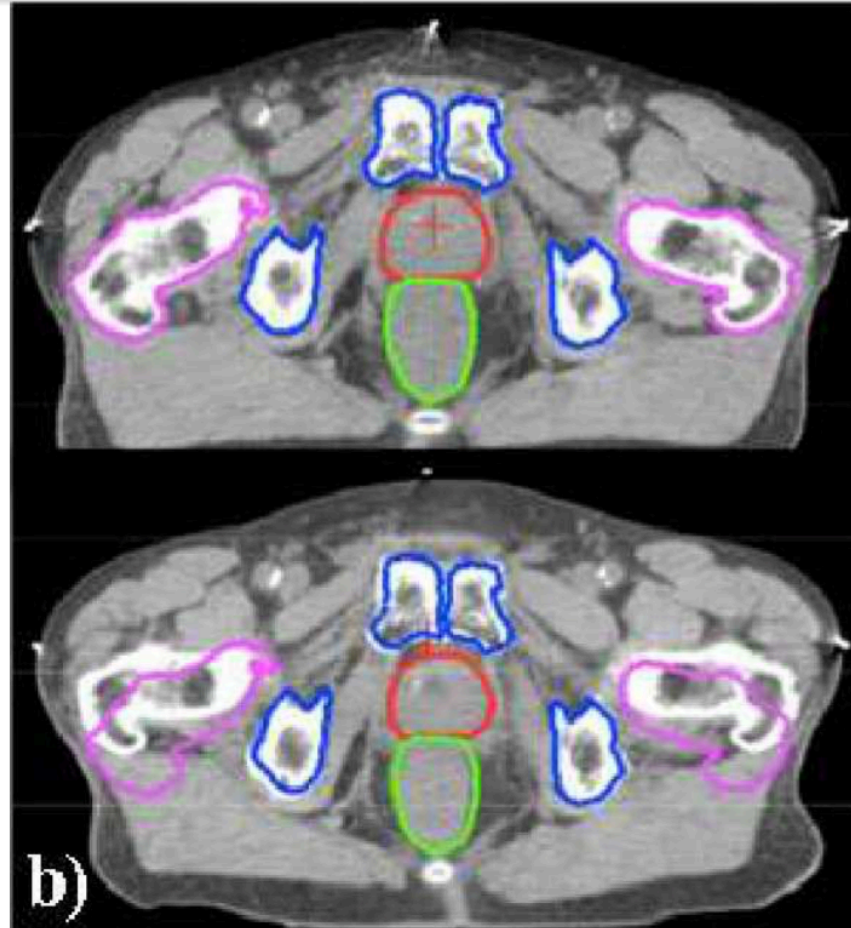


Engelsman and Bert 2011
Lüchtenborg PhD 2012

II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: patient displacement/deformation

- Mispositioning (interfraction)

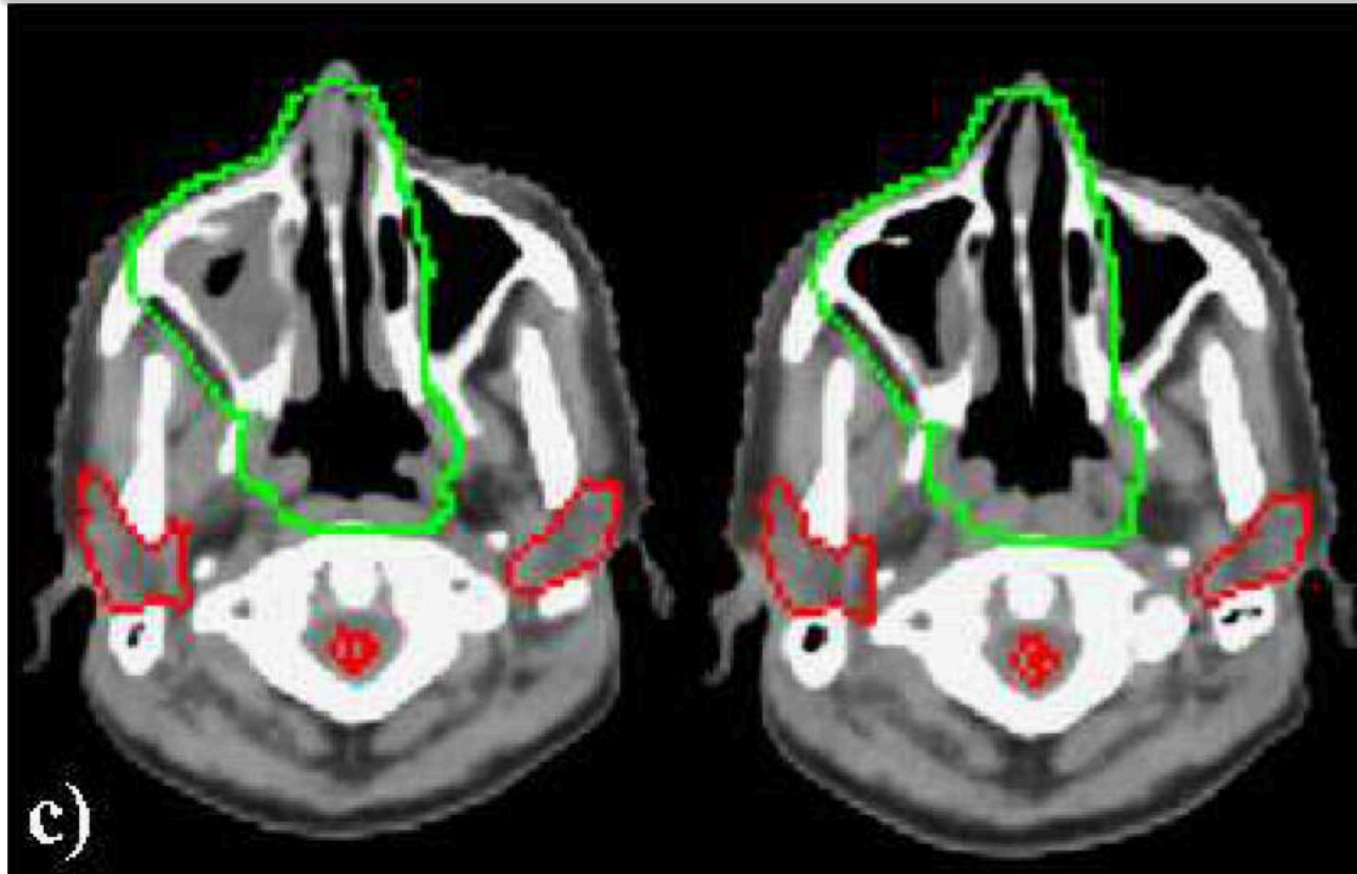


Engelsman and Bert 2011
Lüchtenborg PhD 2012

II - 2. Rationale for in-vivo imaging in proton RT

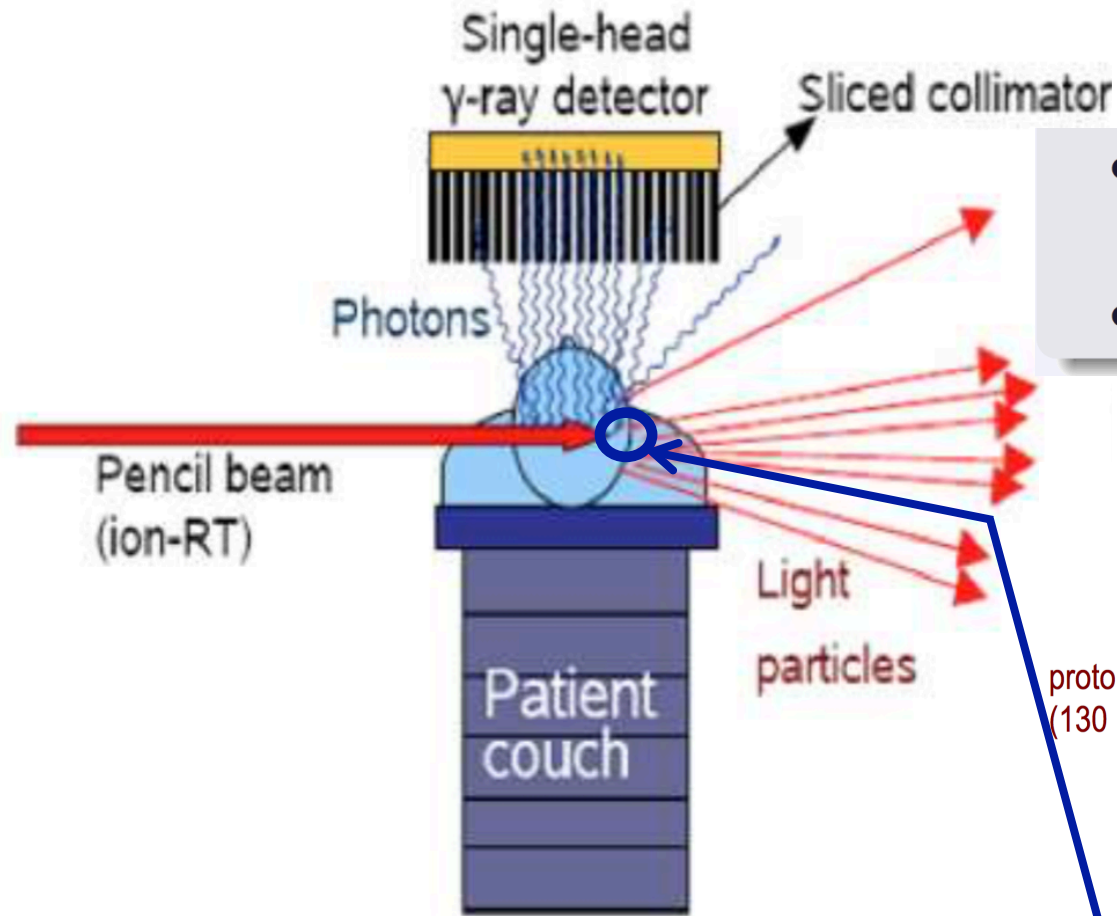
Target volumes and organ motion: cavity filling/wall thickening

- Tissue-density modification (interfraction)

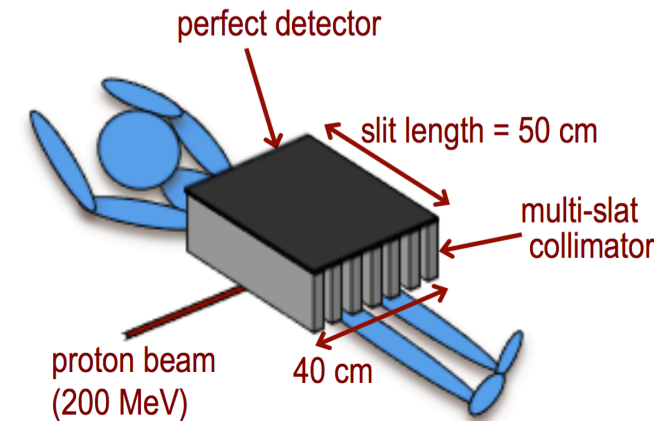
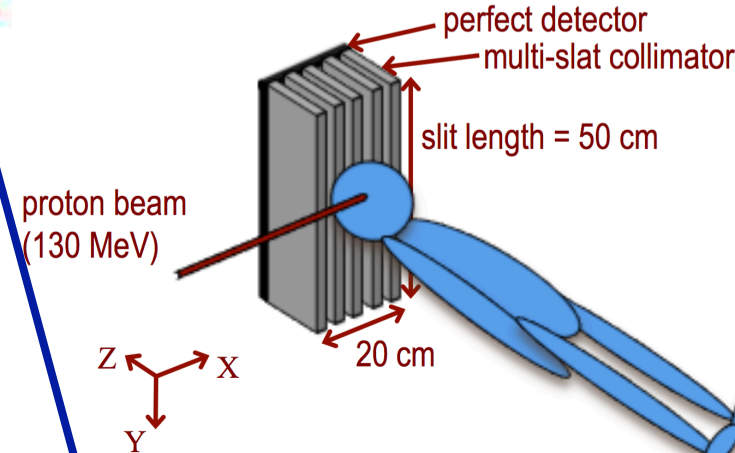


Engelsman and Bert 2011
Lüchtenborg PhD 2012

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT



- Head irradiation: nasal cavities (cavity filling) and pituitary (change in brain density)
- Pelvic irradiation: prostate (patient mispositioning)



(Cambraila Lopes PhD 2017)

Provides real-time images of selected region without rotation of beam source.

Image with prompt gammas “stops” at beam range

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.1 Filling of nasal cavity

Head irradiation (*NCAT*)

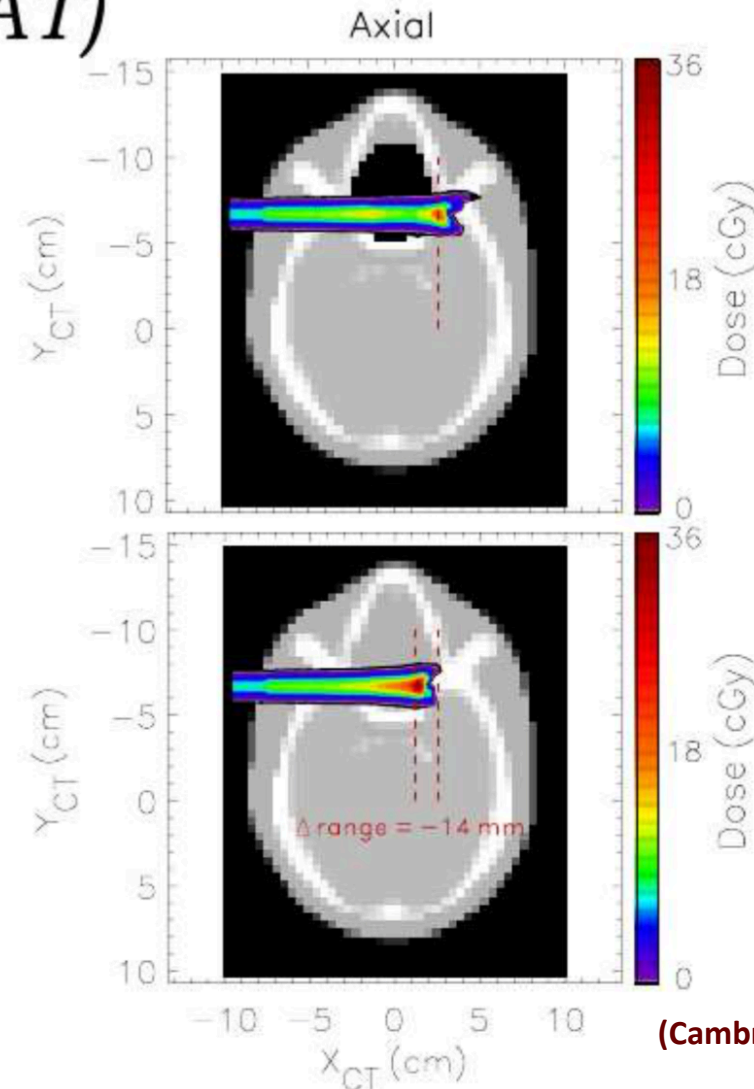
① Sphenoid region

❖ Treatment plan:

- Irradiation of a hypothetical tumor located in the sphenoid bone region
- **Empty nasal cavity** (air-filled)

❖ Compromised treatment:

- **Filled nasal cavity** with PMMA-like material
- Under-range shift of 14 mm
- Possible causes:
 - Patient cold → presence of mucus
 - Response after irradiation → edema, tissue swelling
 - Tumor growth

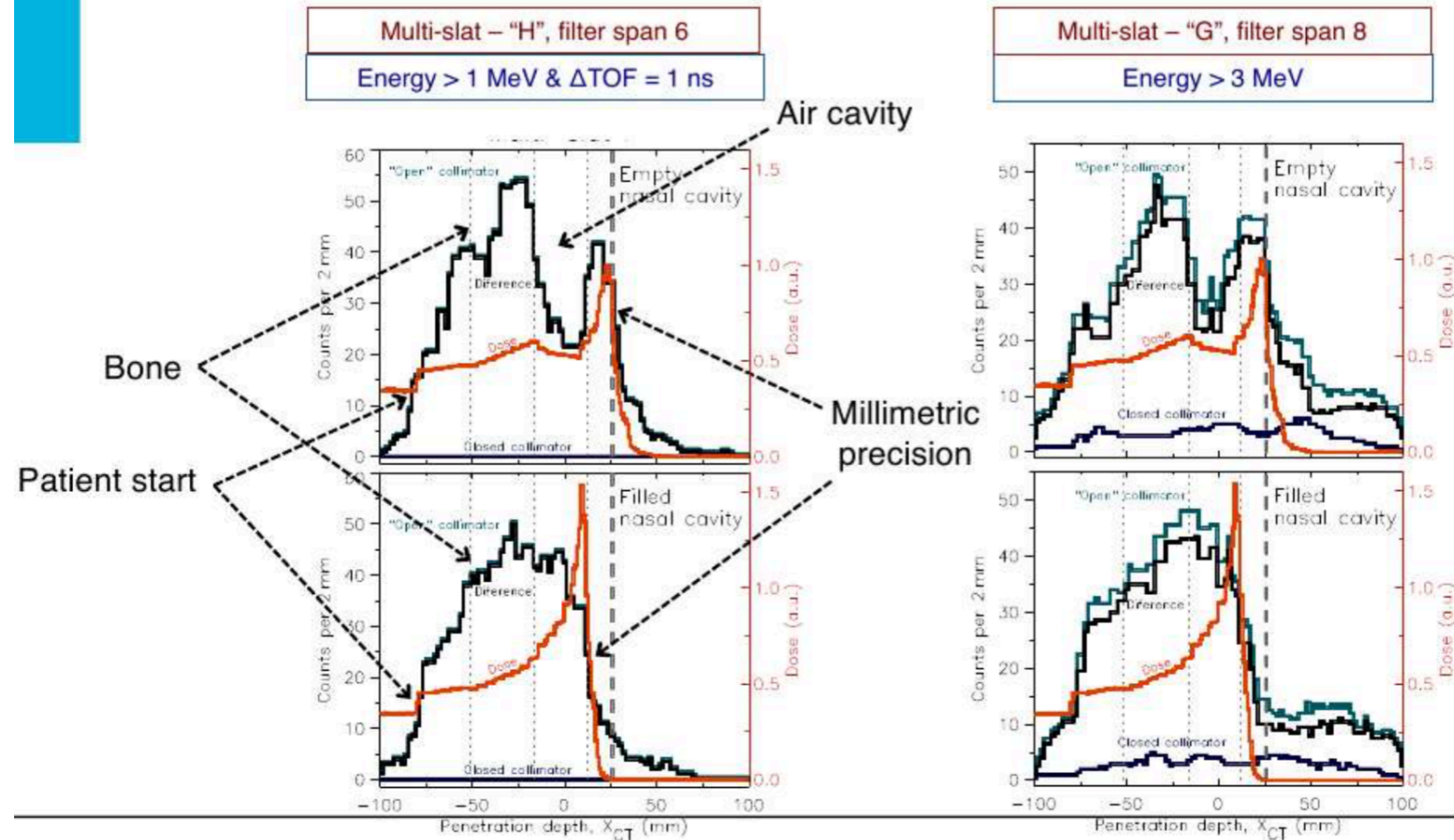


(Cabraia Lopes PhD 2017)

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.1 Filling of nasal cavity

① Sphenoid region Collimated PG profiles

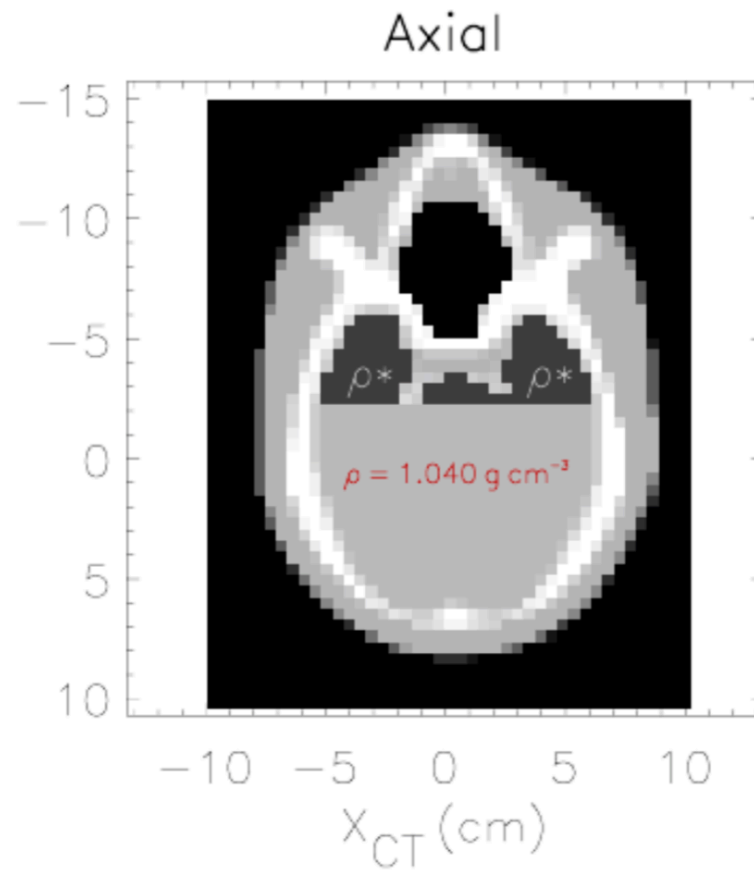


(Cabraia Lopes PhD 2017)

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.2 Change of brain density due to fractionated RT

- Conjecture: brain tissue hypo/hyperdense due to fractionated RT **Denham et al Radiother Oncol 2002**

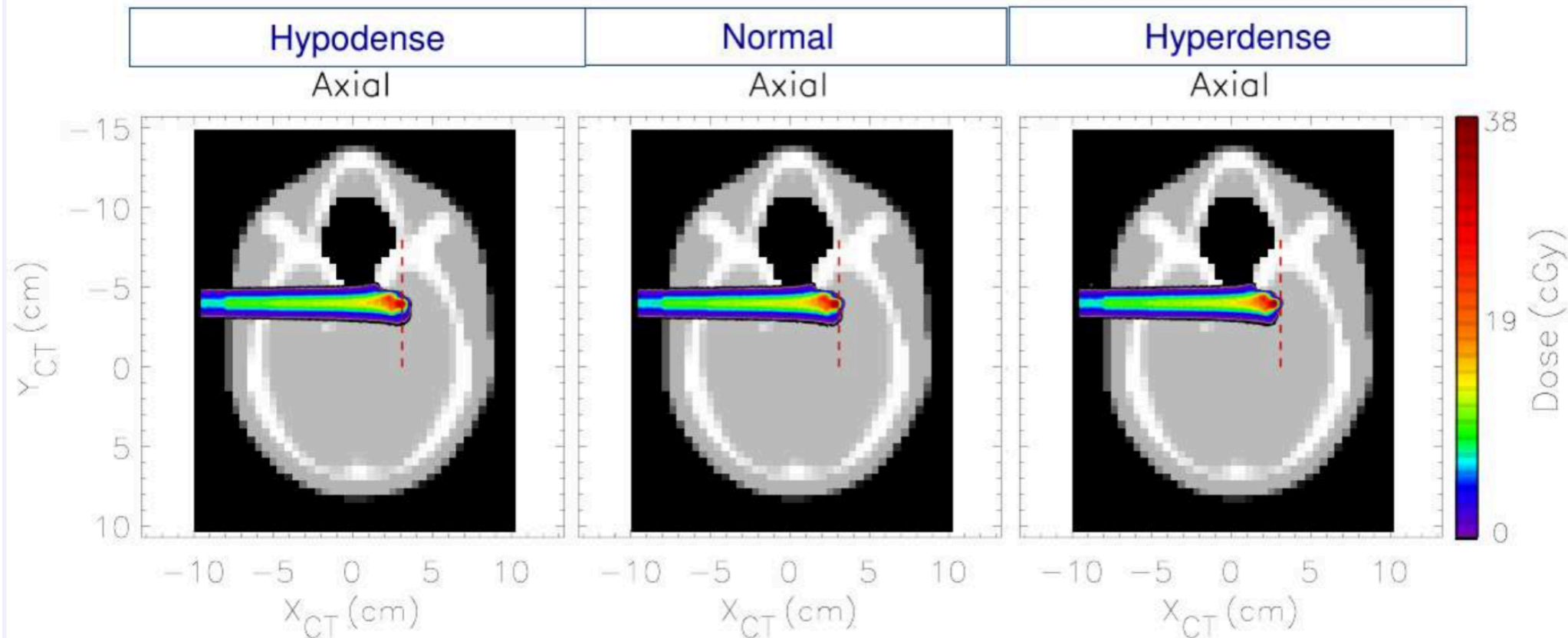


(Cabraia Lopes PhD 2017)

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.2 Change of brain density due to fractionated RT

- Conjecture: brain tissue hypo/hyperdense
- Corresponding dose distributions (protons):

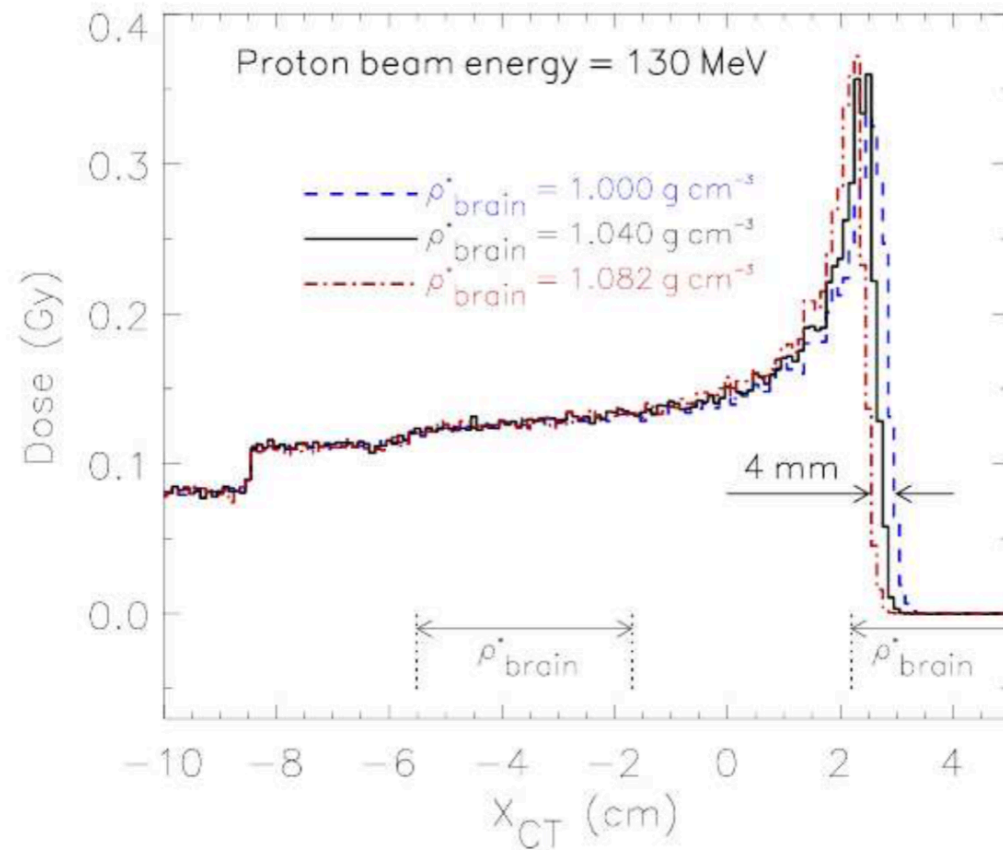


(Cambrailo Lopes PhD 2017)

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.2 Change of brain density due to fractionated RT

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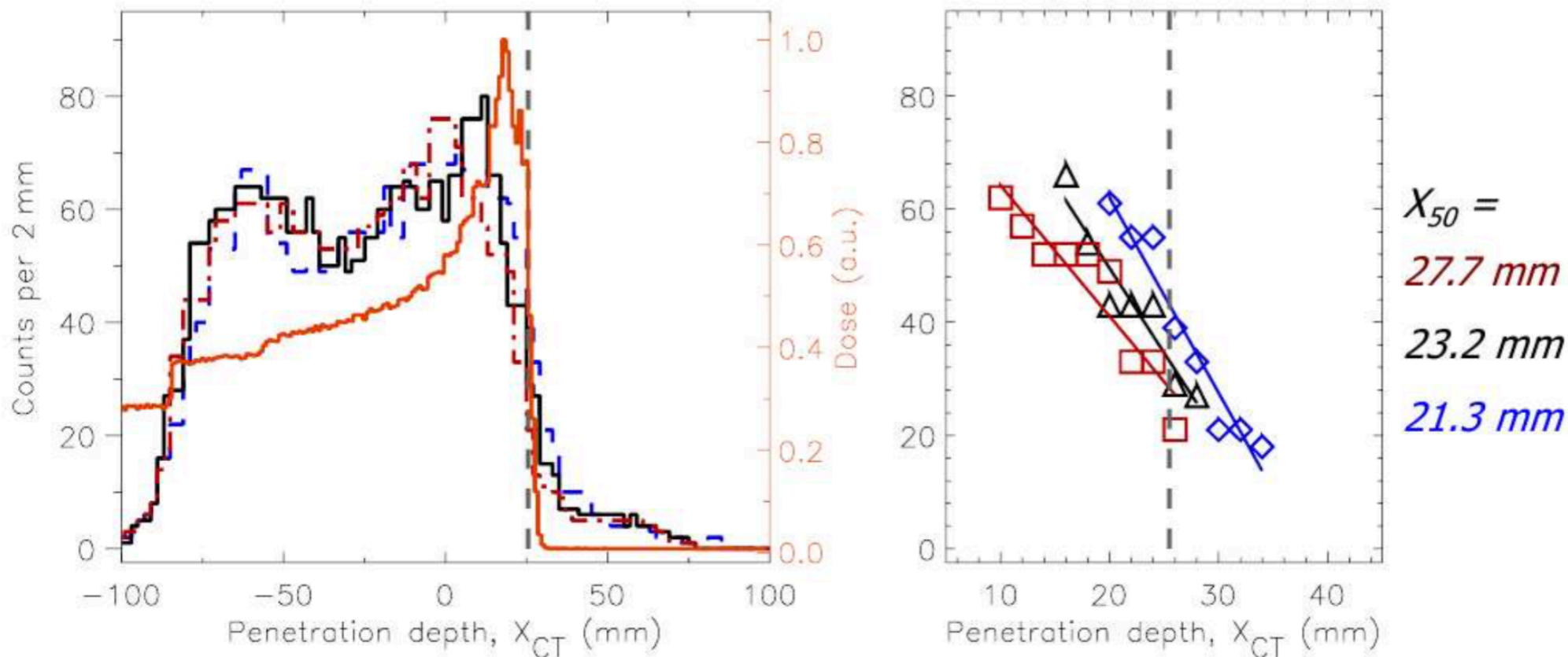


(Cabraia Lopes PhD 2017)

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.2 Change of brain density due to fractionated RT

- Conjecture: brain tissue hypo/hyperdense
- Monte Carlo results with proposed detector (Geant4):



(Cambrailo Lopes PhD 2017)

II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.3 Prostate: patient mispositioning Pelvis irradiation (*NCAT*)

Prostate

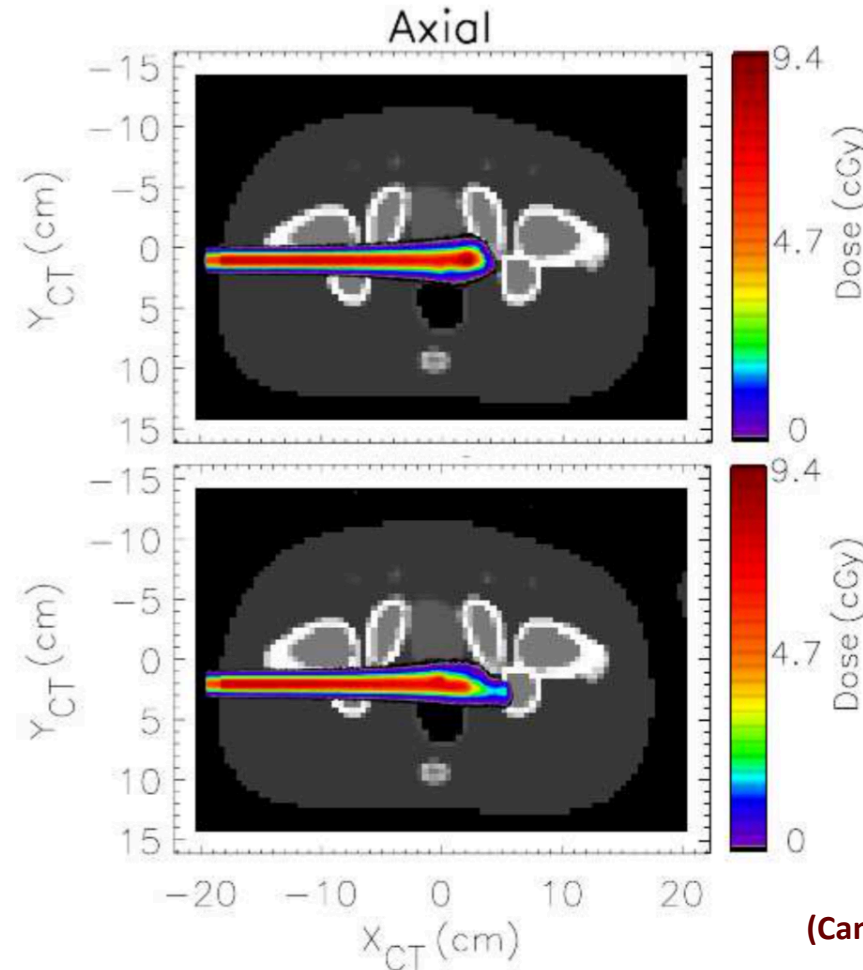
❖ Treatment plan:

- Irradiation of a hypothetical tumor in the prostate

❖ Compromised treatment:

○ Misalignment

- Patient 1 cm to ventral
- Dose proximal displacement
→ tumor underdosage
- Possible causes:
 - Mispositioning
 - Patient weight change



(Cambrailo Lopes PhD 2017)

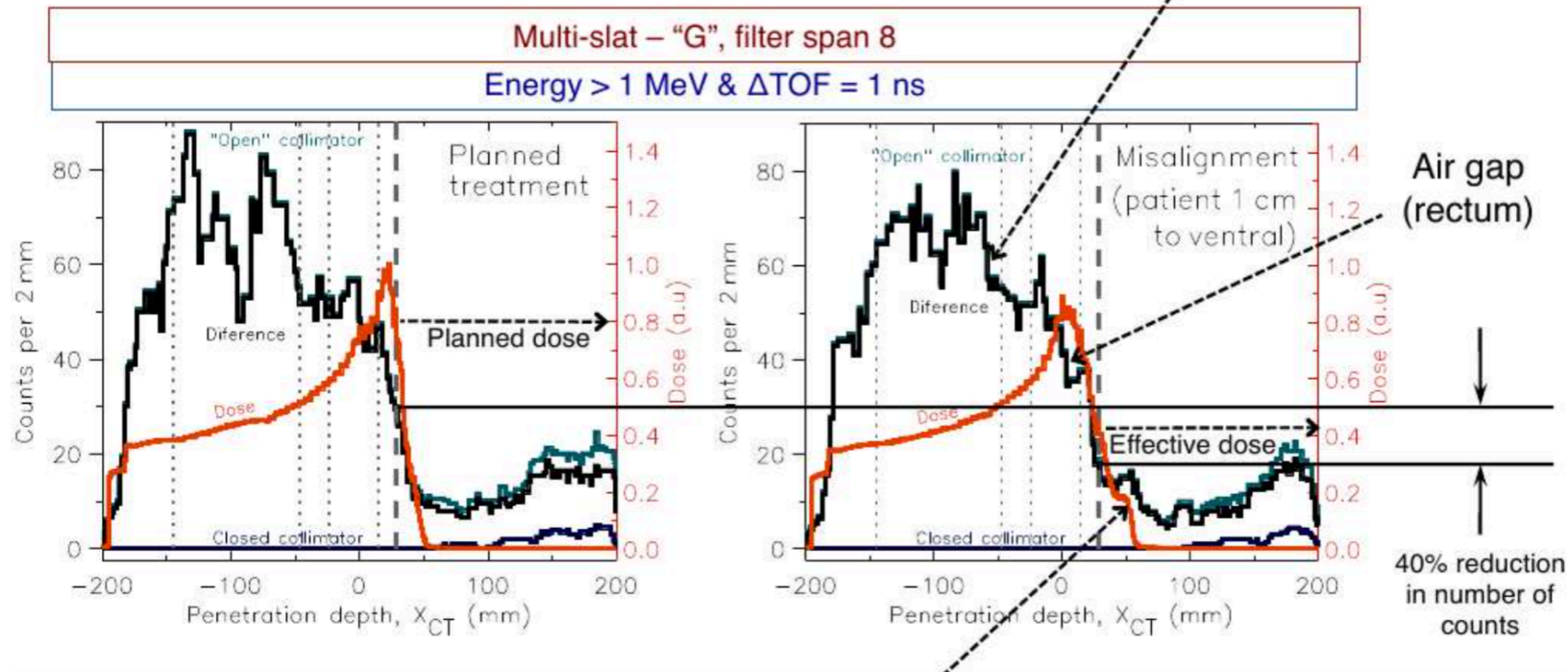
II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.3 Prostate: patient mispositioning

③ Prostate

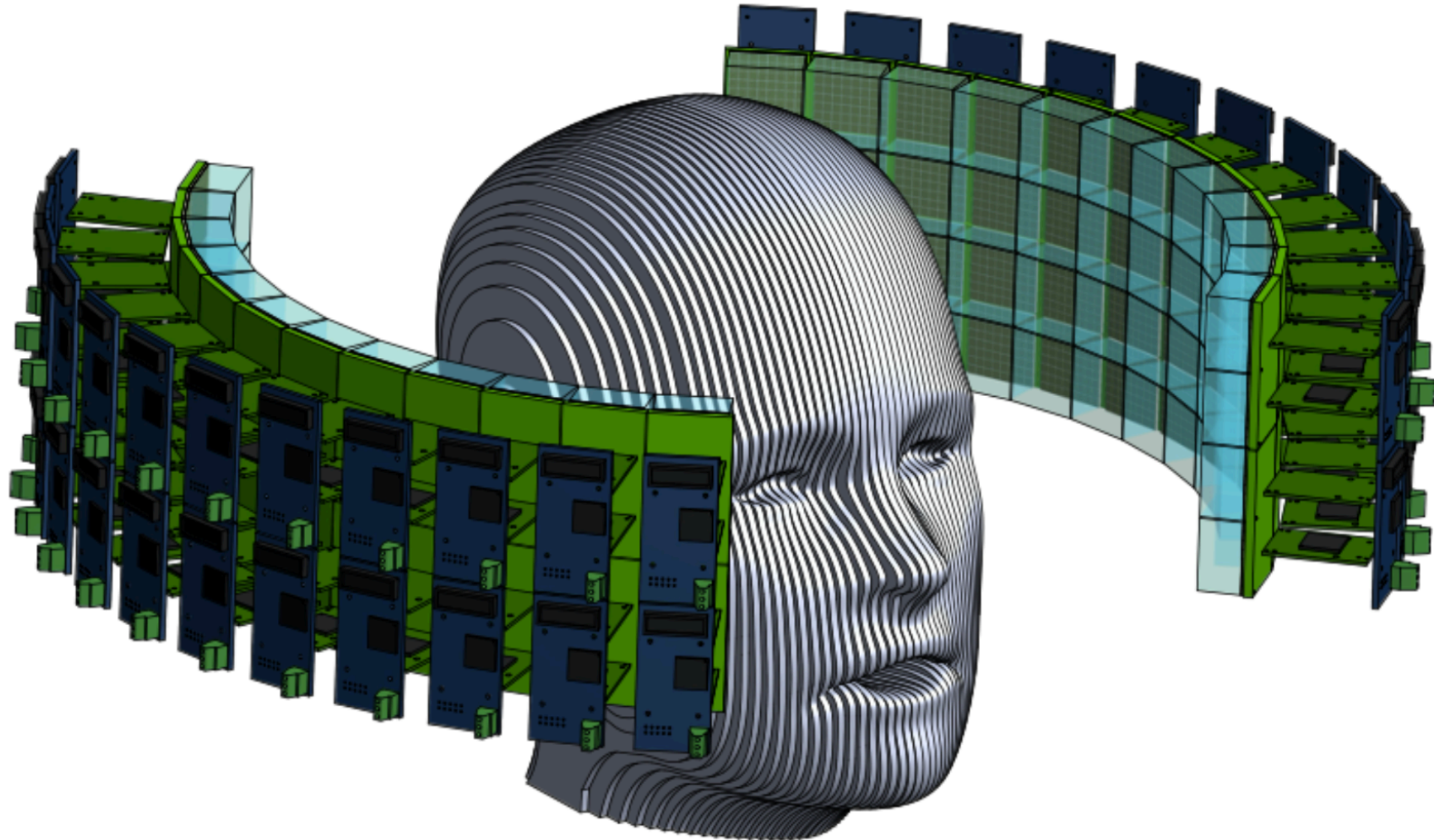
Collimated PG profiles

- Dose reduction of $\sim 46\%$ detected
- Correlation with anatomic features



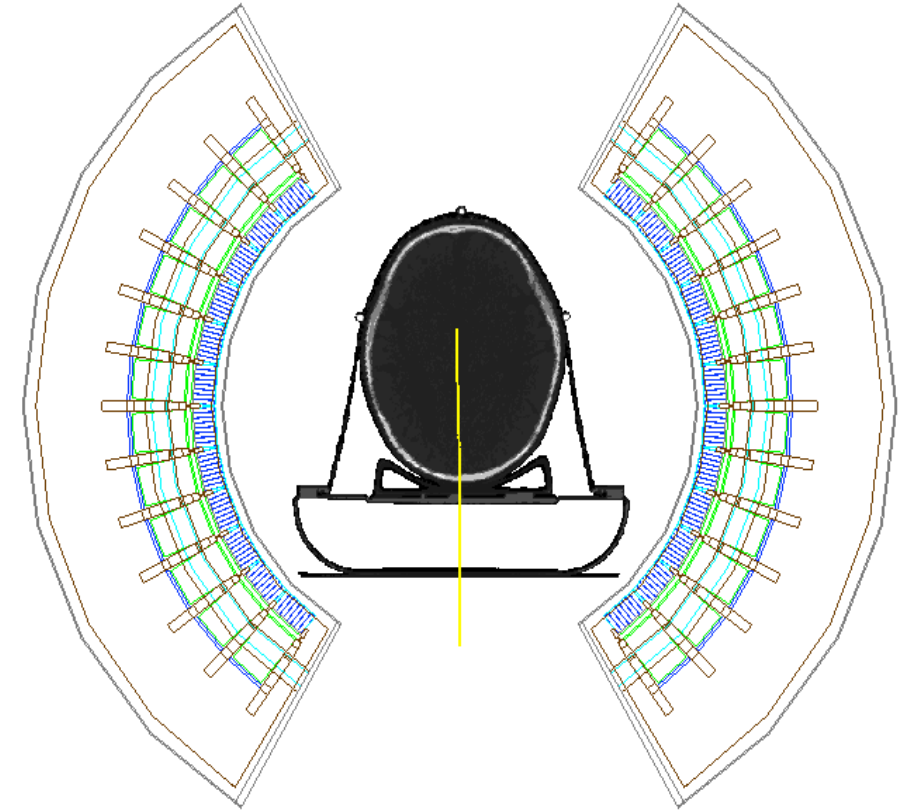
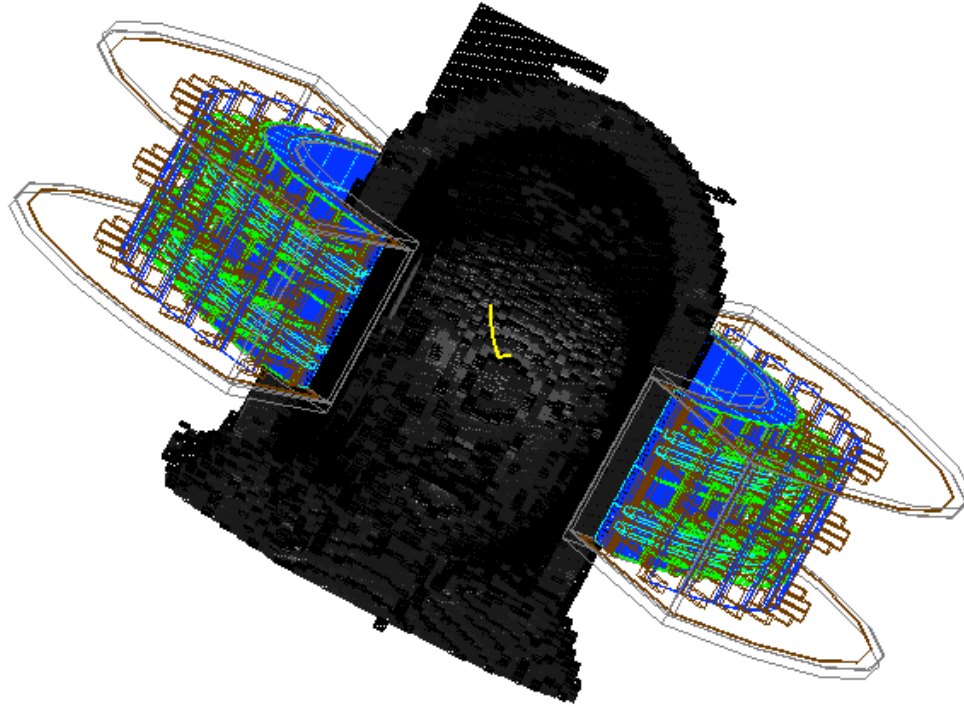
Excess dose corroborated by PG profile (Cambráia Lopes PhD 2017)

II - 4. In-beam time-of-flight PET for proton RT



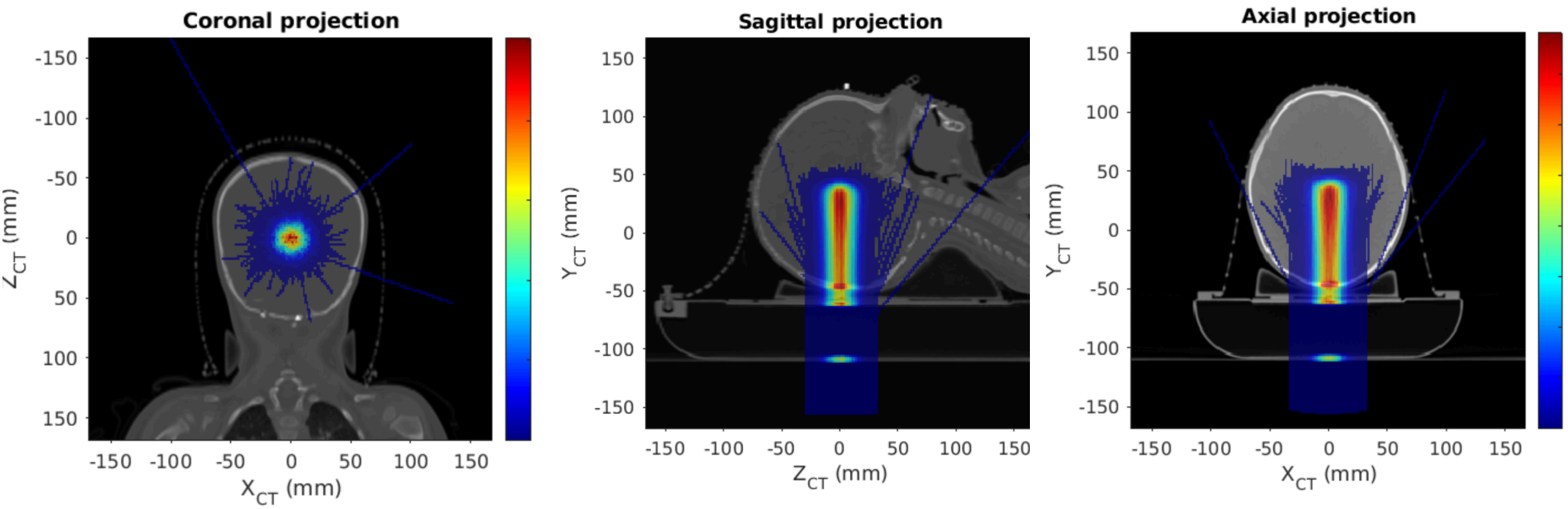
II - 4. In-beam time-of-flight PET for proton RT

A full simulation with an arbitrary single beamlet



Starting position: (0, -155, 0)
Direction: Y (gantry angle of 180 degrees)
Energy: 131 MeV
Beamlet spread size: 8.42 mm sigma
Beamlet duration: 4 ms

II - 4. In-beam time-of-flight PET for proton RT



Thank you for your attention

- The authors acknowledge the informatics support from the staff of the high-performance computing clusters of the University of Coimbra and Delft University of Technology (thousands of hours of parallel computation).
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- This work was funded in part by the Foundation for Fundamental Research (FOM), The Netherlands (grant no. 09NIG18), and by the European Union Seventh Framework program (grant agreements nos. 241851 and 264552).
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- Funding:



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