Particle Physics Techniques Applied to Health

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LIP training internship

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Outline

- I Advances in Nuclear Medicine
 - 1. RPC-based TOF-PET
 - 2. Development of New Gamma Cameras
- II Advances in Imaging in Proton Radiotherapy
 - 1. Motivation
 - 2. Rationale for in-vivo imaging in proton radiotherapy (RT)
 - 3. The multi-slat concept for prompt-gamma imaging in proton RT
 - 4. In-beam time-of-flight PET for proton RT

Rationale is based on state-of-the-art of PET (positron emission tomography):

• Technique experiences growing utilization in nuclear medicine, e.g. for diagnostic/screening/staging of oncologic, neurologic, and cardiac disease.



- E.g. Palmisano et al. Saudi J Gastroenterol 2011
- F, 64 a., symptoms: palpable supracavicular, ganglionic adenopathies, asthenia, anorexia.
- PET-based diagnostic: adenocarcinoma of the ascendent colon.

I - 1. RPC-based TOF-PET Rationale:

 PET technology is extremely costly (millions of €); patient examinations are equally costly (ca. 4000 €), lengthy in time, morphologically imprecise, often inconclusive when imaging small lesions (detectability, sensitivity, and specificity); and the patient bears a non-negligible amount of radiation dose.



I - 1. RPC-based TOF-PET



I - 1. RPC-based TOF-PET



LIP, July 8th, 2021

I - 1. RPC-based TOF-PET

Implementation (software):

• R&D in simulation and reconstruction



- Collaboration between Laboratório de Instrumentação e Física Experimental de Partículas, **LIP** and the Universitary Hospital of Coimbra **Nuclear Medicine Department**
- Gamma cameras are used to perform scintigraphy: a medical imaging modality used to obtain functional images. E.g. cardiology, pneumology, oncology (staging of tumors, evaluate therapeutic response)

Heart

study



Bone scans



Lung scintigraphy



Kidneys study

Mid

Mid

Rest

Systole

Stress

Diastole

Areas without

normal blood flow



Normal

Gamma camera working principle



Collimators prototypes



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Parallel-holes collimator (hexagones 0.5 mm "diameter)



Made of tungsten using Selective laser melting







- Specification by João Marcos
- Designed by Eng. Rui Alves (LIP mechanical workshop)
- Manufactured by M&I Materials

Collimators prototypes



Pinhole collimator (1 mm hole, 0.5 mm channel edge height)

Made of Tungsten alloy (95.5% W, 4.5% Co)

- Specification by João Marcos
- **Designed** by DURIT (Albergaria-a-Velha)
- Manufactured by DURIT









Phantom imaging



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Pinhole collimator



Parallel-hole collimator



Crossed capillary tubes phantom







Event density vs XY



II - 1. Motivation: Proton therapy physical advantage over photons



II - 1. Motivation: Proton therapy physical advantage over IMRT



(Proton Therapy Today 2019)

II - 1. Motivation: Proton therapy clinical benefits



Lung

56% relative reduction in incidences of grade 3 esophagitis

50% reduction in relative risk of recurrence

Higher radiation dose to the tumor while reducing risks of overall side effects

64% relative increase in 5-year overall survival

Esophageal

3 to 4-day reduction in average hospital stay
5.1-22.8% overall reduction in pulmonary complications
68% relative reduction in wound complications

Prostate

4.9% higher overall 5 year survival rate

35% less radiation to bladder and 59% less radiation to the rectum

Proton patients are almost twice as likely to report **treatment had NO IMPACT on their quality of life** compared to surgery, conventional radiation, and brachytherapy

Half as many incidences of long term (2+ years) moderate or severe bowel problems

42% reduction in relative risk of developing a secondary malignancy

Significantly fewer reports of gastrointestinal, genitourinary, endocrine, or "other" complications

Rectal/Anal

More than 50% reduction in radiation dose to critical structures including bone marrow

Overall 31% relative reduction in occurrence of secondary cancers after treatment



*References available upon request. Results from separate studies compared in some instances. The benefits of proton therapy for each individual patient will vary based on their individual diagnosis. A personal consultation with a proton-trained physician is recommended in all cases.

Brain/Head & Neck

45% reduction in overall risk of needing a feeding tube for nasopharyngeal cancer

27% reduction in overall risk of needing a feeding tube for oropharyngeal cancer

44% increase of relative 5-year disease free survival rate for nasal and paranasal sinus cavity cancers

50% overall increase of disease control for chordomas

Less side effects during first 3 months after treatment, quicker return to normal function

50% less likely to have secondary tumor from treatment

Breast

Delivers 8-18 times less overall radiation to the heart than IMRT

50-83% less relative risk of heart attack or another major coronary event depending on age

50% reduction of clinically significant radiation doses to the heart

97% of partial breast irradiation patients experience no breast tumor recurrence at 5 years

90% of cases result in good to excellent cosmetic outcomes at 5 years

(Hepatocellular) 58% higher overall survival rate (2 years)

> **Bile Duct** 54% higher overall survival (4 years)

Sarcoma 49-75% reduction in complications

II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: tumor displacement

• Breathing (intrafraction)



Engelsman and Bert 2011 Lüchtenborg PhD 2012

II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: patient displacement/deformation

• Mispositioning (interfraction)



Engelsman and Bert 2011 Lüchtenborg PhD 2012

II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: cavity filling/wall thickening

• Tissue-density modification (interfraction)



Engelsman and Bert 2011 Lüchtenborg PhD 2012



region without rotation of beam source.

- 3.1 Filling of nasal cavity Head irradiation (NCAT)
 - ① Sphenoid region
 - Treatment plan:
 - Irradiation of a hypothetical tumor located in the sphenoid bone region
 - Empty nasal cavity (air-filled)
 - Compromised treatment:
 - Filled nasal cavity with PMMA-like material
 - Under-range shift of 14 mm
 - o Possible causes:
 - Patient cold → presence of mucus
 - Response after irradiation → edema, tissue swelling
 - Tumor growth



II - 3. The multi-slat concept for prompt-gamma imaging in proton RT



3.2 Change of brain density due to fractionated RT

• Conjecture: brain tissue hypo/hyperdense due to fractionated RT Denham et al Radiother Oncol 2002



- II 3. The multi-slat concept for prompt-gamma imaging in proton RT
 - 3.2 Change of brain density due to fractionated RT
 - Conjecture: brain tissue hypo/hyperdense
 - Corresponding dose distributions (protons):



II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

3.2 Change of brain density due to fractionated RT

- Conjecture: brain tissue hypo/hyperdense
- Corresponding dose profiles (protons):



- II 3. The multi-slat concept for prompt-gamma imaging in proton RT
 - 3.2 Change of brain density due to fractionated RT
 - Conjecture: brain tissue hypo/hyperdense
 - Monte Carlo results with proposed detector (Geant4):



3.3 Prostate: patient mispositioning Pelvis irradiation (NCAT)

Prostate

- Treatment plan:
 - Irradiation of a hypothetical tumor in the prostate
- Compromised treatment:
 - o Misalignment
 - →Patient 1 cm to ventral
 - Dose proximal displacement
 - → tumor underdosage
 - Possible causes:
 - Mispositioning
 - Patient weight change





II - 4. In-beam time-of-flight PET for proton RT

II - 4. In-beam time-of-flight PET for proton RT

A full simulation with an arbitrary single beamlet

Starting position: (0, -155, 0) Direction: Y (gantry angle of 180 degrees) Energy: 131 MeV Beamlet spread size: 8.42 mm sigma Beamlet duration: 4 ms

II - 4. In-beam time-of-flight PET for proton RT

Thank you for your attention

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