

# Particle Physics Techniques Applied to Health

Paulo Crespo<sup>1,2</sup>



# Outline

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## I – Advances in Nuclear Medicine

1. RPC-based TOF-PET
2. Development of New Gamma Cameras

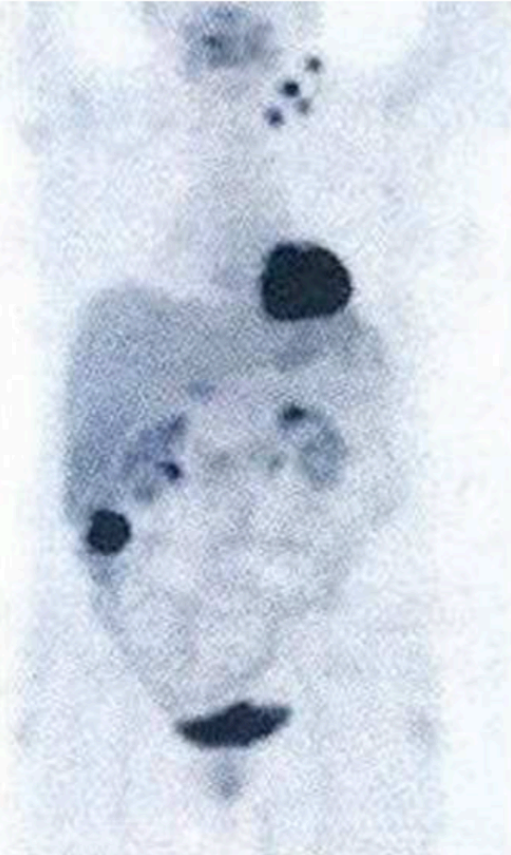
## II – Advances in Imaging in Proton Radiotherapy

1. Motivation
2. Rationale for in-vivo imaging in proton radiotherapy (RT)
3. The multi-slat concept for prompt-gamma imaging in proton RT
4. In-beam time-of-flight PET for proton RT

# I - 1. RPC-based TOF-PET

Rationale is based on state-of-the-art of PET (positron emission tomography):

- Technique experiences growing utilization in nuclear medicine, e.g. for diagnostic/screening/staging of oncologic, neurologic, and cardiac disease.

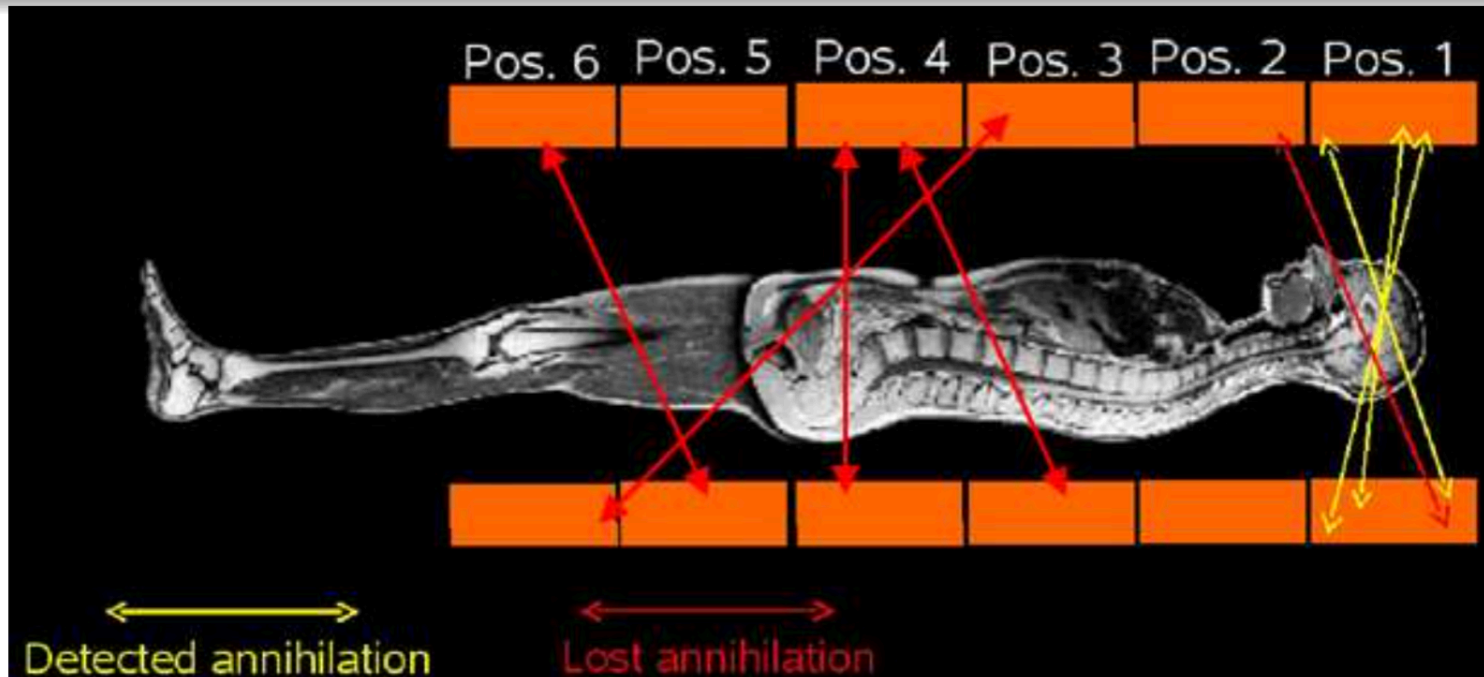


- E.g. **Palmisano et al. Saudi J Gastroenterol 2011**
- F, 64 a., symptoms: palpable supracavicular, ganglionic adenopathies, asthenia, anorexia.
- PET-based diagnostic: adenocarcinoma of the ascendent colon.

# I - 1. RPC-based TOF-PET

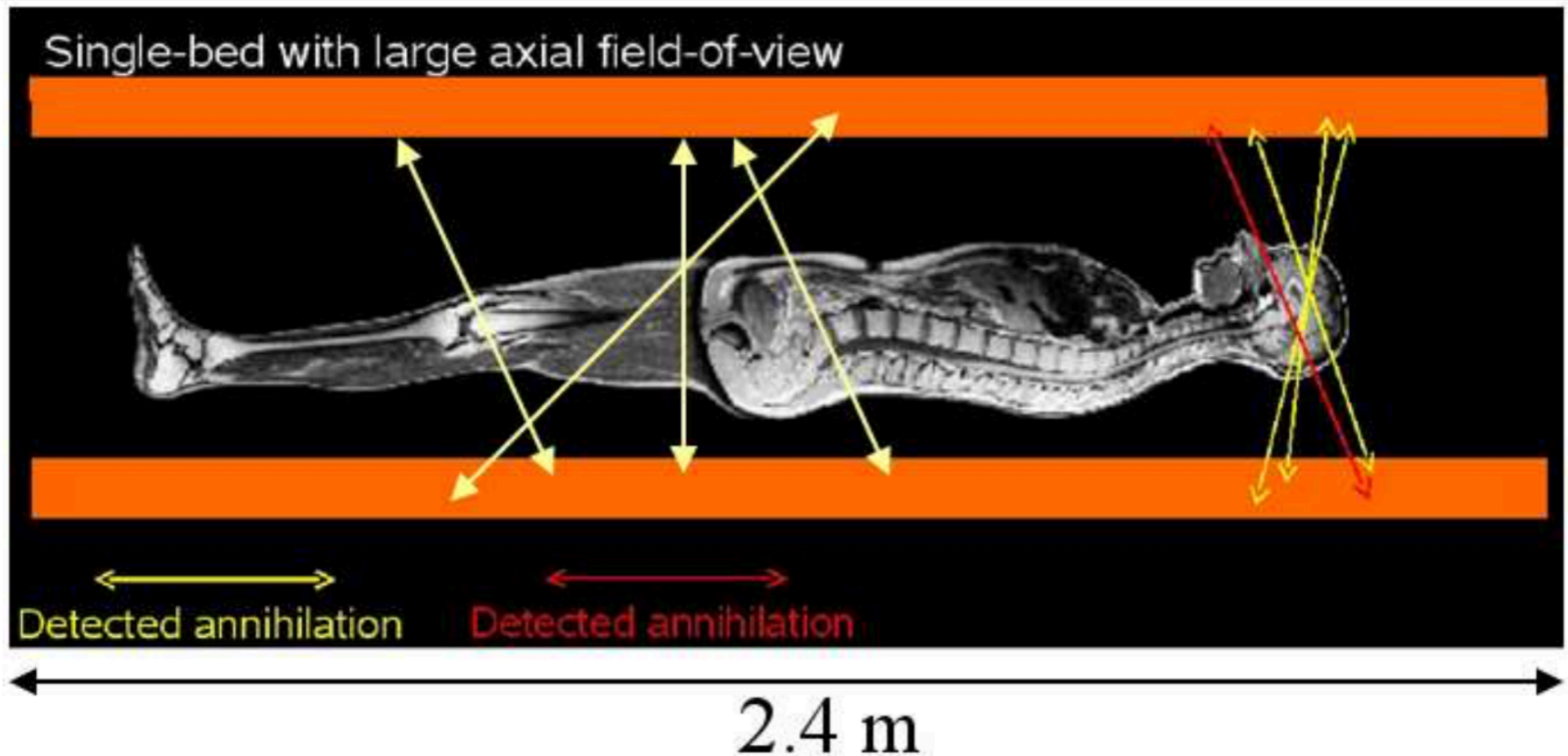
## Rationale:

- PET technology is extremely costly (millions of €); patient examinations are equally costly (ca. 4000 €), lengthy in time, morphologically imprecise, often inconclusive when imaging small lesions (detectability, sensitivity, and specificity); and the patient bears a non-negligible amount of radiation dose.





# I - 1. RPC-based TOF-PET



# I - 1. RPC-based TOF-PET



Electrónica de aquisição cedida pelo grupo de DAQ de HADES (GSI, Alemanha)

Electrónica de coincidências

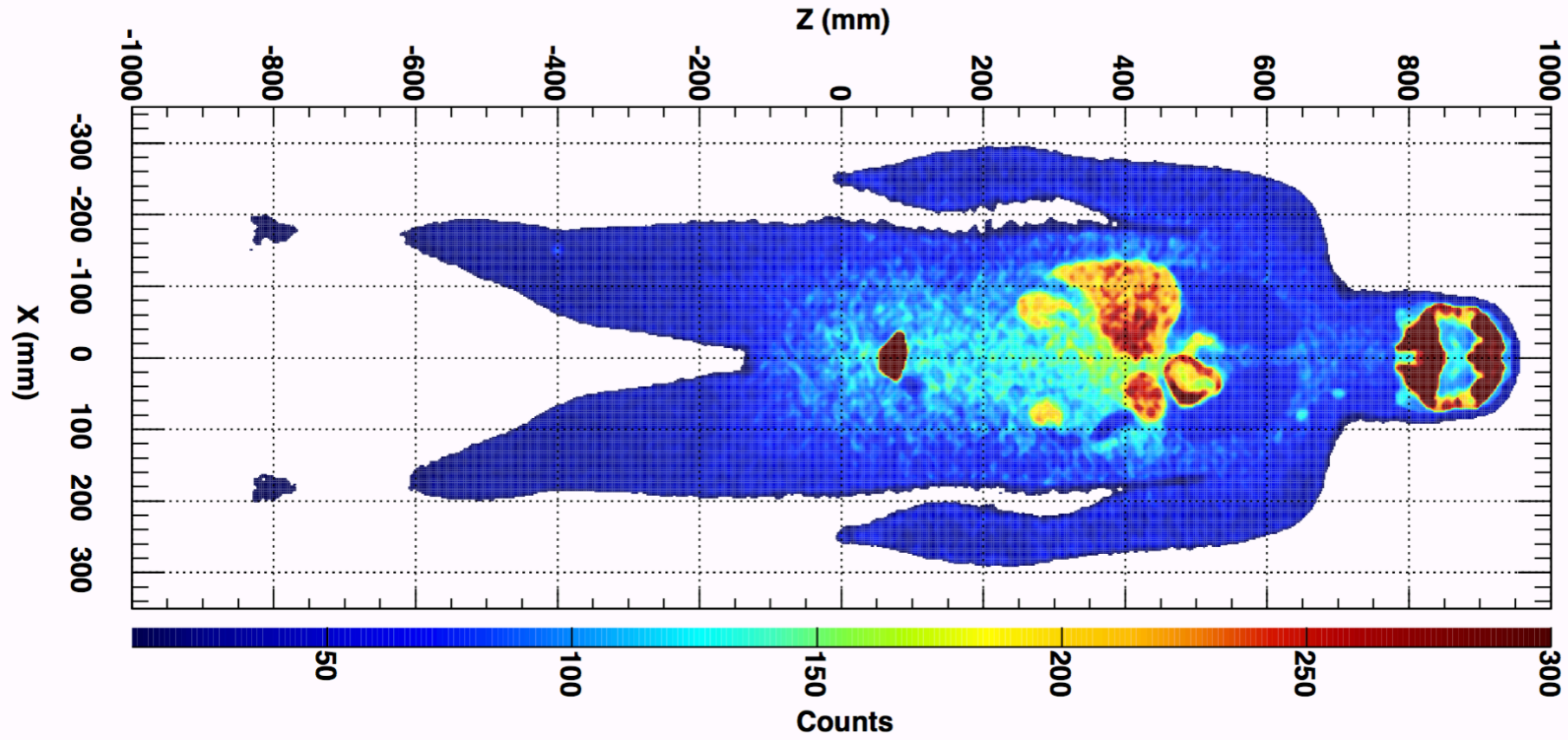
Detectores RPC-PET (uma cabeça)



# I - 1. RPC-based TOF-PET

Implementation (software):

- R&D in simulation and reconstruction

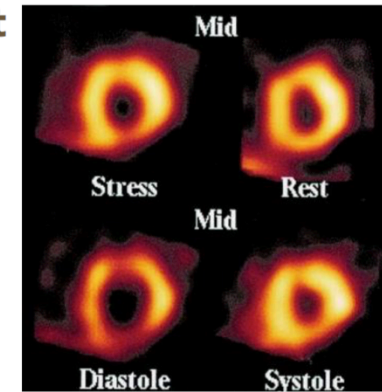


# 1 - 2. Development of New Gamma Cameras

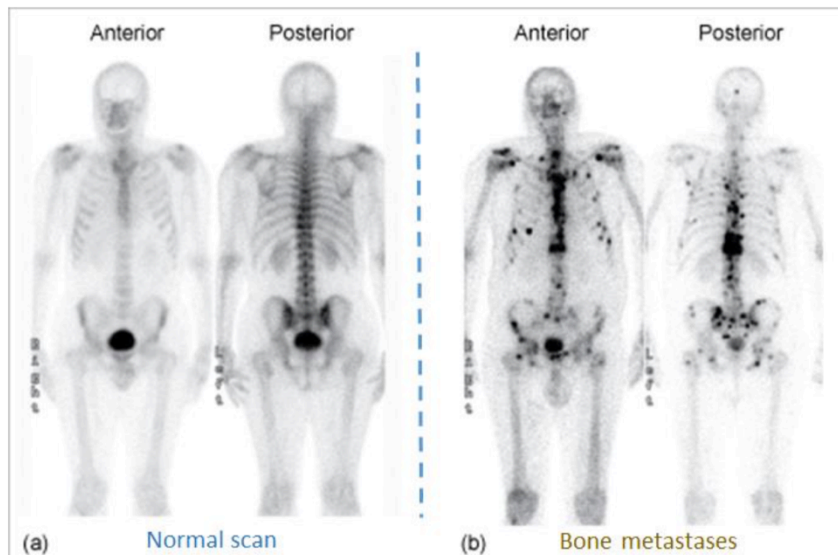
- Collaboration between Laboratório de Instrumentação e Física Experimental de Partículas, **LIP** and the University Hospital of Coimbra – **Nuclear Medicine Department**
- Gamma cameras are used to perform **scintigraphy**: a medical imaging modality used to obtain functional images. E.g. cardiology, pneumology, oncology (staging of tumors, evaluate therapeutic response)



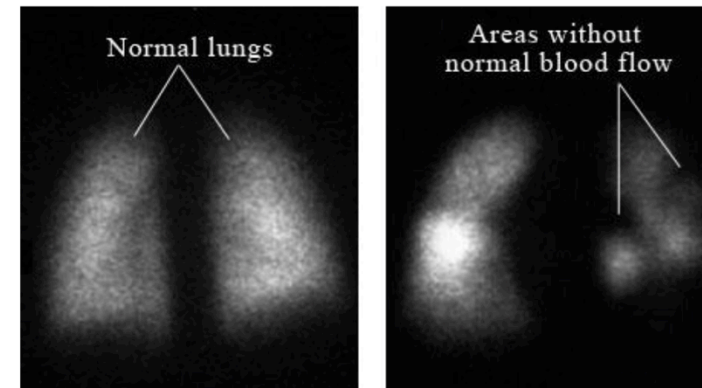
**Heart study**



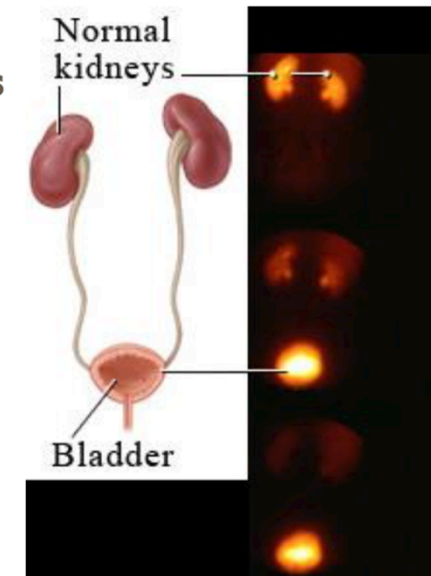
**Bone scans**



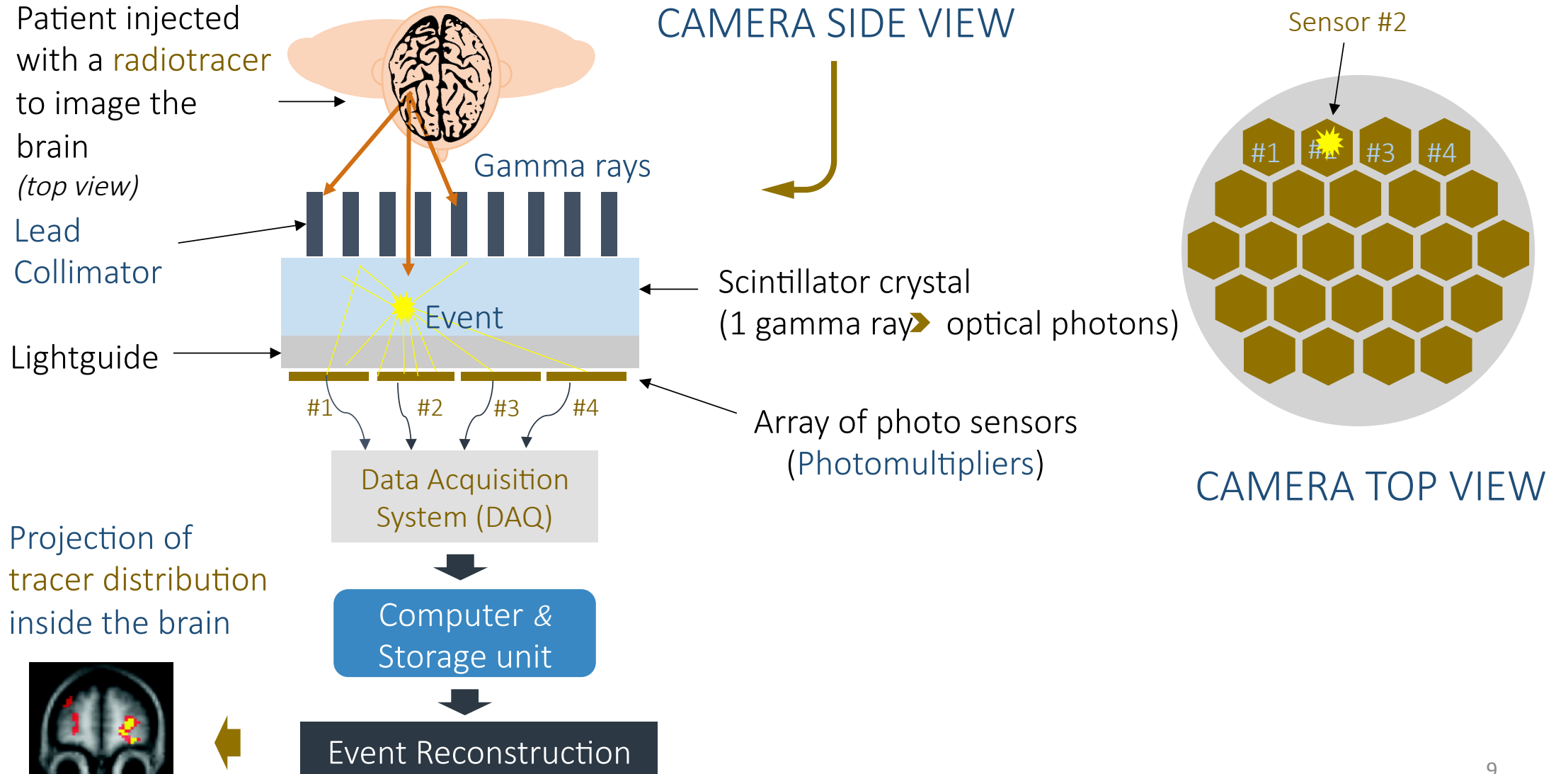
**Lung scintigraphy**



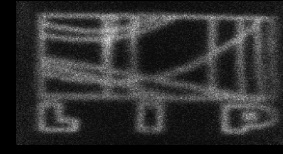
**Kidneys study**



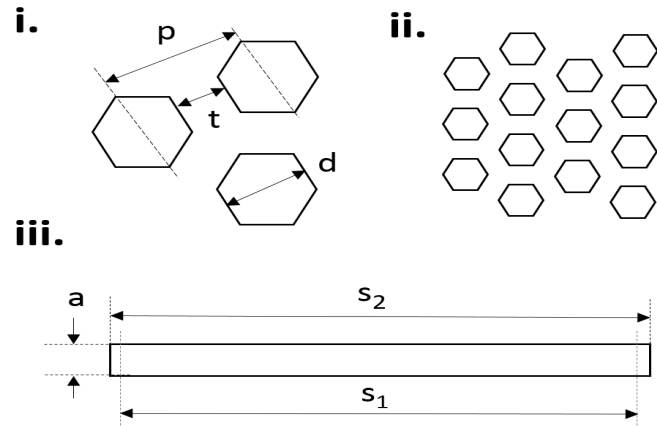
# Gamma camera working principle



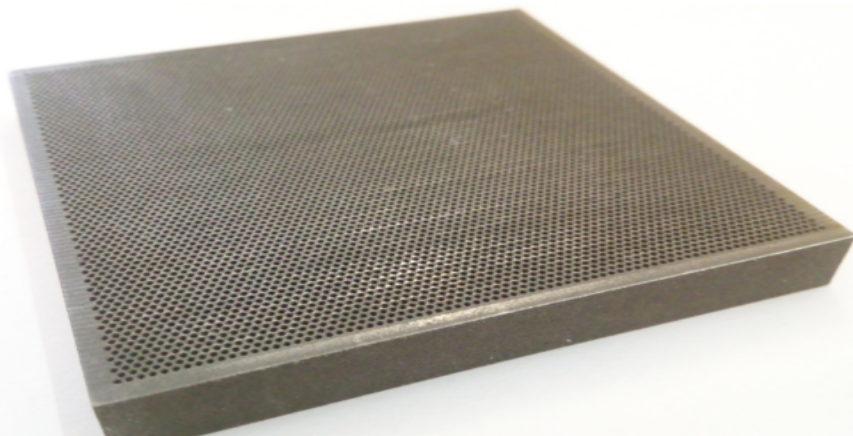
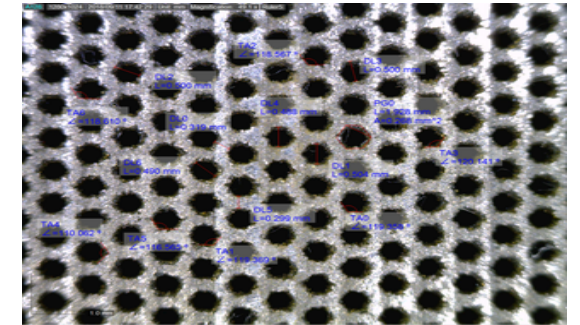
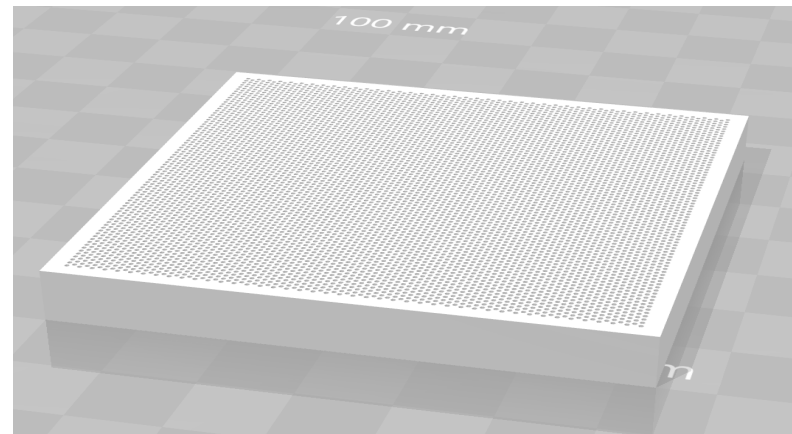




Parallel-holes collimator (hexagones 0.5 mm "diameter)

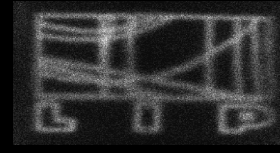


Made of tungsten using Selective laser melting



- **Specification** by João Marcos
- **Designed** by Eng. Rui Alves (LIP mechanical workshop)
- **Manufactured** by M&I Materials

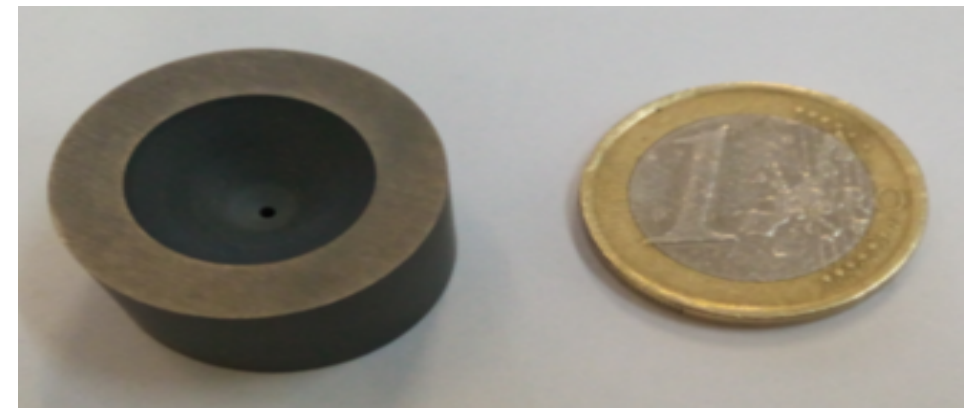
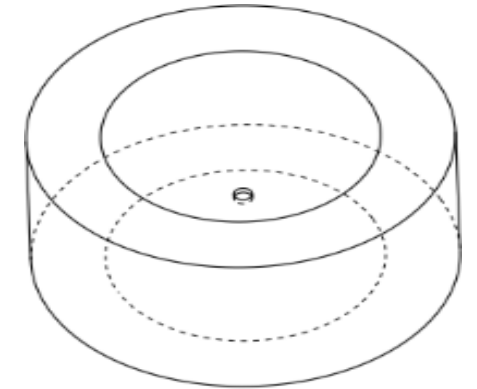
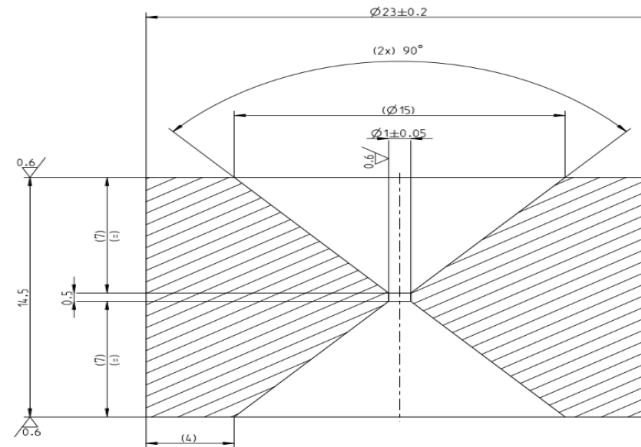
# Collimators prototypes



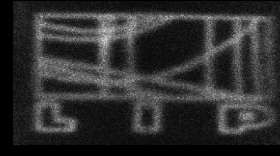
Pinhole collimator (1 mm hole, 0.5 mm channel edge height)

**Made of Tungsten alloy (95.5% W, 4.5% Co)**

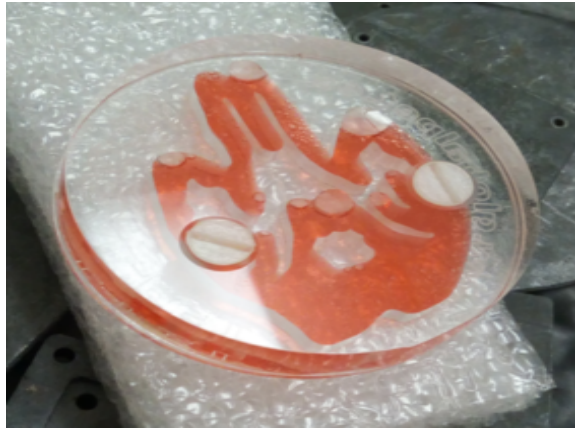
- **Specification** by João Marcos
- **Designed** by DURIT (Albergaria-a-Velha)
- **Manufactured** by DURIT



# Phantom imaging

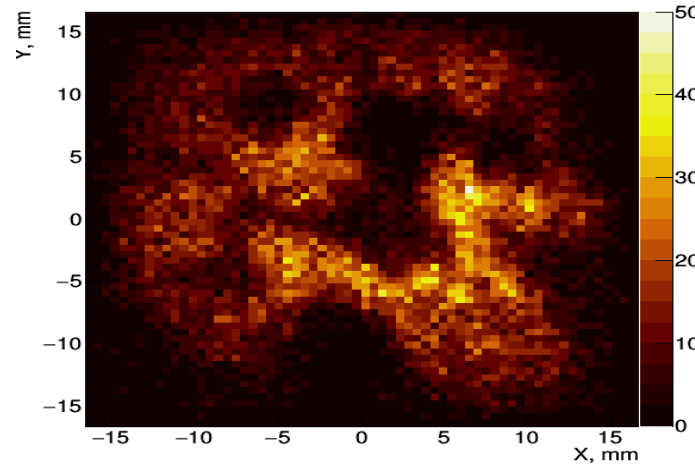


## Brain slice phantom



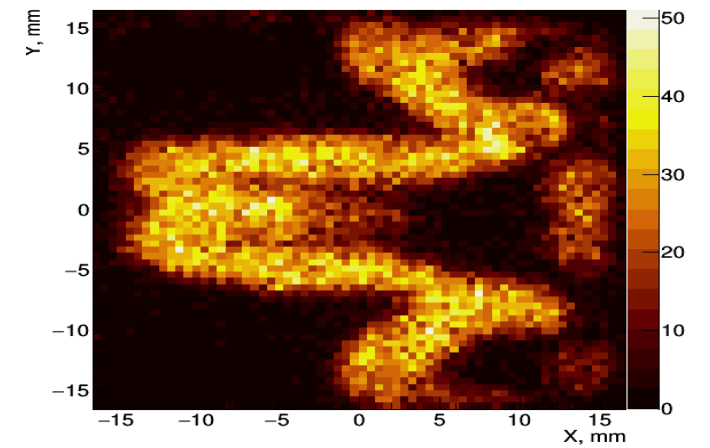
### Pinhole collimator

Event density vs XY

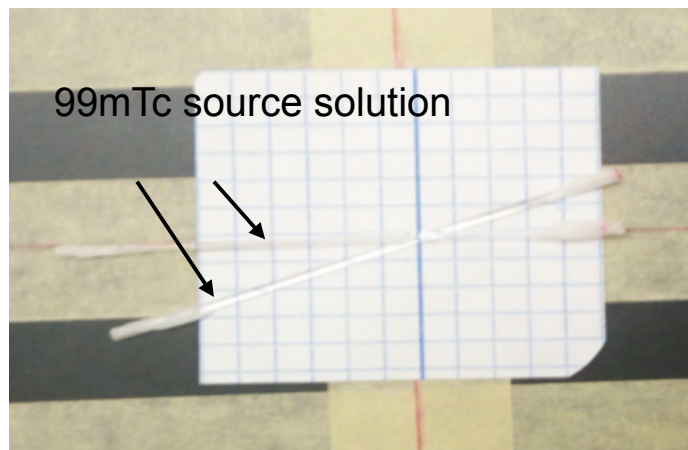


### Parallel-hole collimator

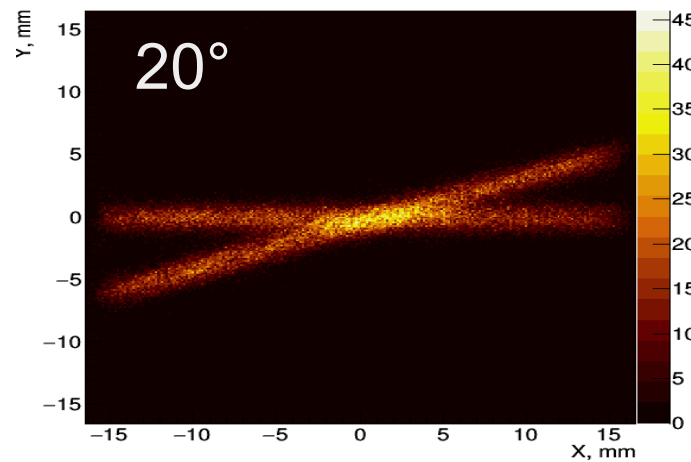
Event density vs XY



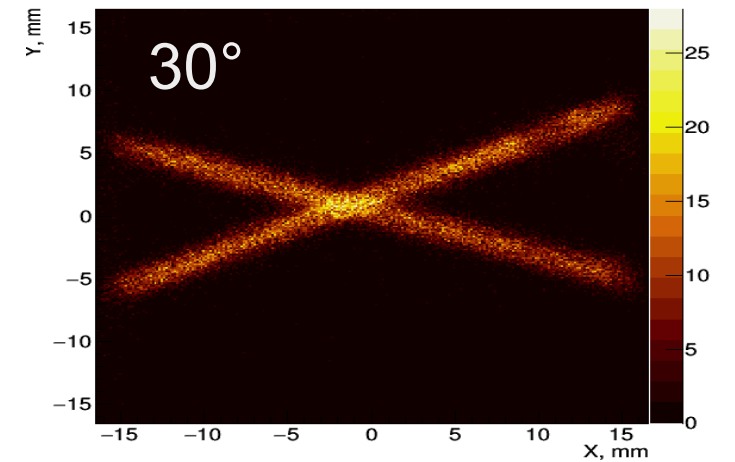
## Crossed capillary tubes phantom



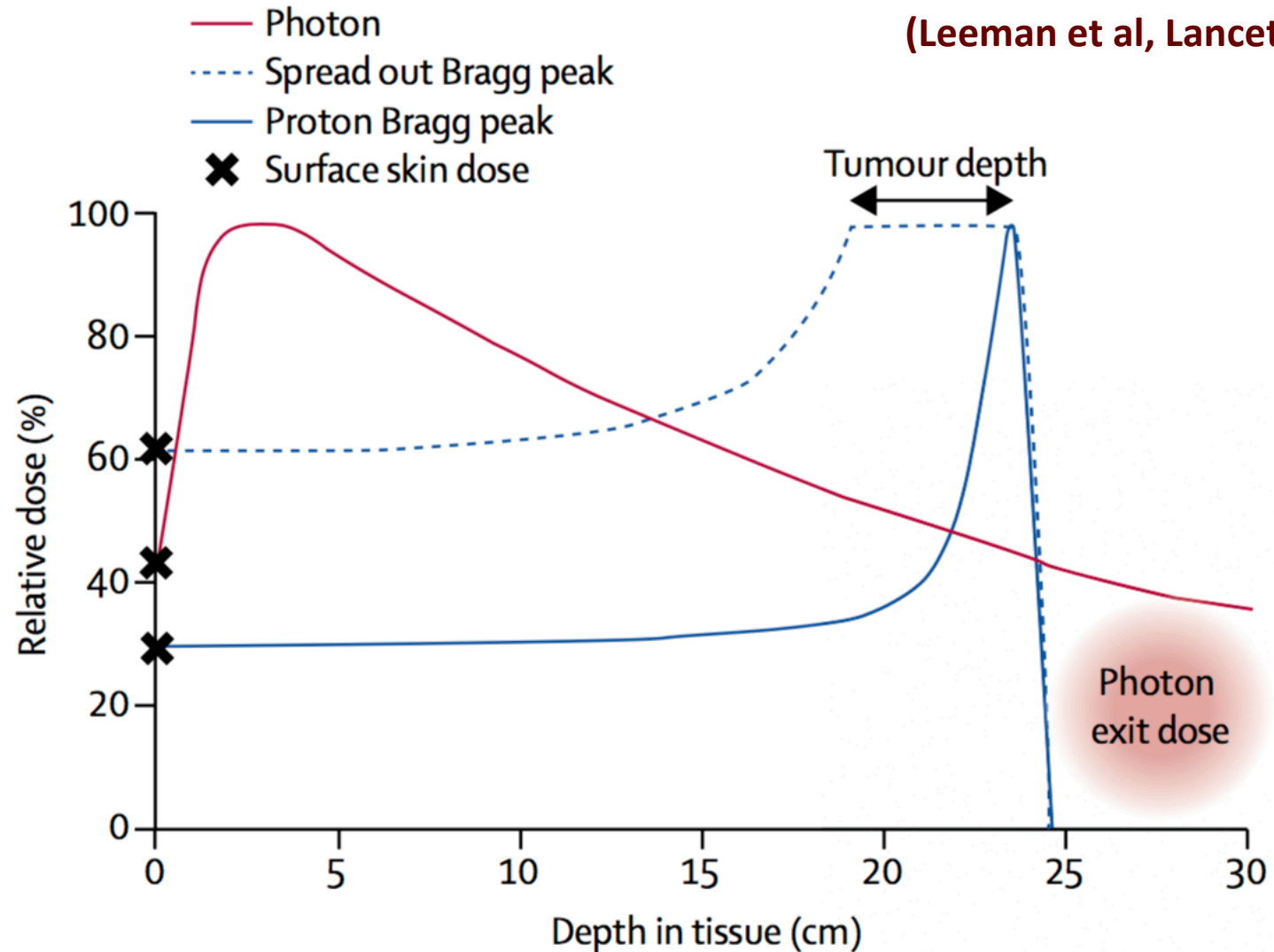
Event density vs XY



Event density vs XY

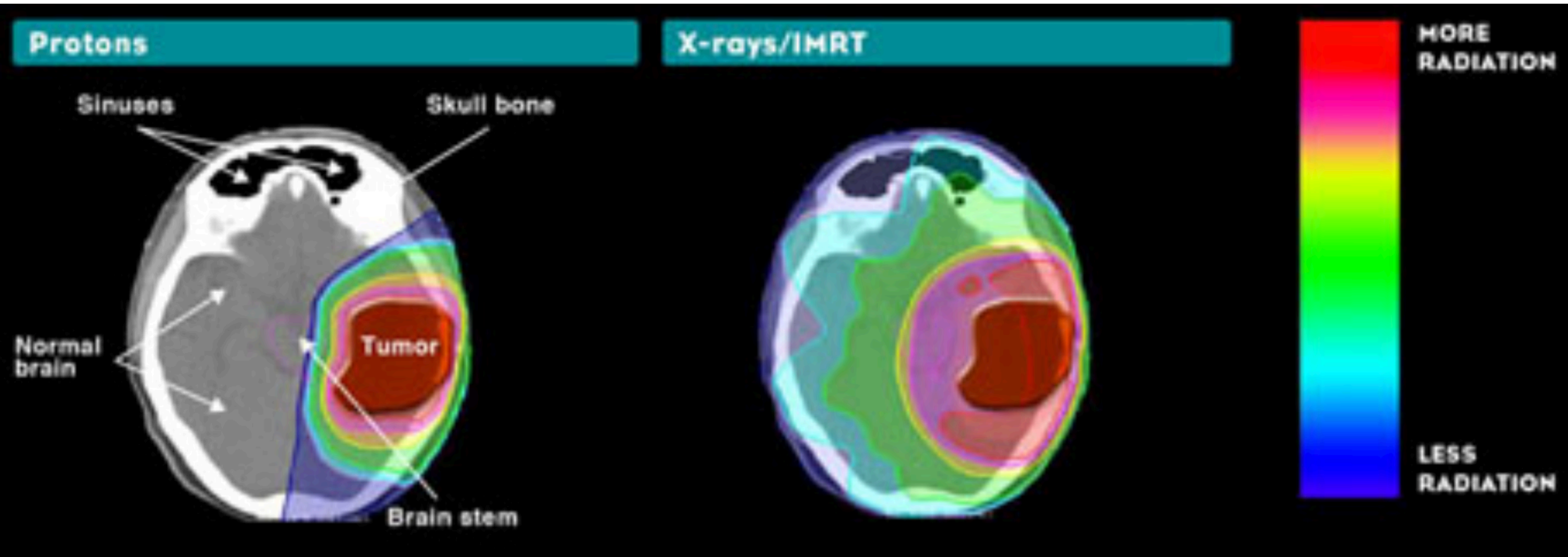


# II - 1. Motivation: Proton therapy physical advantage over photons





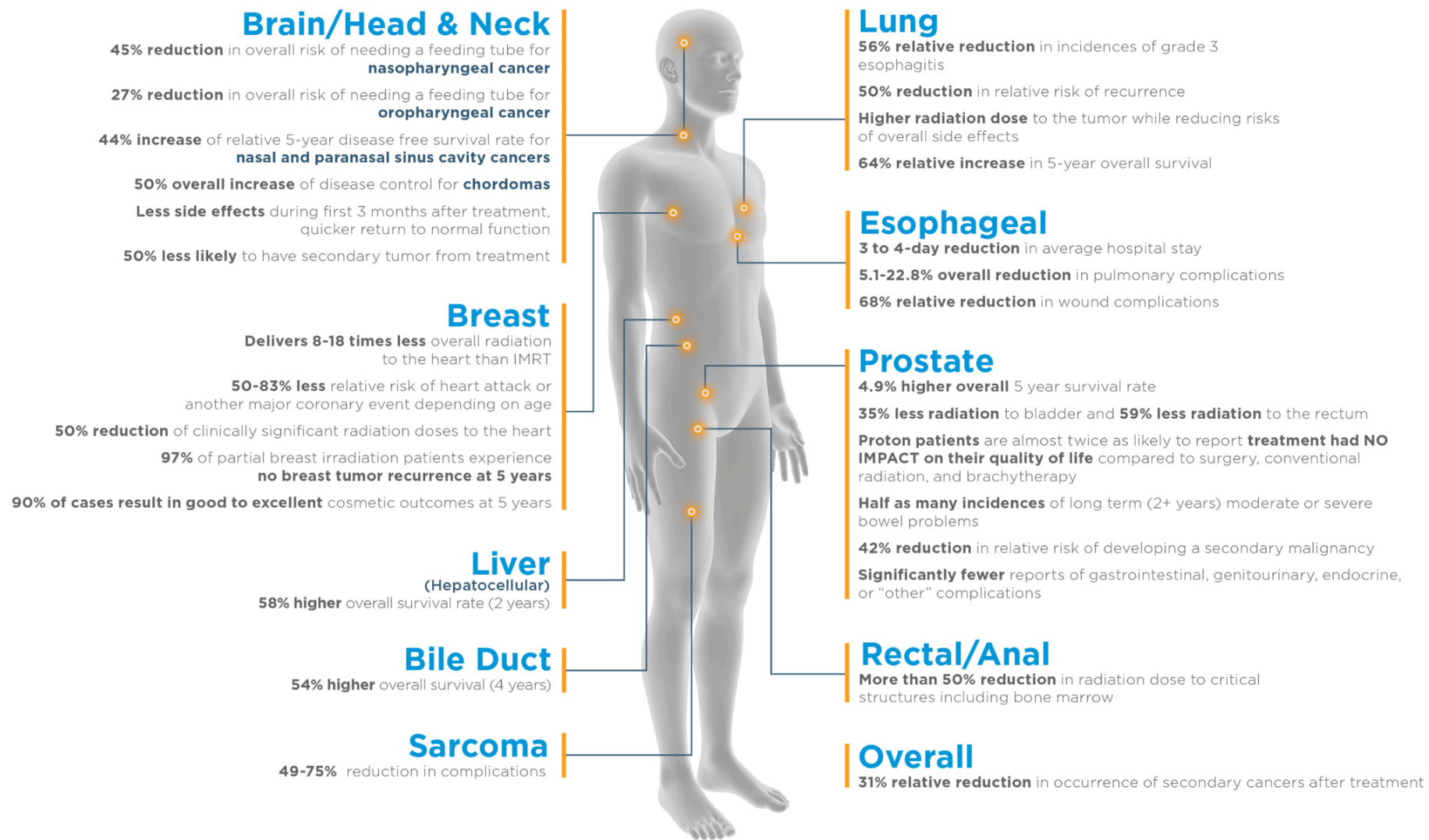
## II - 1. Motivation: Proton therapy physical advantage over IMRT



(Proton Therapy Today 2019)



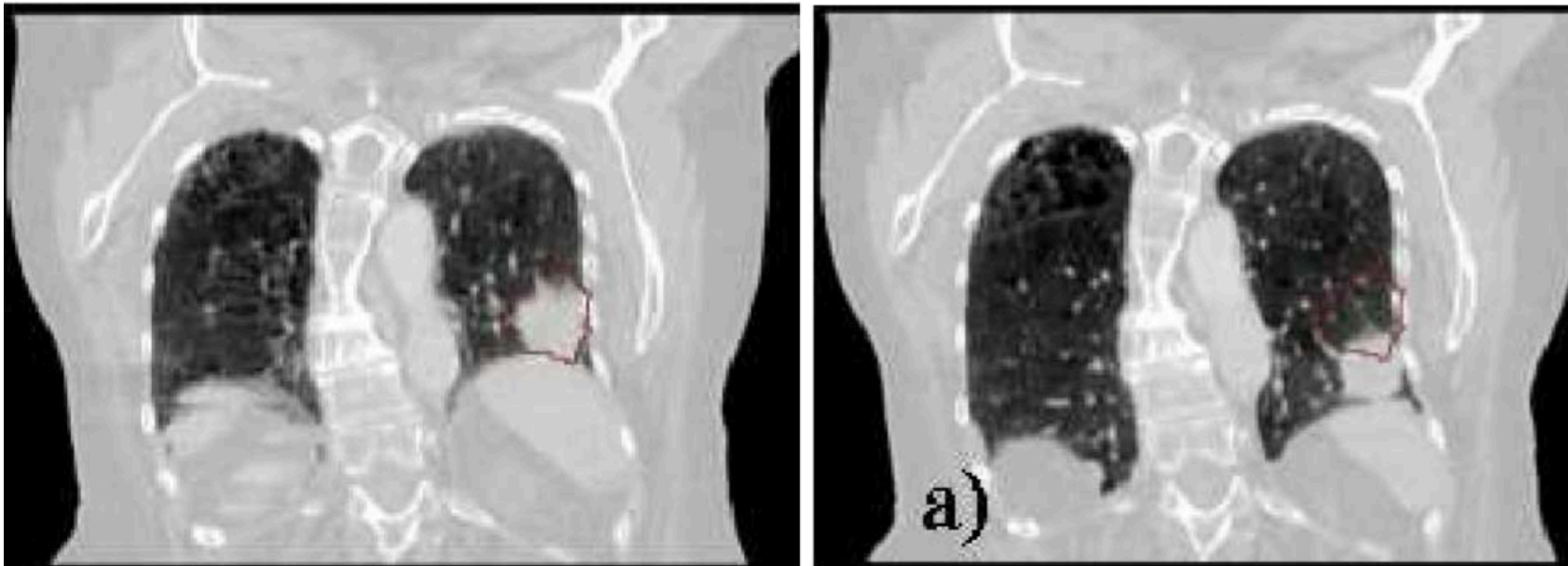
# II - 1. Motivation: Proton therapy clinical benefits



# II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: tumor displacement

- Breathing (intrafraction)

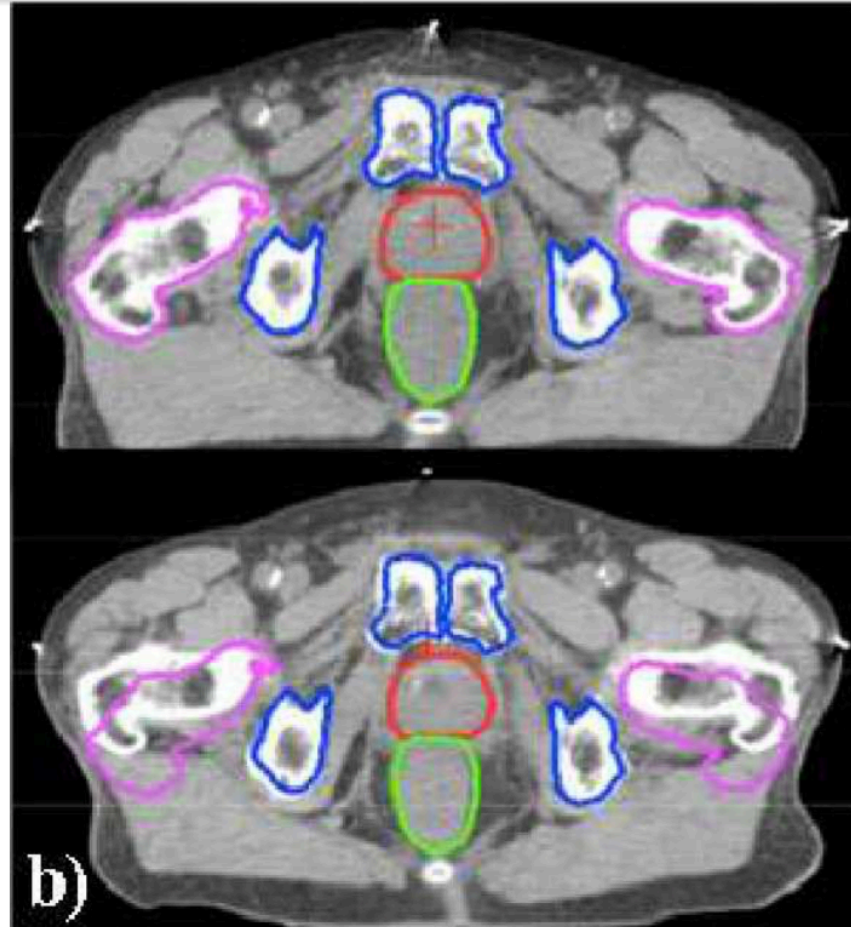


Engelsman and Bert 2011  
Lüchtenborg PhD 2012

# II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: patient displacement/deformation

- Mispositioning (interfraction)

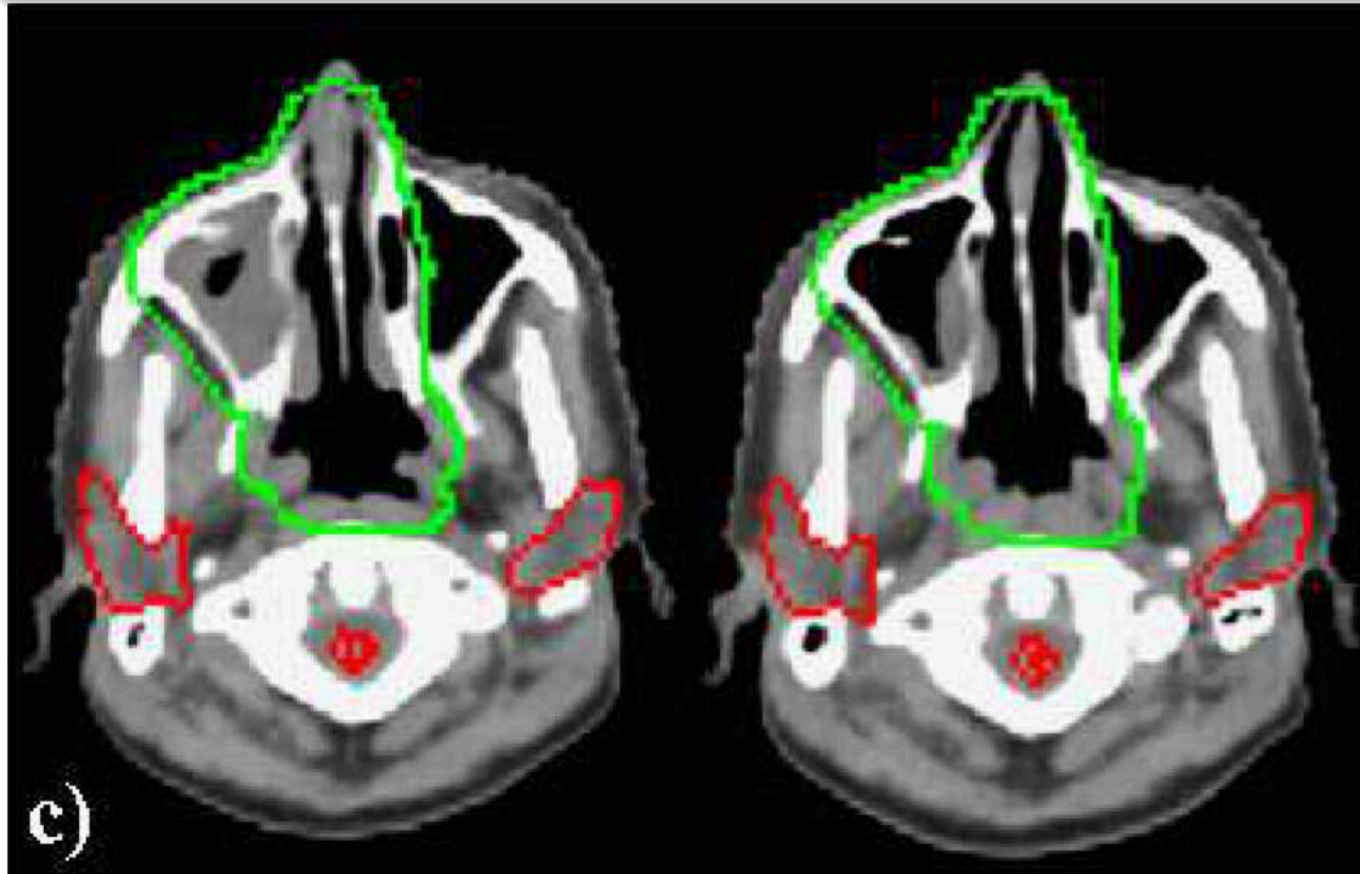


Engelsman and Bert 2011  
Lüchtenborg PhD 2012

## II - 2. Rationale for in-vivo imaging in proton RT

Target volumes and organ motion: cavity filling/wall thickening

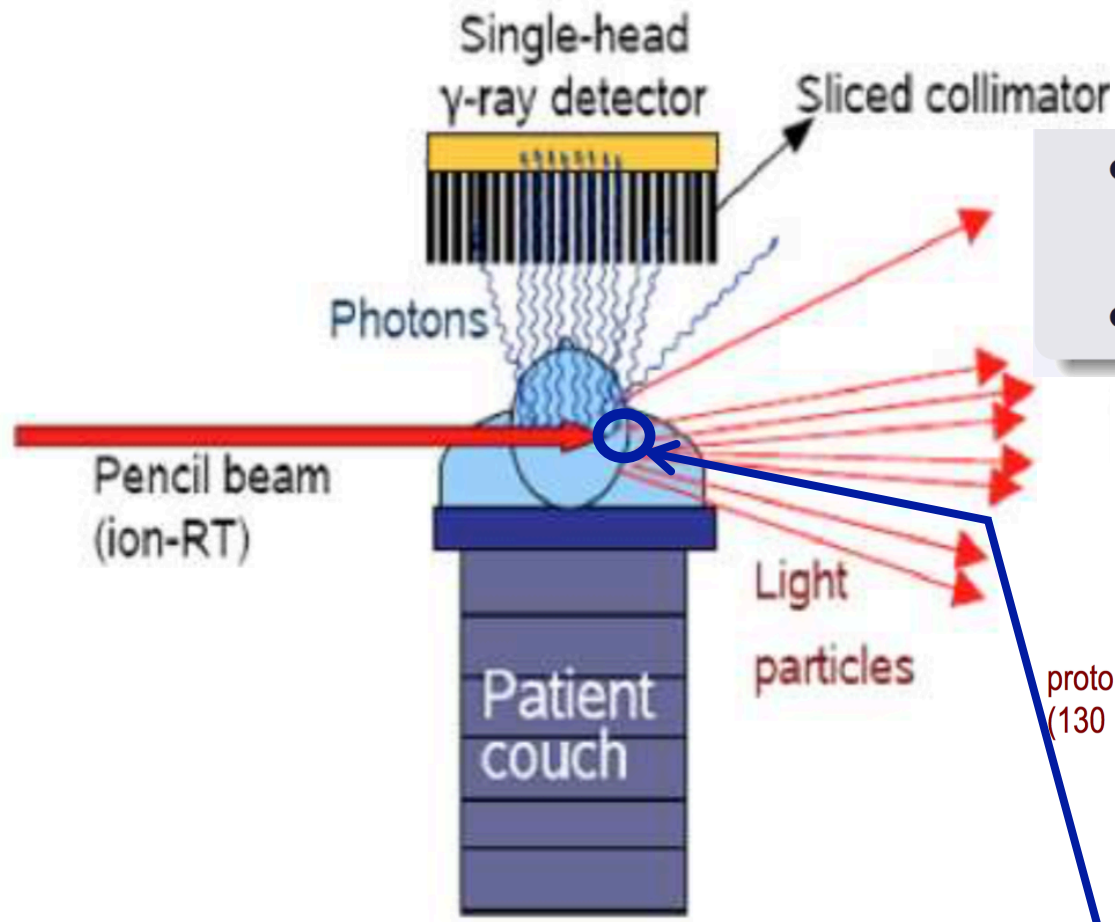
- Tissue-density modification (interfraction)



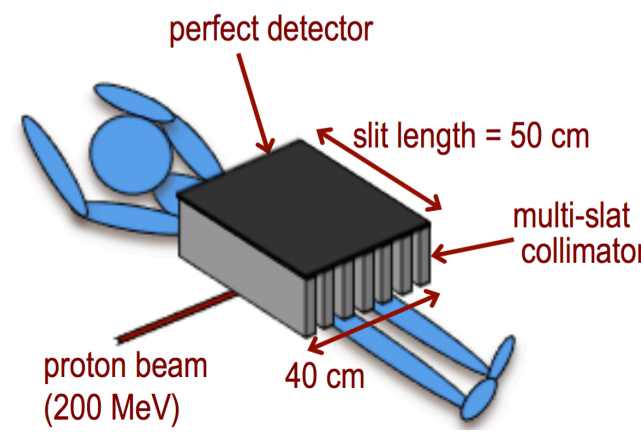
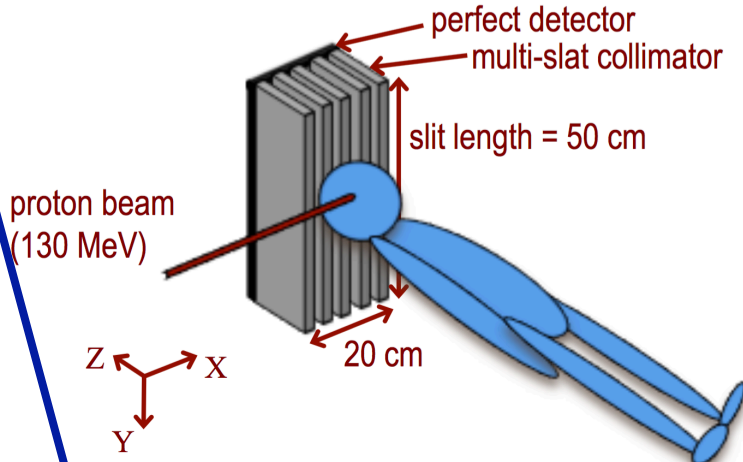
Engelsman and Bert 2011  
Lüchtenborg PhD 2012



# II - 3. The multi-slat concept for prompt-gamma imaging in proton RT



- Head irradiation: nasal cavities (cavity filling) and pituitary (change in brain density)
- Pelvic irradiation: prostate (patient mispositioning)



(Cambraila Lopes PhD 2017)

Provides real-time images of selected region without rotation of beam source.

Image with prompt gammas “stops” at beam range



# II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

## 3.1 Filling of nasal cavity

### Head irradiation (*NCAT*)

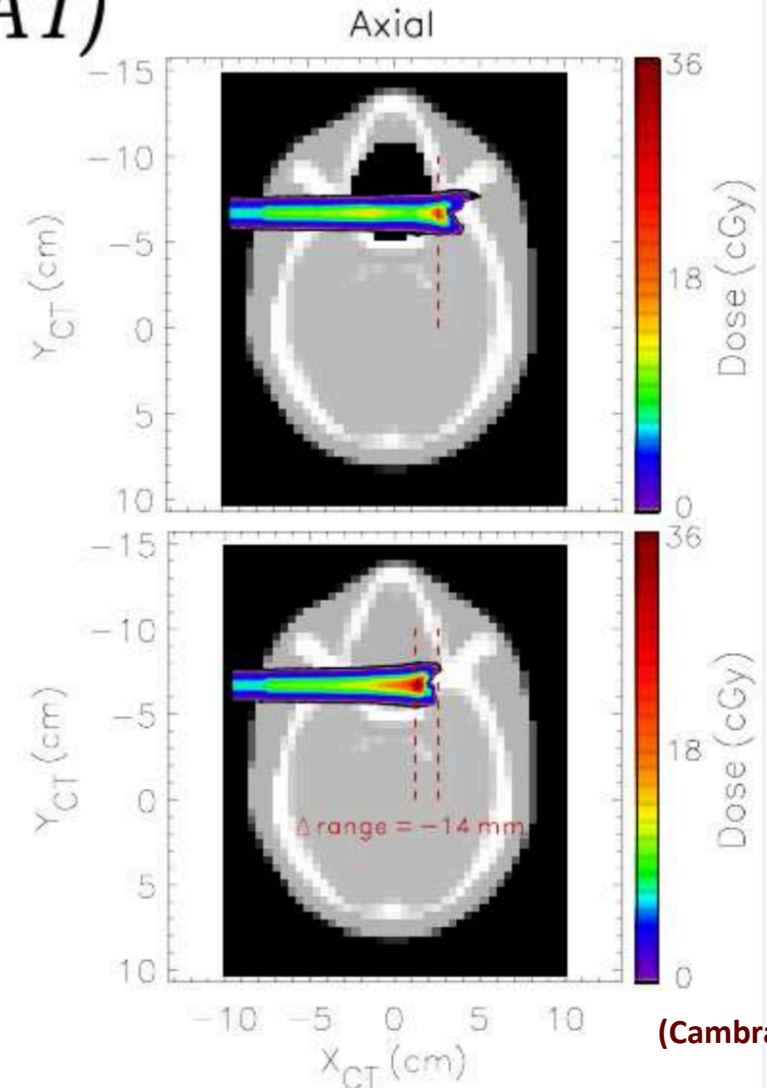
#### ① Sphenoid region

##### ❖ Treatment plan:

- Irradiation of a hypothetical tumor located in the sphenoid bone region
- **Empty nasal cavity** (air-filled)

##### ❖ Compromised treatment:

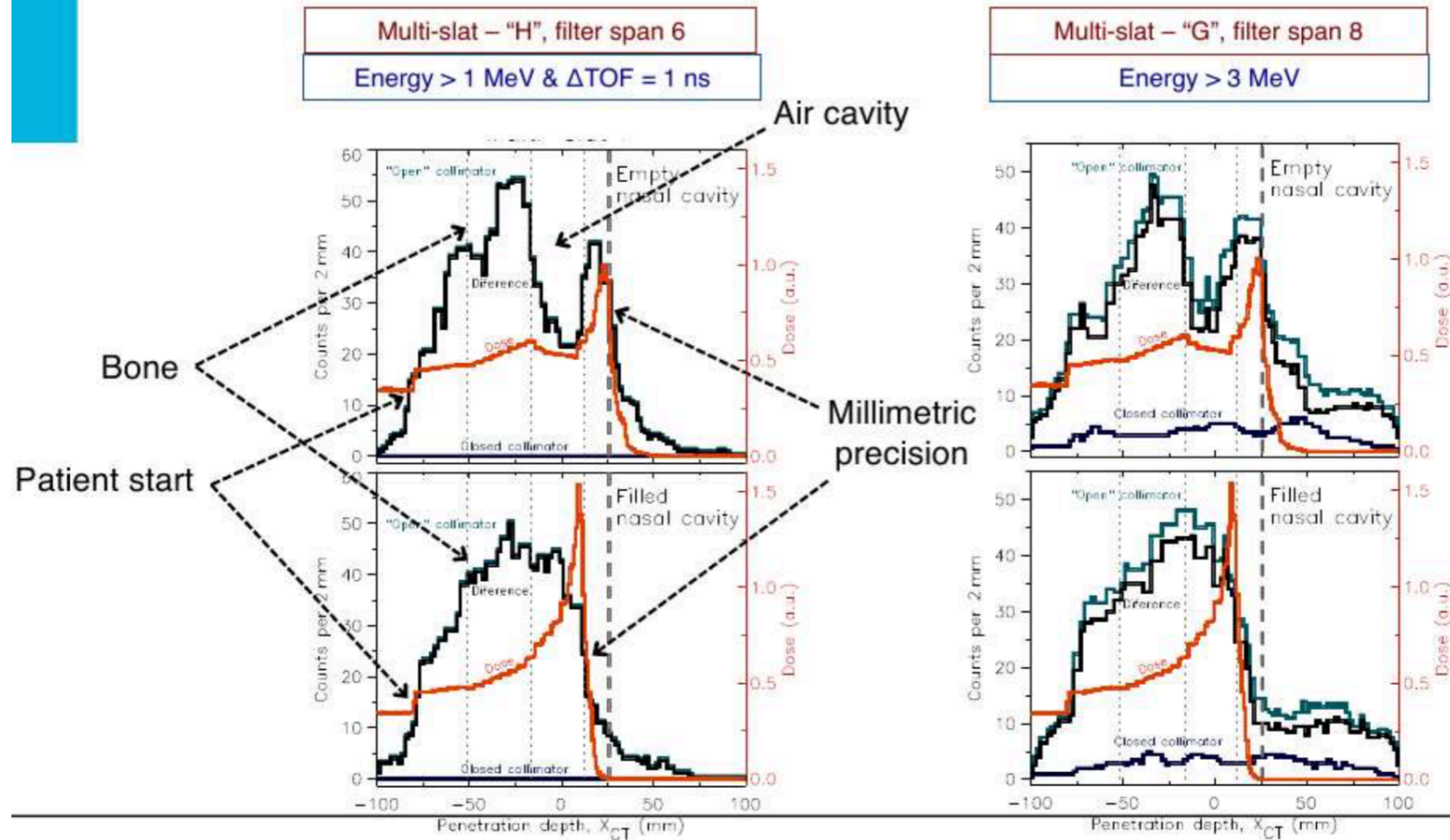
- **Filled nasal cavity** with PMMA-like material
- Under-range shift of 14 mm
- Possible causes:
  - Patient cold → presence of mucus
  - Response after irradiation → edema, tissue swelling
  - Tumor growth



# II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

## 3.1 Filling of nasal cavity

### ① Sphenoid region Collimated PG profiles

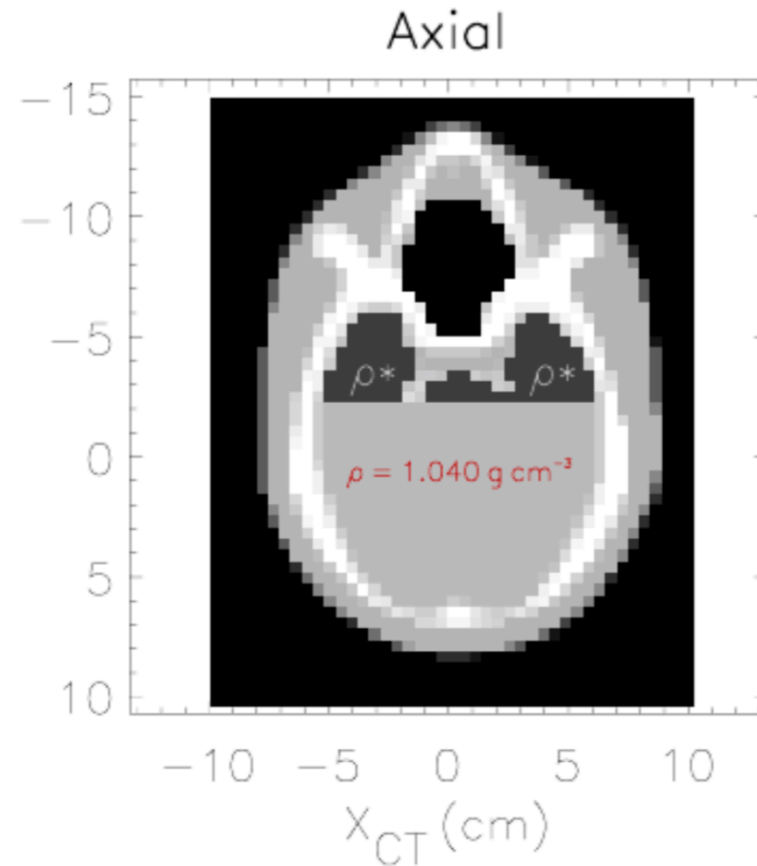


(Cabraia Lopes PhD 2017)

## II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

### 3.2 Change of brain density due to fractionated RT

- Conjecture: brain tissue hypo/hyperdense due to fractionated RT **Denham et al Radiother Oncol 2002**

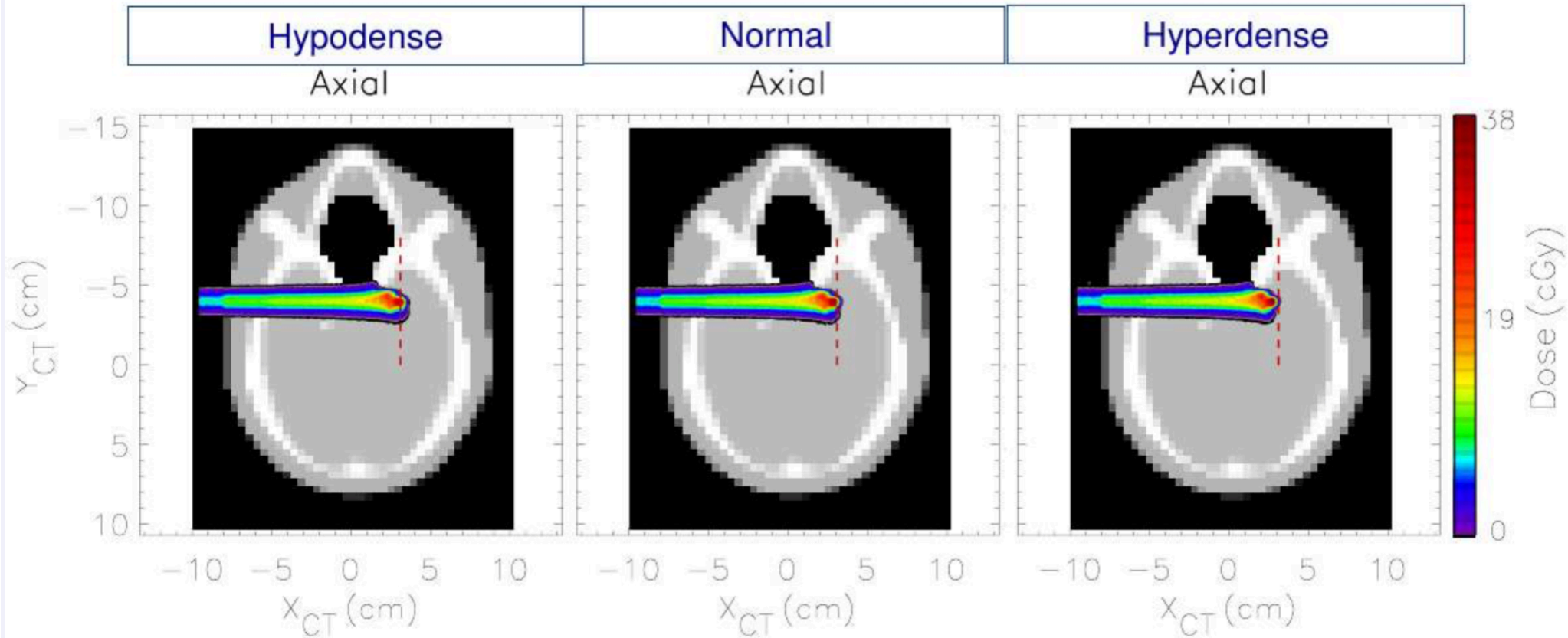


(Cabraia Lopes PhD 2017)

## II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

### 3.2 Change of brain density due to fractionated RT

- **Conjecture: brain tissue hypo/hyperdense**
- **Corresponding dose distributions (protons):**

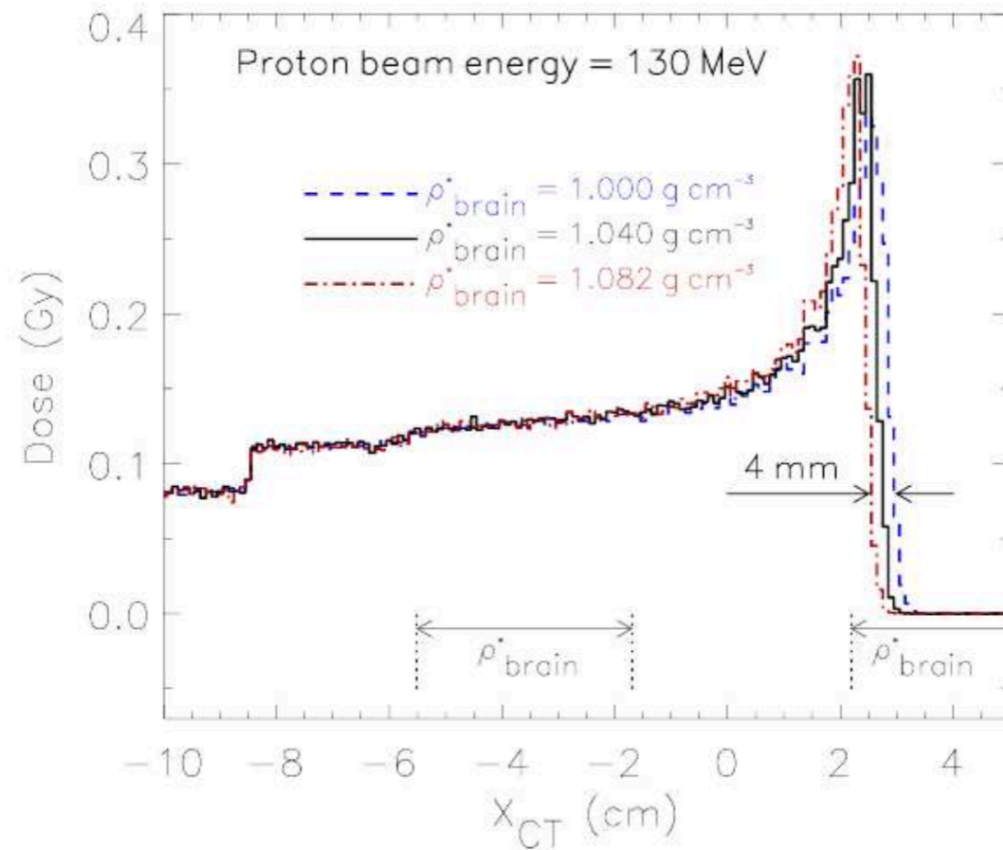


(Cambralia Lopes PhD 2017)

# II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

## 3.2 Change of brain density due to fractionated RT

- Conjecture: brain tissue hypo/hyperdense
- Corresponding dose profiles (protons):



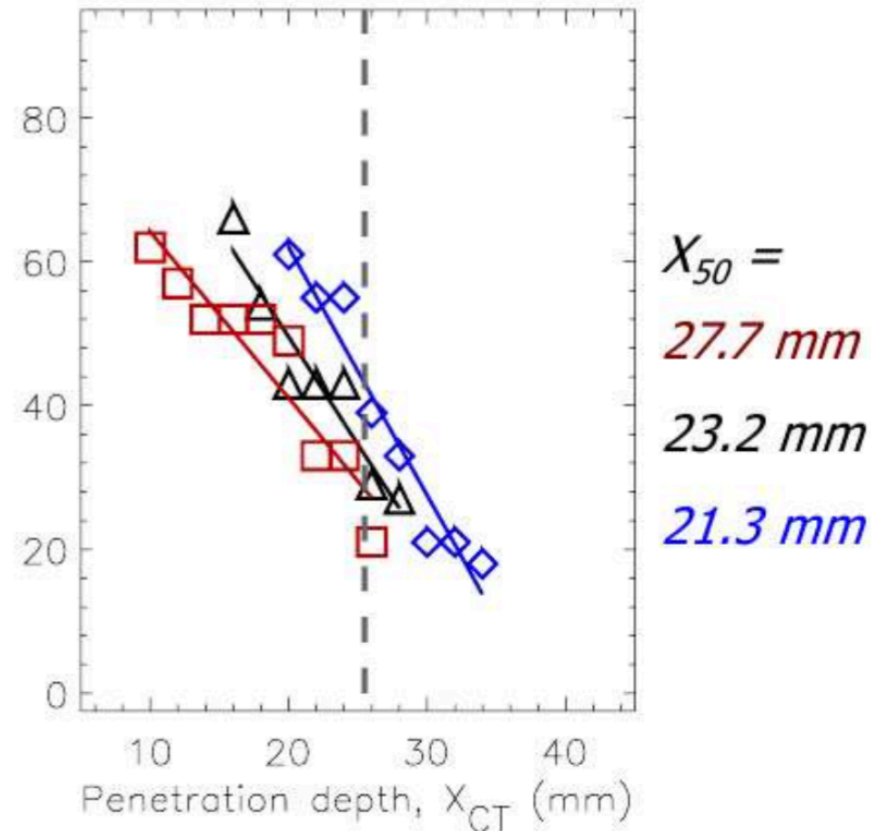
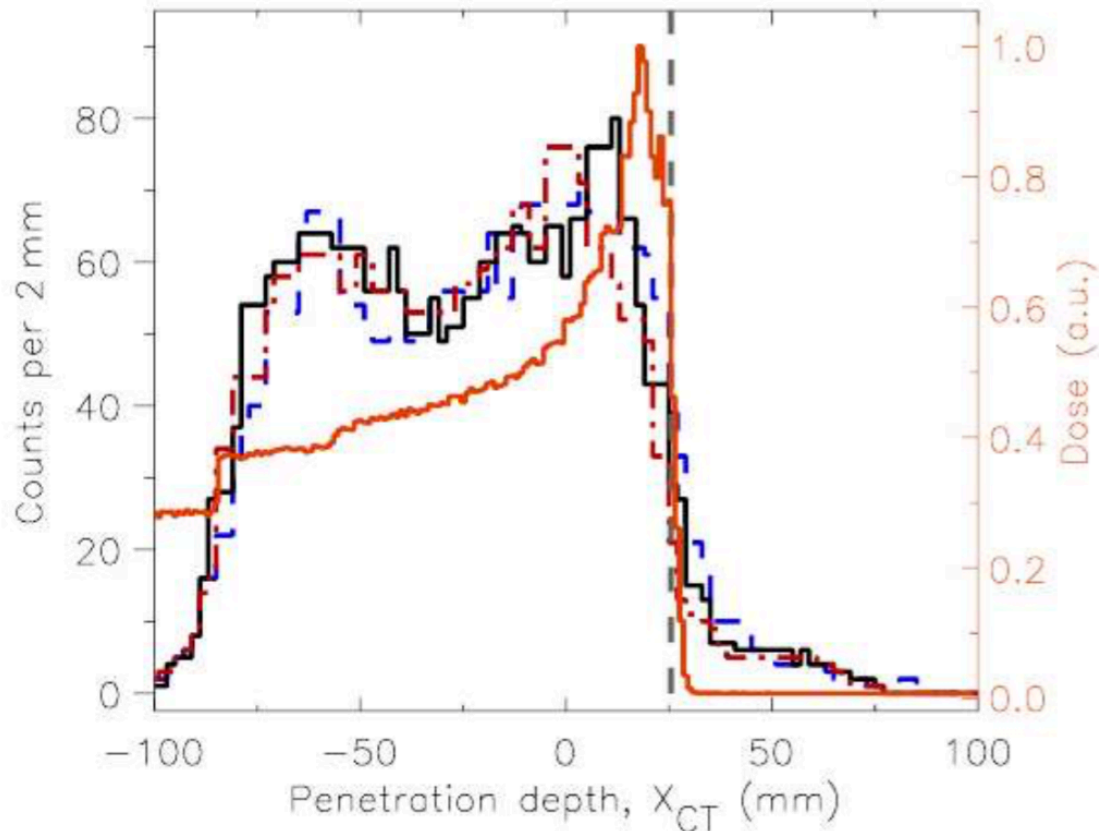
(Cabraia Lopes PhD 2017)



## II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

### 3.2 Change of brain density due to fractionated RT

- Conjecture: brain tissue hypo/hyperdense
- Monte Carlo results with proposed detector (Geant4):



# II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

## 3.3 Prostate: patient mispositioning Pelvis irradiation (*NCAT*)

### Prostate

#### ❖ Treatment plan:

- Irradiation of a hypothetical tumor in the prostate

#### ❖ Compromised treatment:

##### ○ Misalignment

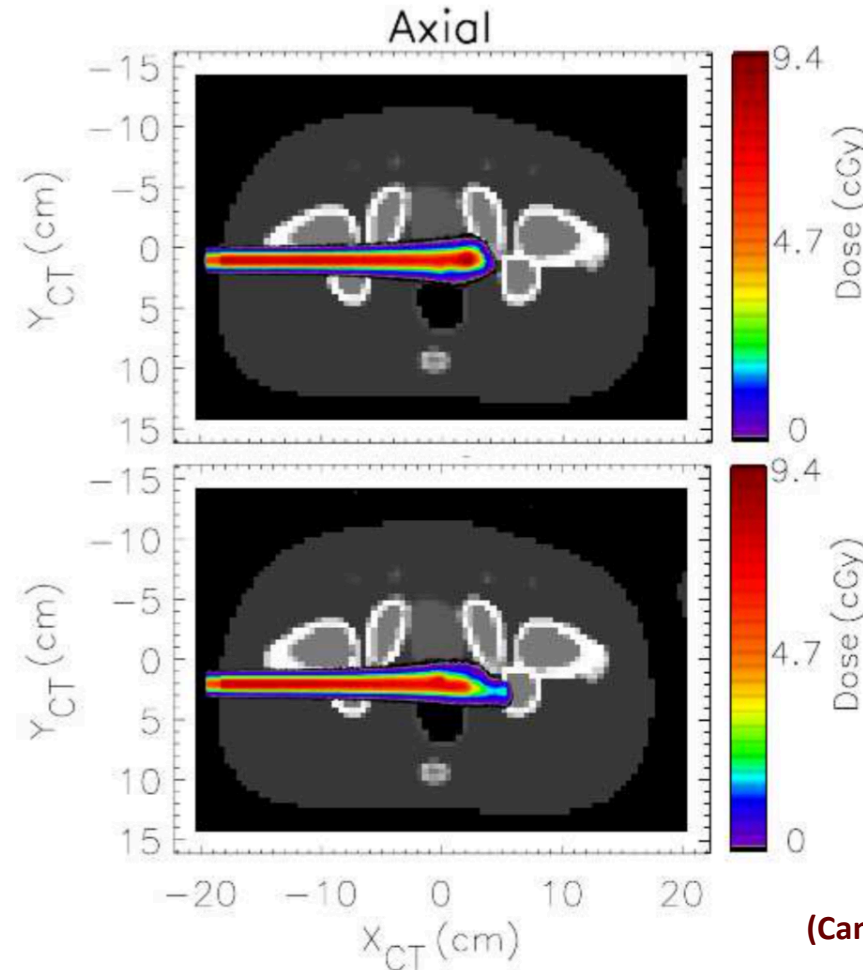
→ Patient 1 cm to ventral

- Dose proximal displacement

→ tumor underdosage

- Possible causes:

- Mispositioning
- Patient weight change



(Cabraia Lopes PhD 2017)

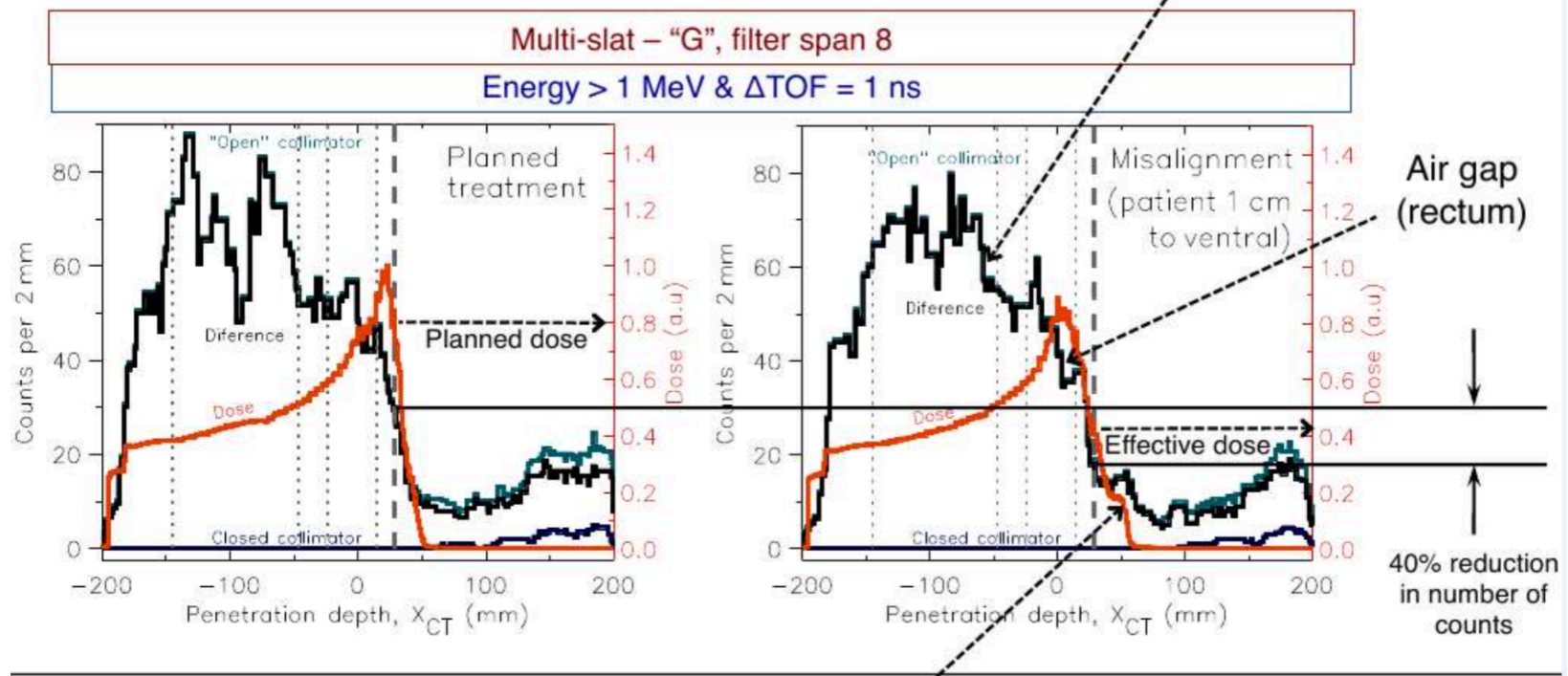
# II - 3. The multi-slat concept for prompt-gamma imaging in proton RT

## 3.3 Prostate: patient mispositioning

### ③ Prostate

#### Collimated PG profiles

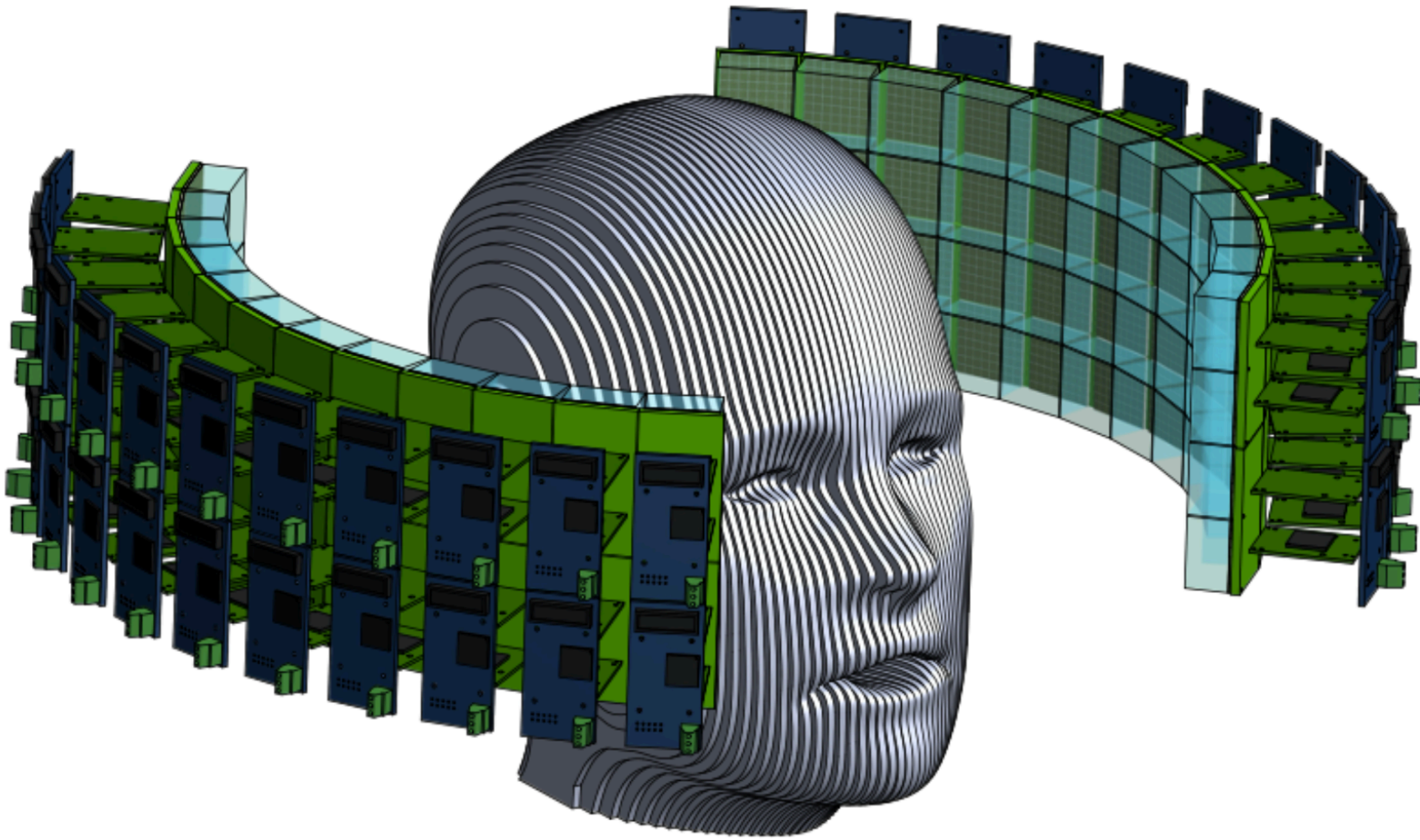
- Dose reduction of ~ 46% detected
- Correlation with anatomic features



Excess dose corroborated by PG profile (Cabraia Lopes PhD 2017)

# II - 4. In-beam time-of-flight PET for proton RT

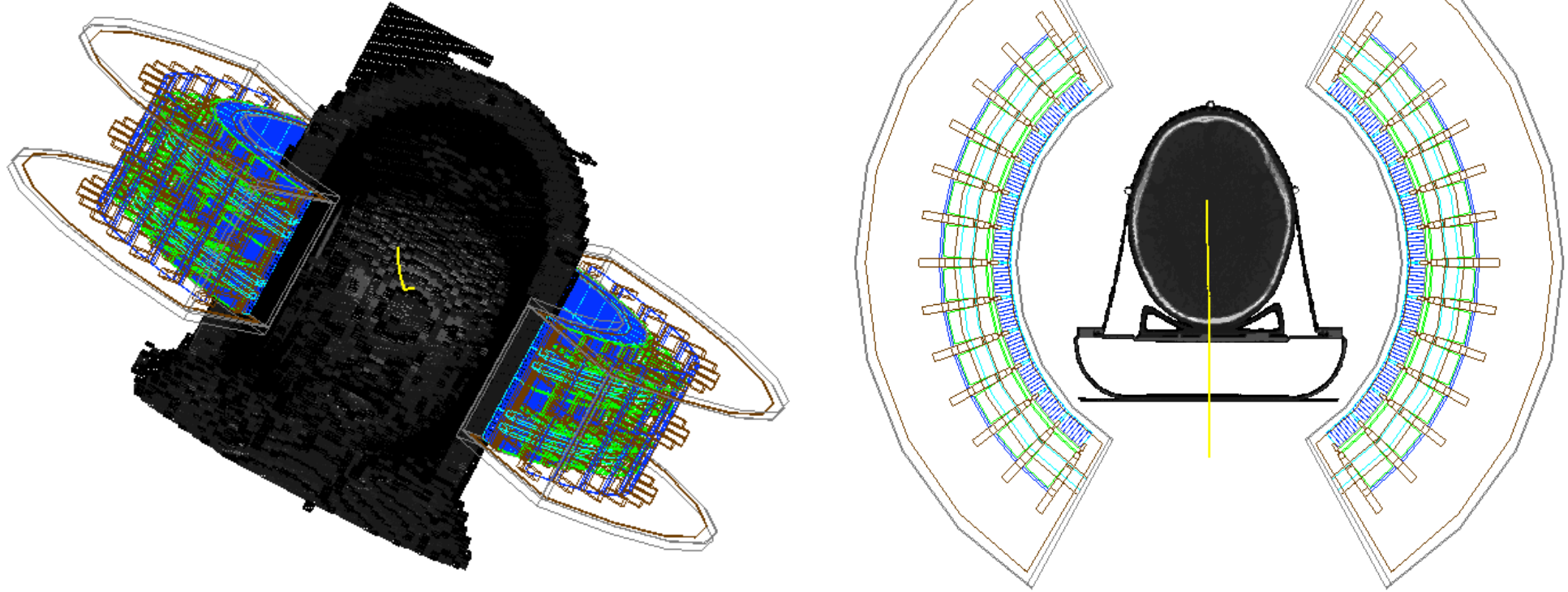
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# II - 4. In-beam time-of-flight PET for proton RT

A full simulation with an arbitrary single beamlet

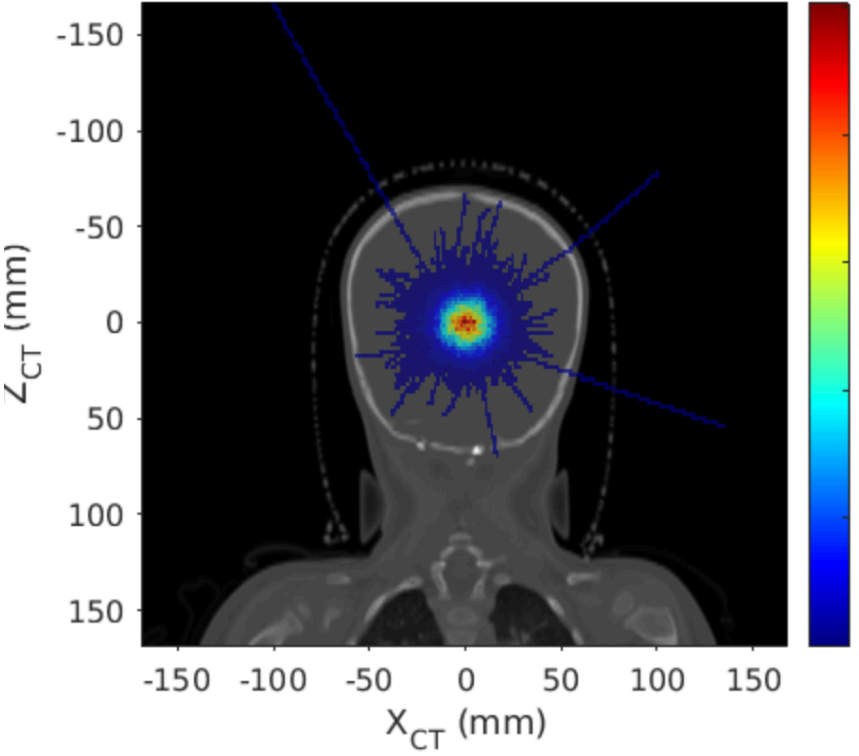


Starting position: (0, -155, 0)  
Direction: Y (gantry angle of 180 degrees)  
Energy: 131 MeV  
Beamlet spread size: 8.42 mm sigma  
Beamlet duration: 4 ms

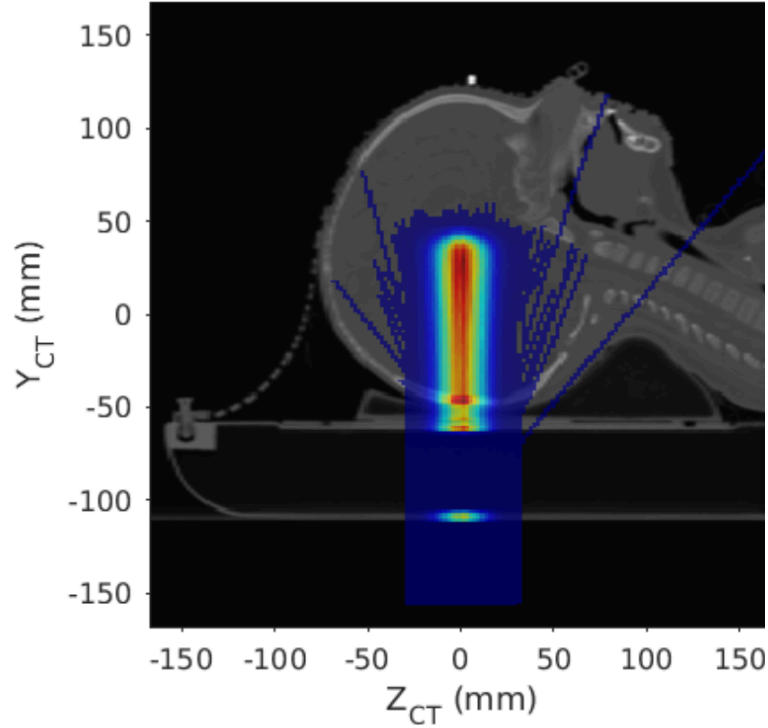


# II - 4. In-beam time-of-flight PET for proton RT

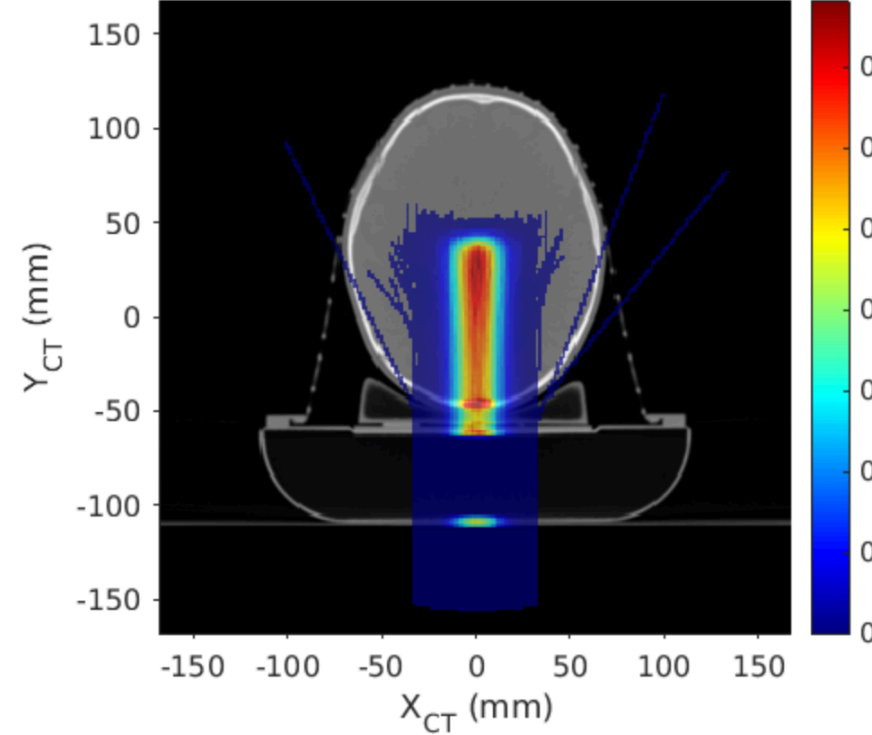
**Coronal projection**



**Sagittal projection**



**Axial projection**



# Thank you for your attention

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- The authors acknowledge the informatics support from the staff of the high-performance computing clusters of the University of Coimbra and Delft University of Technology (thousands of hours of parallel computation).
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Fundos Europeus  
Estruturais e de Investimento