

with pre-treatment single energy CT.

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- 1. Motivation and Aim
- 2. Materials and Methods
- 3. Results and Discussion
- 4. Conclusions and Future Work

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## **Charged Particle Therapy**

Bragg Peak



http://images.iop.org/objects/med/talkingpoint/5/9/1/dam2.jpg



M. Goitein. A Physcist's Eye View. Springer, New York, 2008.

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## **Charged Particle Therapy**



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•Systematic from CT

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1-3% uncertainty

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## 1-3% uncertainty

(Rietzel, 2007; Kanematsu, 2003)

5-26% uncertainty

(Jakel, Reiss, 2007; Koybasi, 2014)

- Random Sources
  - Patient Positioning
  - Day-to-day beam range fluctuation (organ/ tumor motion)

#### Random/Slowly Systematic

- Patient Anatomy

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## **Possible Solution:**

Daily: Carbon Radiography

Weekly/bi-weekly: Carbon Tomography

- RSP distribution of the patient (prior and in between treatments);
- In combination with fast computational hardware, may be able to check the adequacy of the treatment before its delivery, or even modify beam angles to optimize the treatment delivery;
- Pretreatment monitoring of Patient Setup;
- High density resolution and low dose images. (Schneider, 1994)



Clinical expansions because of range uncertainties are 3.5% ± 1mm

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## Hypotheses

Is it possible to reduce clinical range expansions to below 0.5%±1mm using carbon radiography (or Carbon-CT) combined with singleenergy computed tomography (SECT)?

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# E.g. Prostate has a 20cm WEL -> ~8mm expansion is reduced to ~1 - 2mm

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## **2.2. Calibration Phantoms**

#### • GAMMEX PHANTOM

- 33x33x33 cm<sup>3</sup>
- 13 Materials with known composition (Watanabe *et al.*)



#### SLAB PHANTOM

 CB2-30% CaCO<sub>3</sub>; CB2-50% CaCO<sub>3</sub>; Inner Bone; Cortical Bone; LN-450; LN-300; Adipose; CT solid water; Water



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## 2.3. Reference Carbon Radiography and theoretical RSP

• Monte Carlo simulation with Geant4 v.4.9.6, validated for carbon ion therapy (Lechner, A. 2010)

 Theoretical RSP → Stopping Power (SP) of Carbon crossing SLAB phantom

$$RSP_{tissue} = \frac{SP(E)_{tissue}}{SP(E)_{water}}$$

- Reference Carbon Radiography from
  GAMMEX phantom
- $\circ~~$  E\_in, E\_out, Entrance/Exit coordinates and directions







## 2.4. Single Energy Computed Tomography (SECT)

- ImaSim (Landry,2009) to reproduce 120kVp CT image of the phantoms
- Filtered backprojection reconstruction with Shepp-Logan filter.
- HU unit for each material for theoretical calibration curve







## 2.5. Carbon Digitally Reconstructed Radiography (CDRR)

## 2.5.1 Particle Propagation/Path

- Particle by Particle > GPU-based
- Entrance and Exit
- Coordinates
- Direction
- Cubic Spline Path
  - Allows linear and non linear trajectories
  - $\vec{A}t^3 + \vec{B}t^2 + \vec{C}t + \vec{D} = \vec{S}(t)$
- Track of Voxel ID along path

Possible path





## 2.5. Digitally Reconstructed Radiography 2.5.2 Energy Loss

- Compute Total Energy loss of each Carbon
- Binning of the path, allowing multiple steps per voxel ( $\Delta t$ )
- Voxel ID from propagation
- HU to RSP<sub>tissue</sub> from CT

$$E_{out} = E_{initial} - \sum \left( RSP_{tissue} \times SP(E)_{water} \times \Delta t \right)$$

 New Energy distribution - > Carbon Digitally Reconstructed Radiograph

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Gradient Descent
 Optimization

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# Gradient Descent Optimization



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#### 3 iterations



	RSP CNAO	RSP G4	RSP Opt	Error CNAO	Error Opt
LN-300	0.32	0.30	0.33	-6.32	-10.42
LN-450	0.46	0.45	0.48	-2.25	-6.86
Adipose	0.89	0.92	0.94	2.54	-2.28
CTsolidWater	1.00	1.01	0.95	0.86	6.18
Inner Bone	1.09	1.10	1.15	0.49	-4.29
СВ2-30	1.22	1.30	1.28	5.84	1.15
CB2-50	1.39	1.46	1.46	4.86	0.10
Cortical Bone	1.53	1.67	1.61	8.46	4.04

	CNAO	Optimized	=	Reduction
Mean Energy Error:	-0.77	<b>───→</b> -0.04	—	95%

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Mean Energy Error:

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- Mean Energy difference is indeed minimized
- Very many different materials (all errors (each material) average out so we have small mean energy difference)
- Too many RSP (materials) to be optimized



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#### Question

What should we really minimize? The mean Energy difference? Range difference?

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•Better optimization methods (minimization value; optimization method; reduced RSP set to be optimized)

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•Investigate possible systematic errors (material dependent), due to our method

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•Possibility to **use Dual Energy CT** (DECT) and information from **multiple angle carbon radiographs** to better estimate RSP values from different tissue materials.

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•Investigate possible systematic errors (material dependent), due to our method

•Possibility to **use Dual Energy CT** (DECT) and information from **multiple angle carbon radiographs** to better estimate RSP values from different tissue materials.

•Experimental RSP (for reference) for a carbon beam will be obtained and the possibility to use this method on alpha particles will also be considered.

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## 4.2. To Sump Up

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Based on these preliminary results, carbon RSP uncertainties can be reduced using information from combined carbon radiographs and SECT data.

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## 4.2. To Sump Up

Based on these preliminary results, carbon RSP uncertainties can be reduced using information from combined carbon radiographs and SECT data.

We are still far from our aim of reducing range errors to <0.5%

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Massachusetts General Hospital





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## Thank you so much for your attention/time!

**Questions?** 

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