

Extracting myelin and iron maps of the brain using biophysical modelling - some of the many roles of an MRI physicist

José P. Marques



• U  C •

 **1995-99**
undergrad studies

 **IBEB**
Instituto de Biofísica e Engenharia Biomédica

 **2000-01**
doctoral program

FACULDADE DE CIÊNCIAS
UNIVERSIDADE DE LISBOA

coimbra —
lisboa —





Sir Peter Mansfield Magnetic Resonance Centre
the home of epi and slice selection



2001-04
PhD

- Long Range Dipolar Fields
- ΔB_0 due to air tissue interfaces
- GE & SE BOLD sim.





• U  C •

FMUC
IBILI
INSTITUTE OF BIOMEDICAL
RESEARCH IN LIGHT
AND IMAGE

2005-06
postdoc

EEG-fMRI in epilepsy:
ICA-based construction of
the fMRI regressor

coimbra —






ÉCOLE POLYTECHNIQUE
FÉDÉRALE DE LAUSANNE


UNIL | Université de Lausanne

2007-14
Postdoc, MA
senior scientist

Quantitative MRI

Fast Imaging

Motion correction

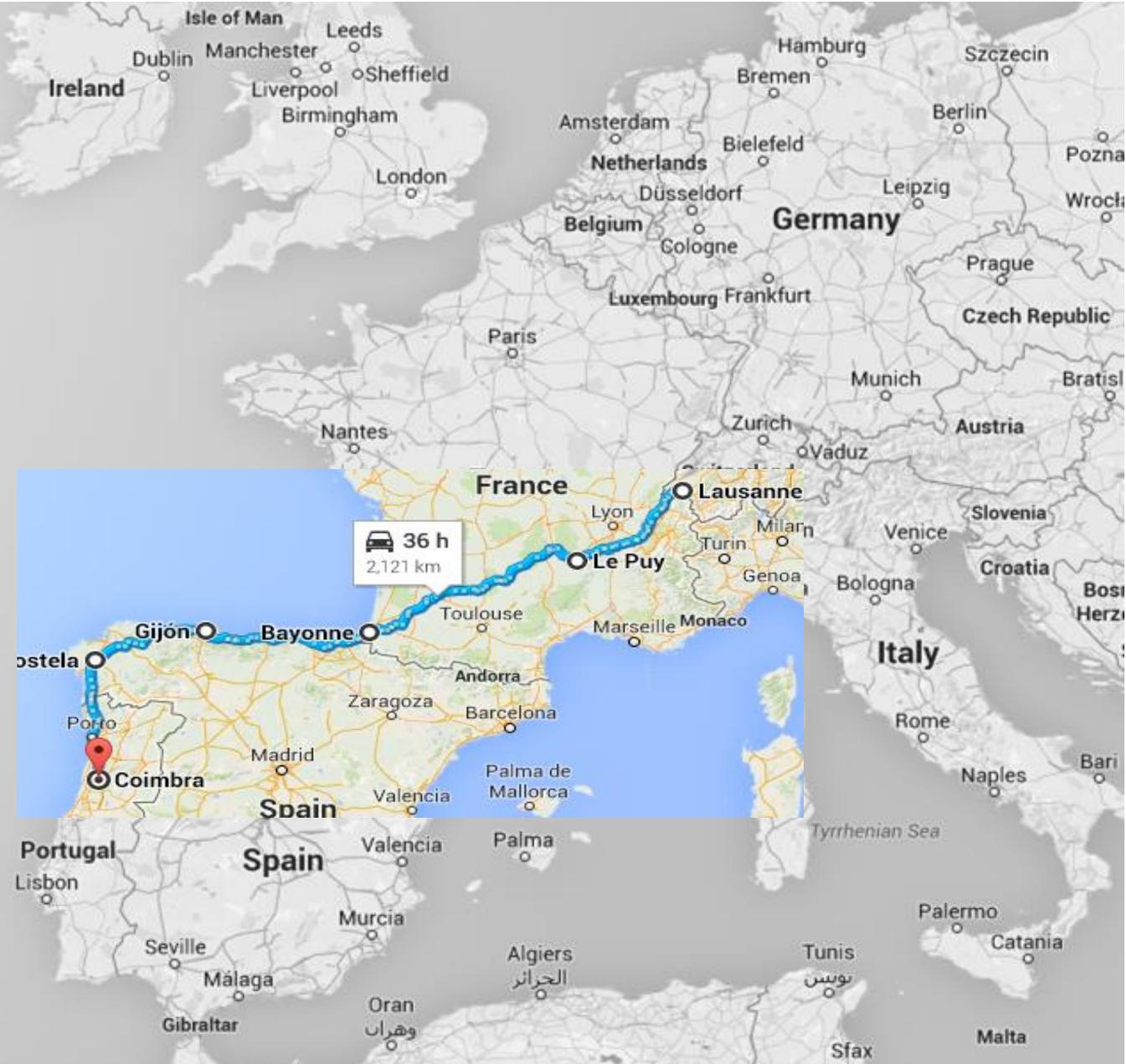





ÉCOLE POLYTECHNIQUE
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UNIL | Université de Lausanne

2007-14
Postdoc, MA
senior scientist





Radboud University



2015- Senior scientist
Associate PI

Quantitative MRI

Myelin Imaging

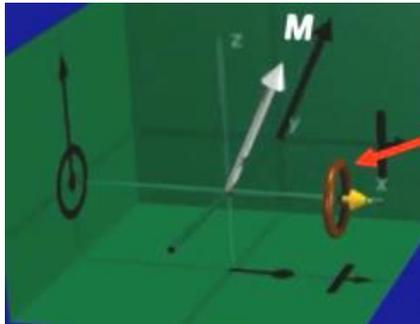
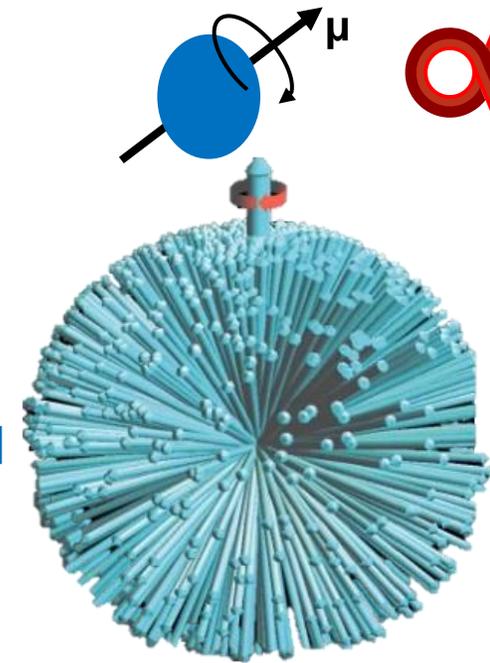
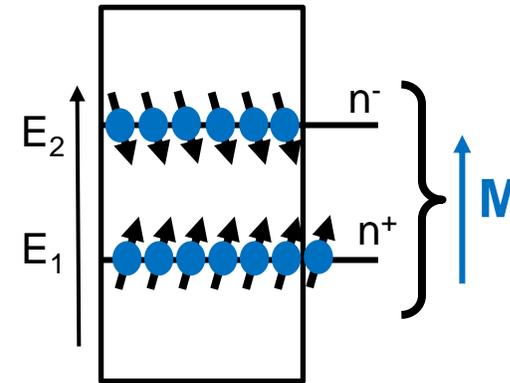
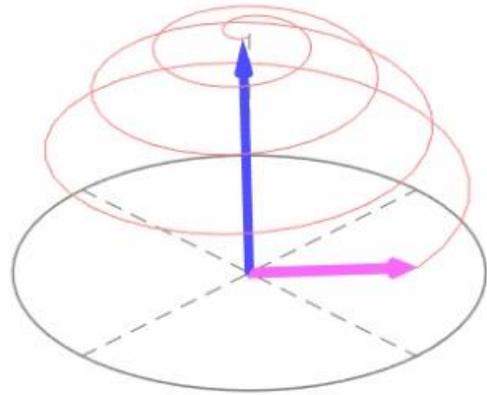
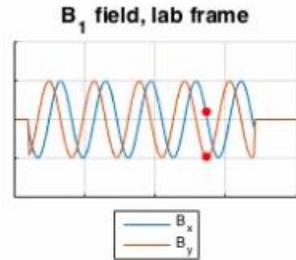


Overview



- ❑ Quick recap on how MRI works
- ❑ What can MRI do (almost) out of the box
- ❑ How can an MR physicist contribute to MRI?
 - ❑ Improving image reconstruction
 - ❑ Making imaging quantitative
 - ❑ Decoding microstructure

How does MRI work?



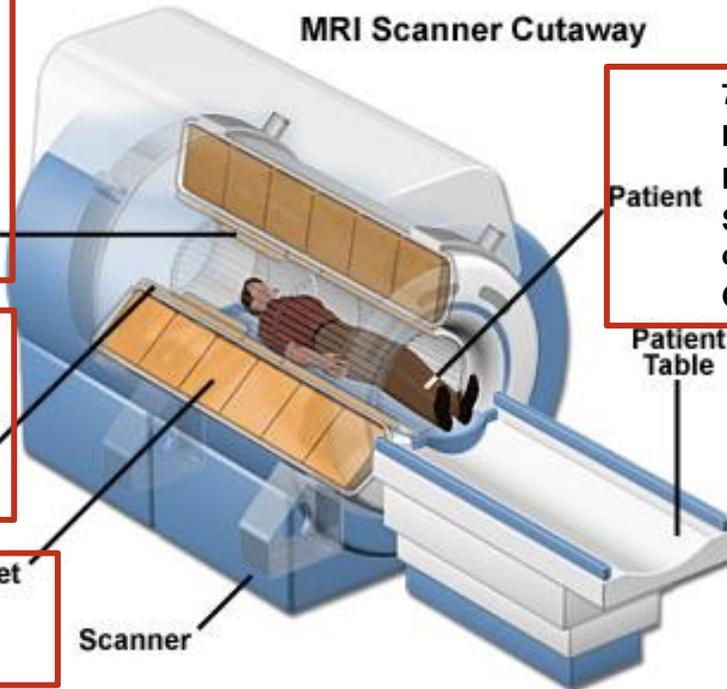
Generates RF wave to change spins state

The precession of this spins can be detected by induction of an antenna

Allows to ask the question of: which spins are precessing where

B₀ Magnet
 Makes sure there are two energy states for spins

MRI Scanner Cutaway



75 % water
 Nuclear spins (are sort of a magnet)
 Energy difference between states
 States transitions can be induced using a on resonance RF pulse
 Coherent spins will precess and relax

Radio Frequency Coil

Gradient Coils

Magnet

Scanner

Patient

Patient Table

What can MRI see?

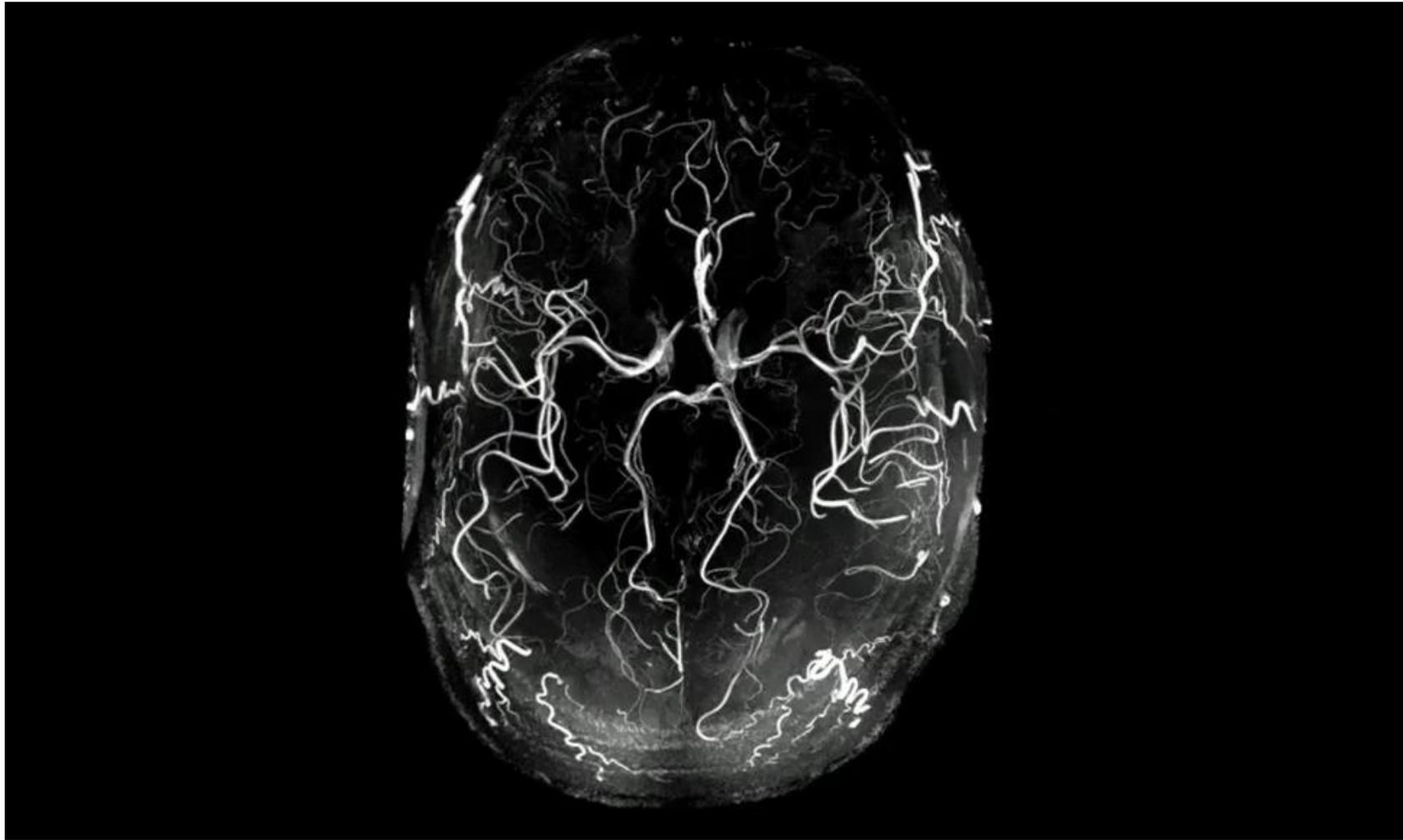


- Hydrogen proton spins in large quantities – Water or Fat
- Water in different environments (magnetic, macromolecular...)
- Water moving in macroscopically
- Water moving microscopically

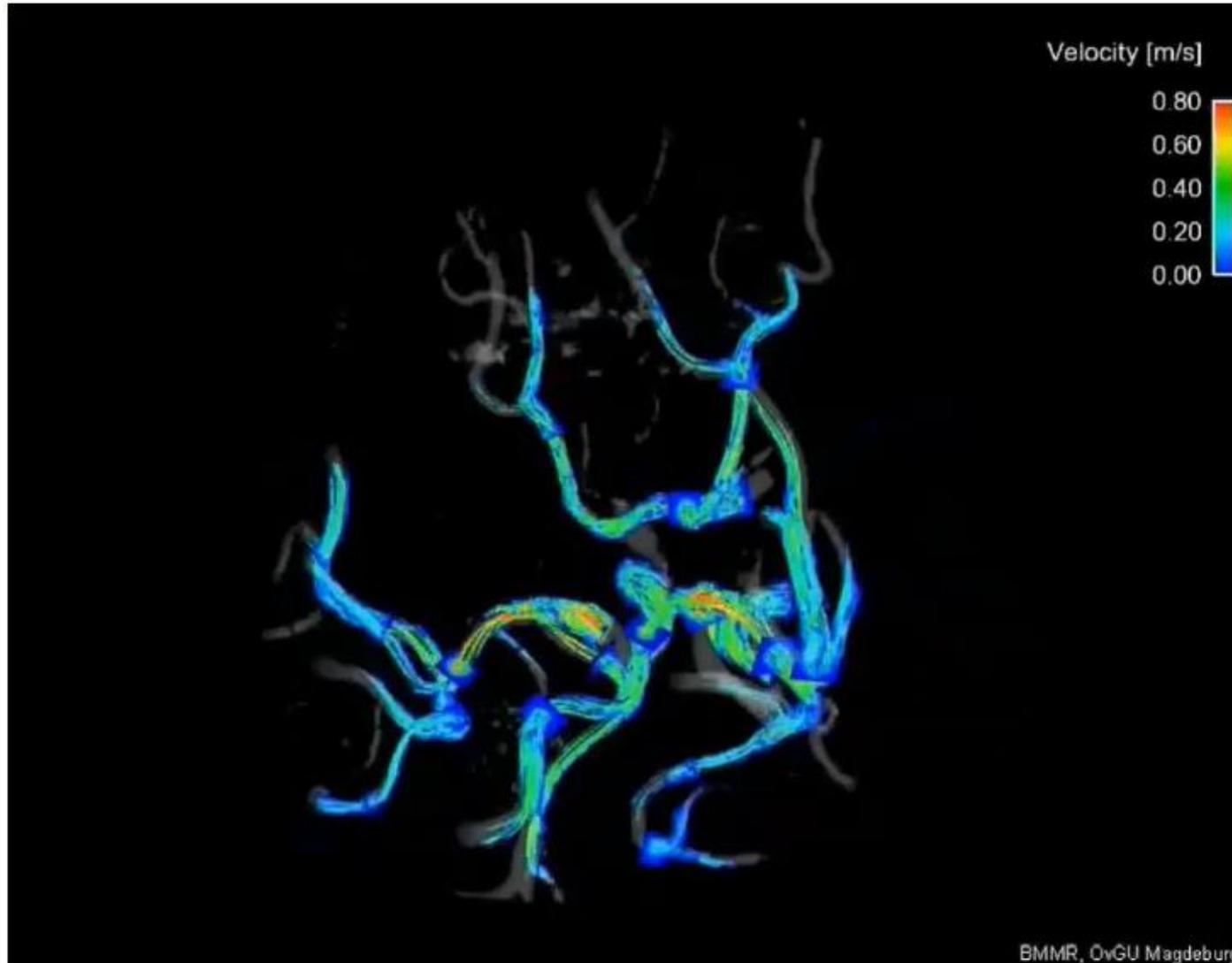
MRI allows looking at brain structure



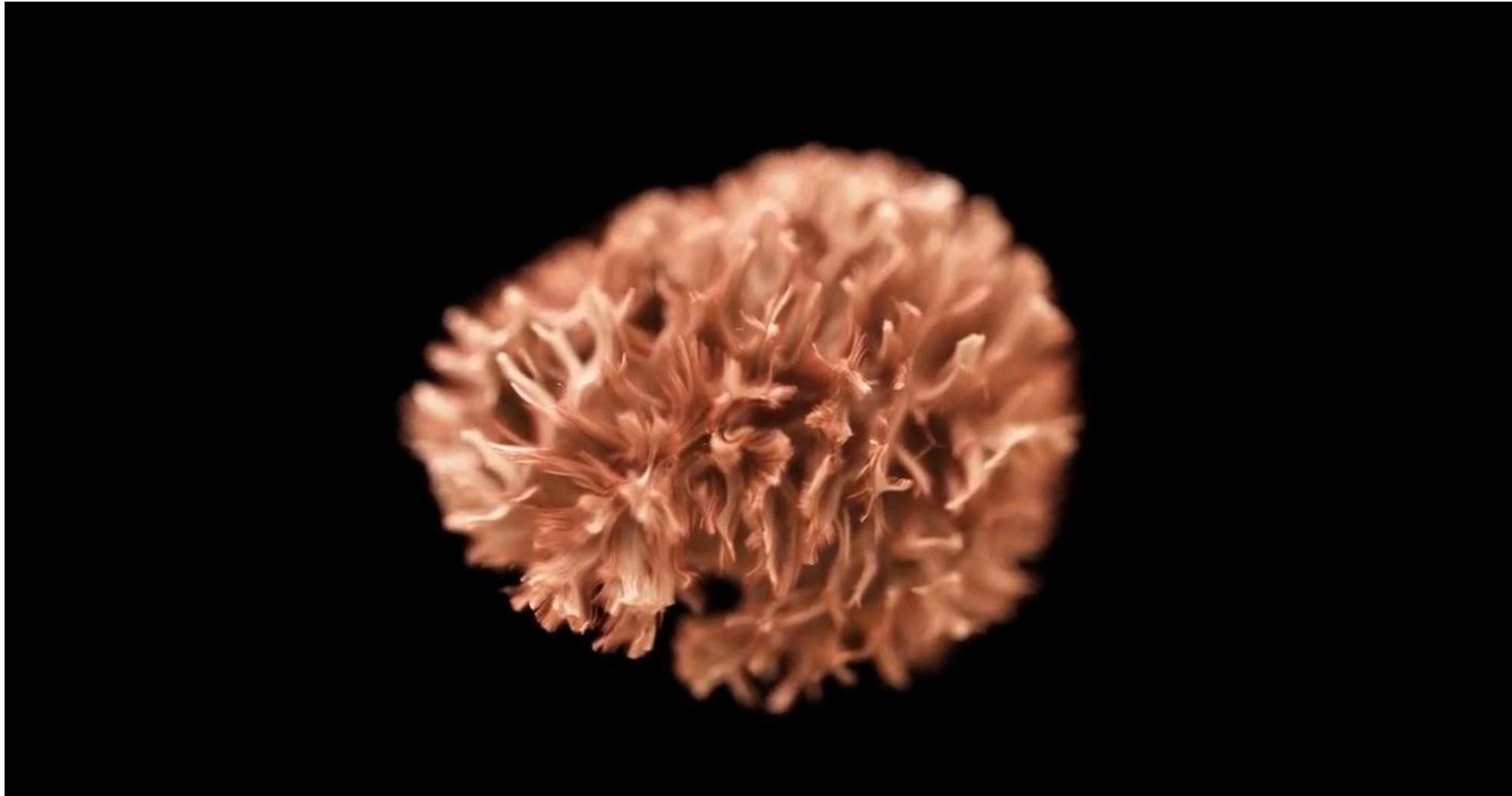
Allows looking at arteries



Allows looking at flow in arteries



MRI allows looking at brain microstructure

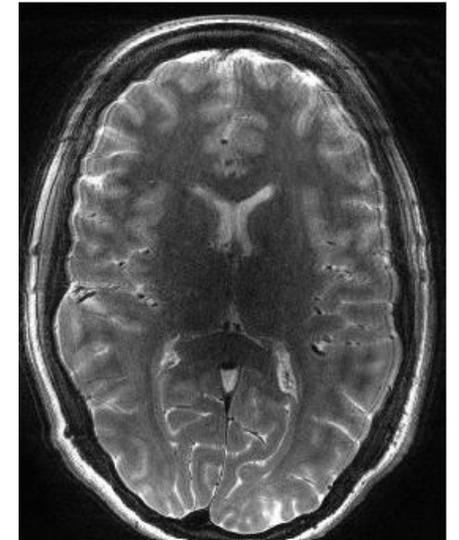
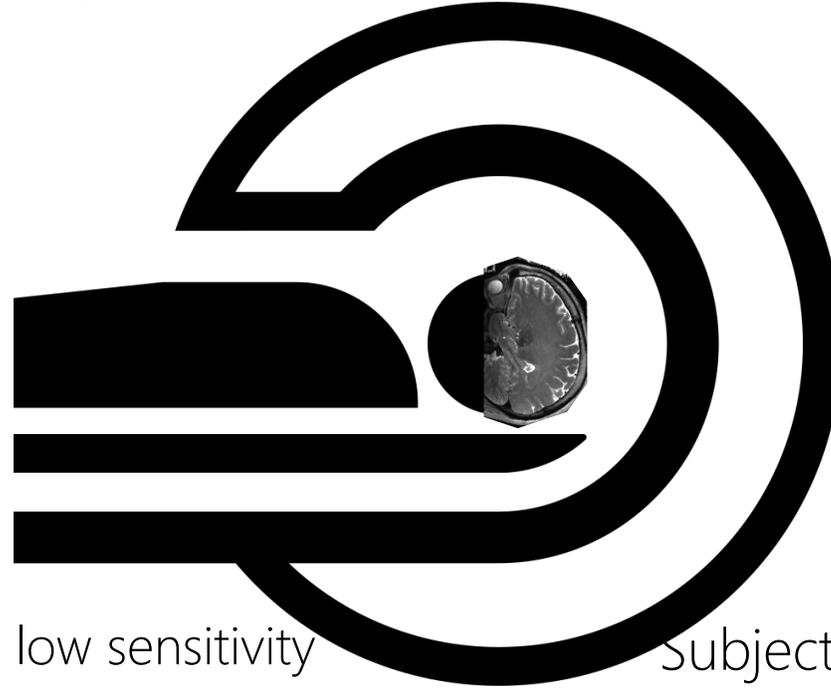
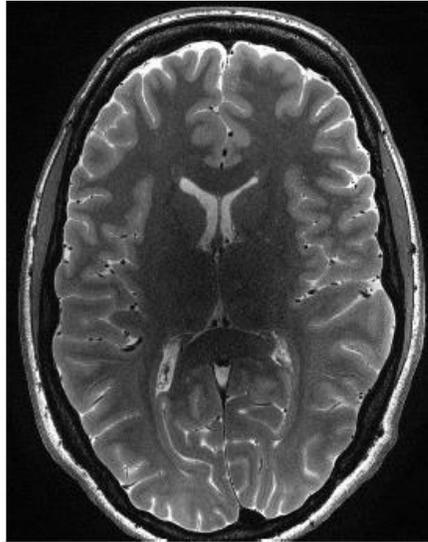


MR Physicist contribution to MRI

- ❑ Hardware design
- ❑ Image encoding and improving image reconstruction
- ❑ Fast and robust contrast encoding strategies
- ❑ Decoding the MR signal – extracting tissue properties



Improving image reconstruction



MRI has inherently a low sensitivity

Anatomical MRI

- high-res data requires long acquisitions
- Subjects are alive...

subject movement results in:

- Aliasing, Blurring, ghosting and ringing...
- Need of rescan in 8 – 30% of subject

Motion causes inconsistency of encoding

$$S(k) = \iiint Im(r, t) e^{ik(t) \cdot r} \quad Im(r) = FFT_{3D}(S(k)) dr$$

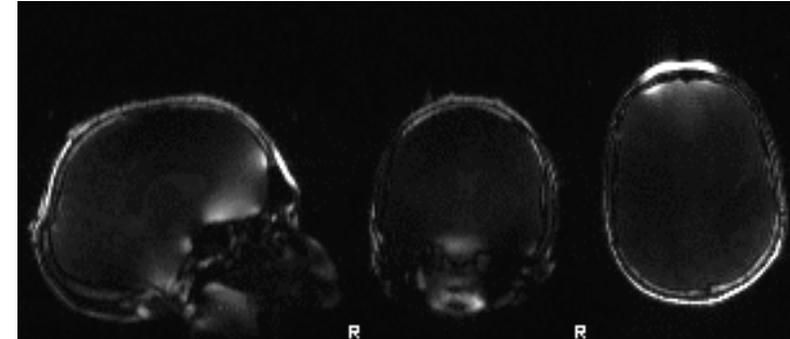
- Signal changes $Im(r, t) \neq Im(r)$
- Encoding the objects in the expected way

$$k_{actual}(t) \neq k_{designed}(t)$$

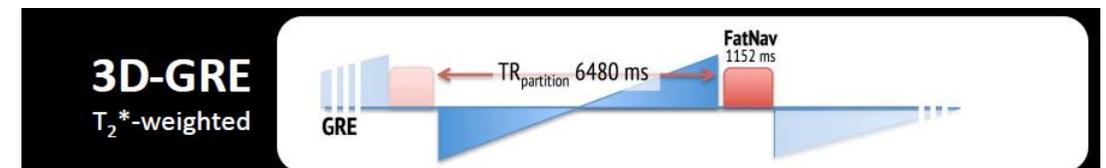
The whole head takes some time to encode...



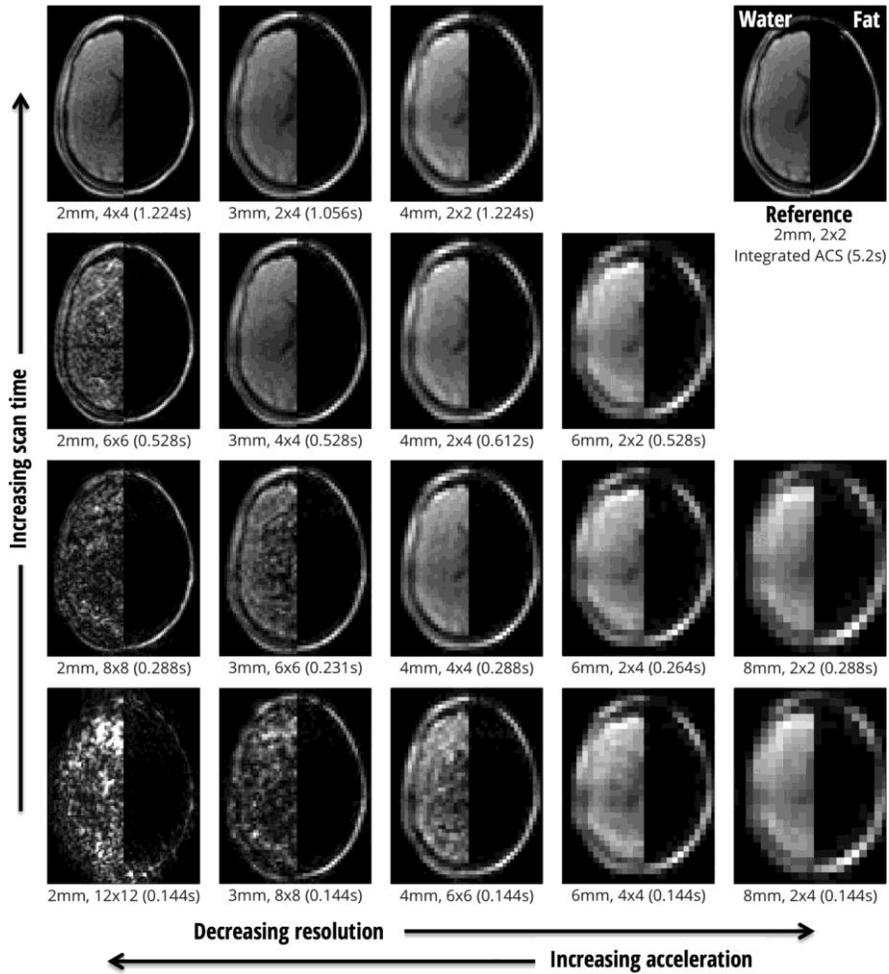
fat is sparse and fast to image ~16-64x



It does not «cost» water signal
Most high field anatomical sequences
have a dead time for a 3D nav



Motion estimation accuracy of Water and Fat Navigators



Examples of motion (un)corrected data

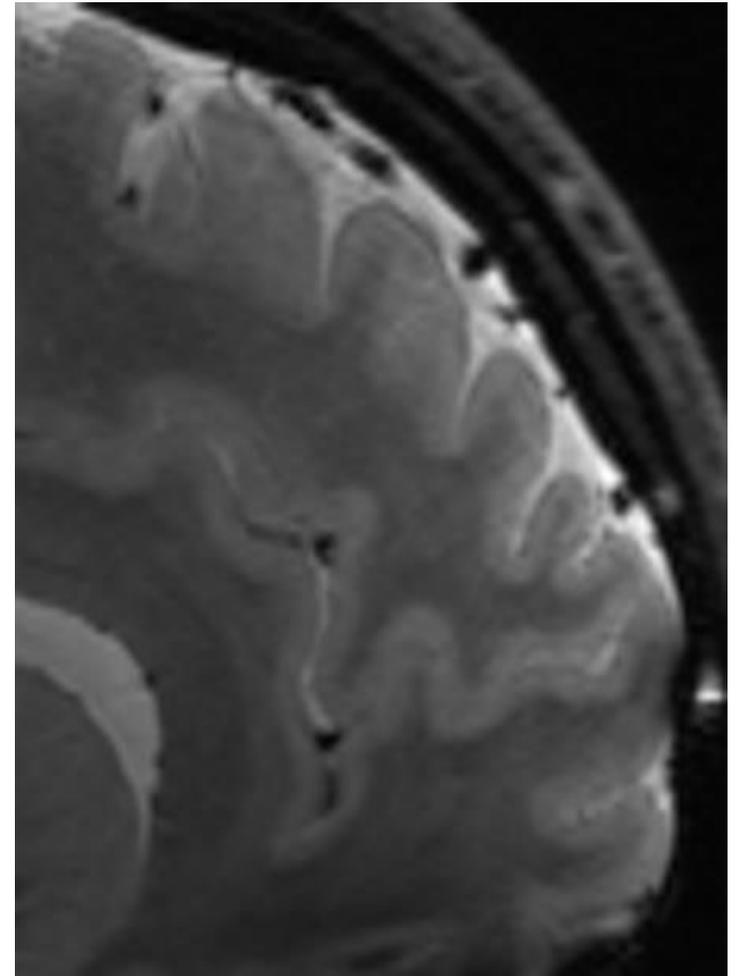
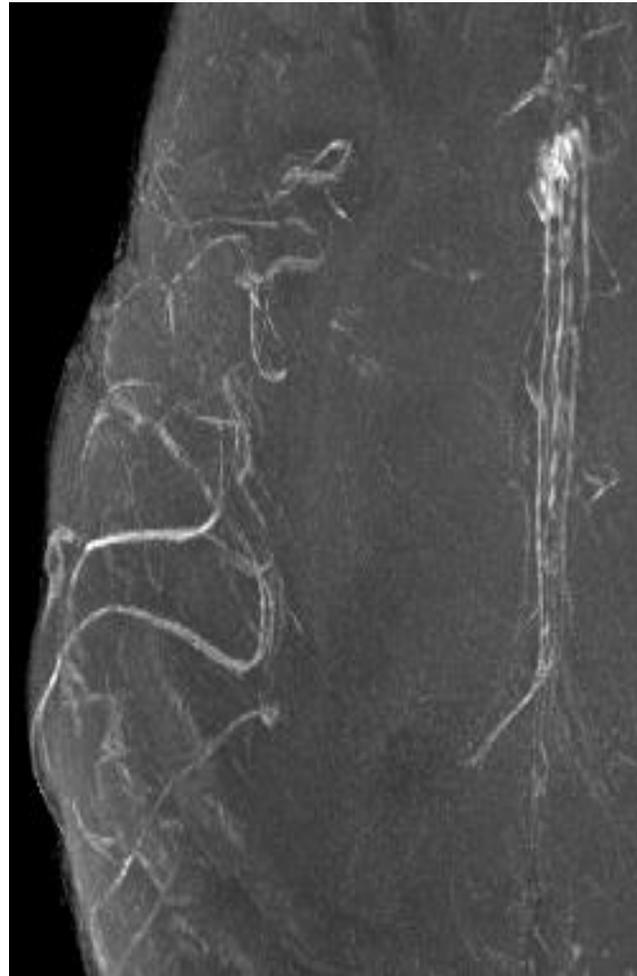
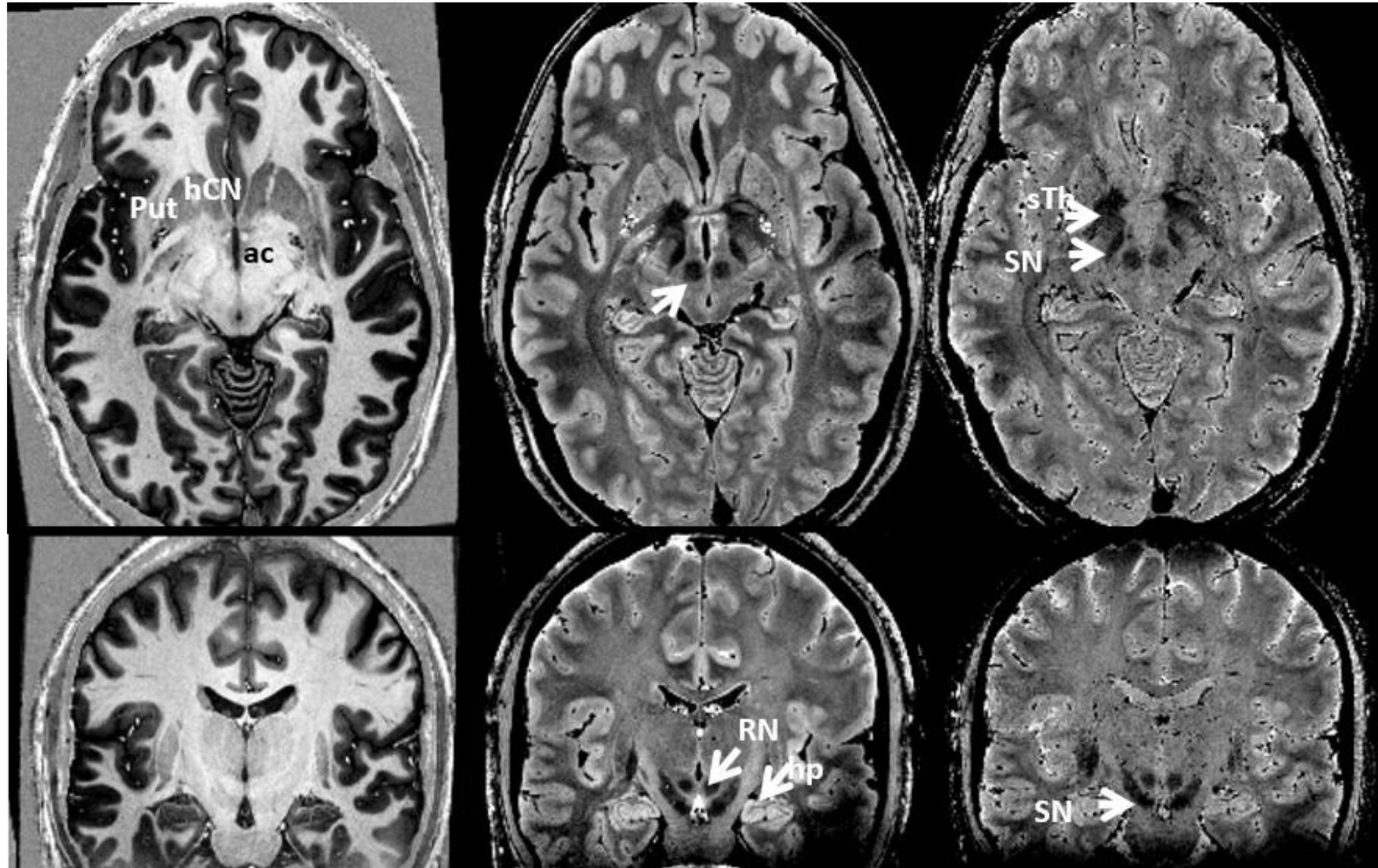


Image Quality Fixed



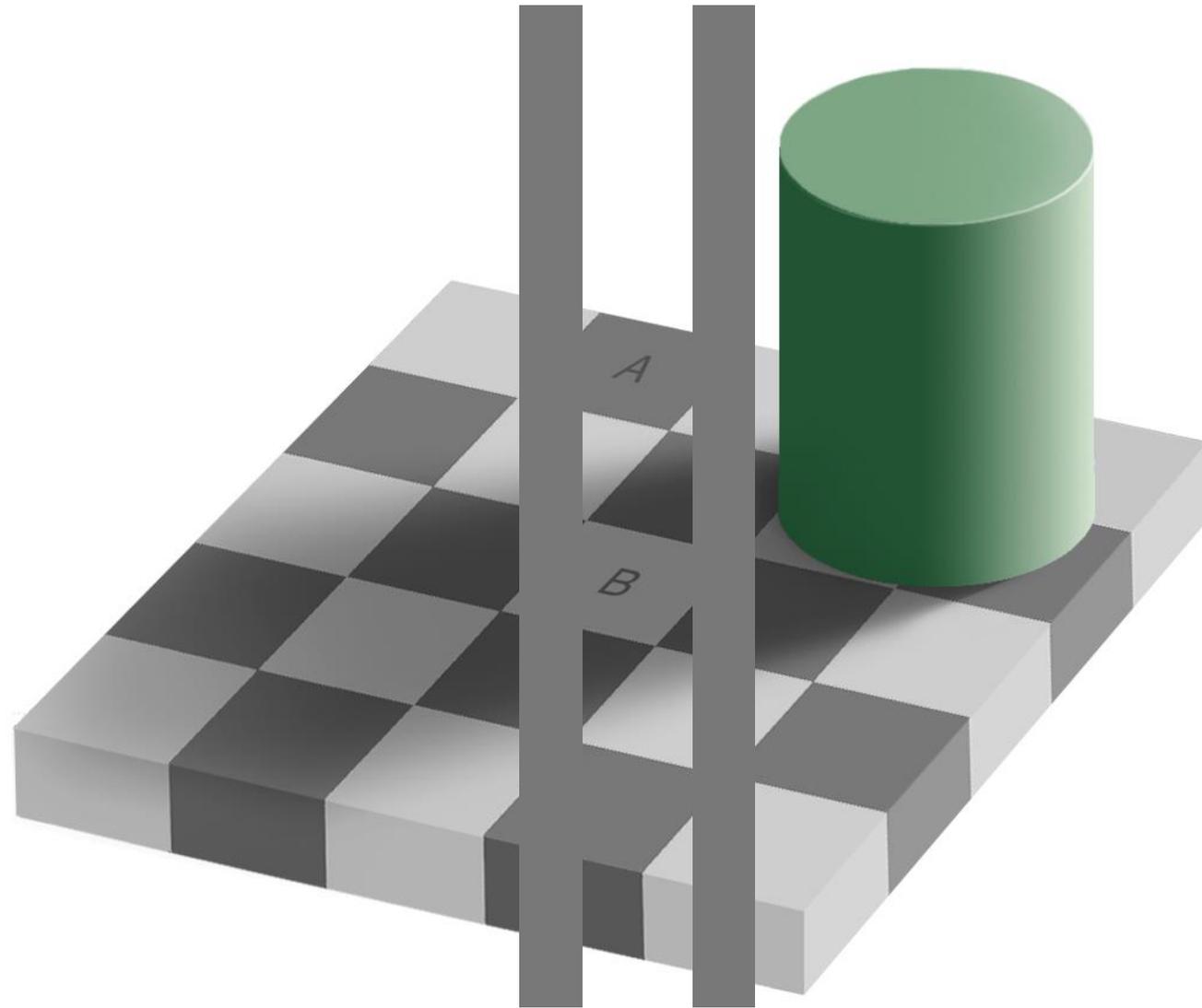
MRI comes with many flavours – “weightings”





The problem

- How does it relate to MRI images?



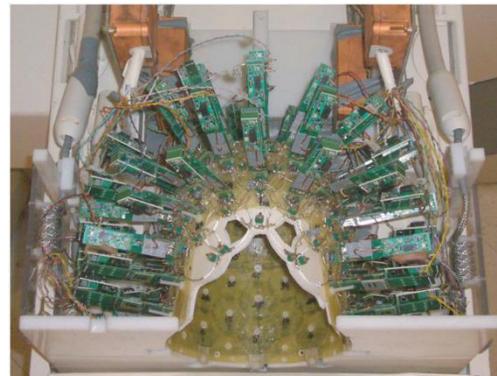
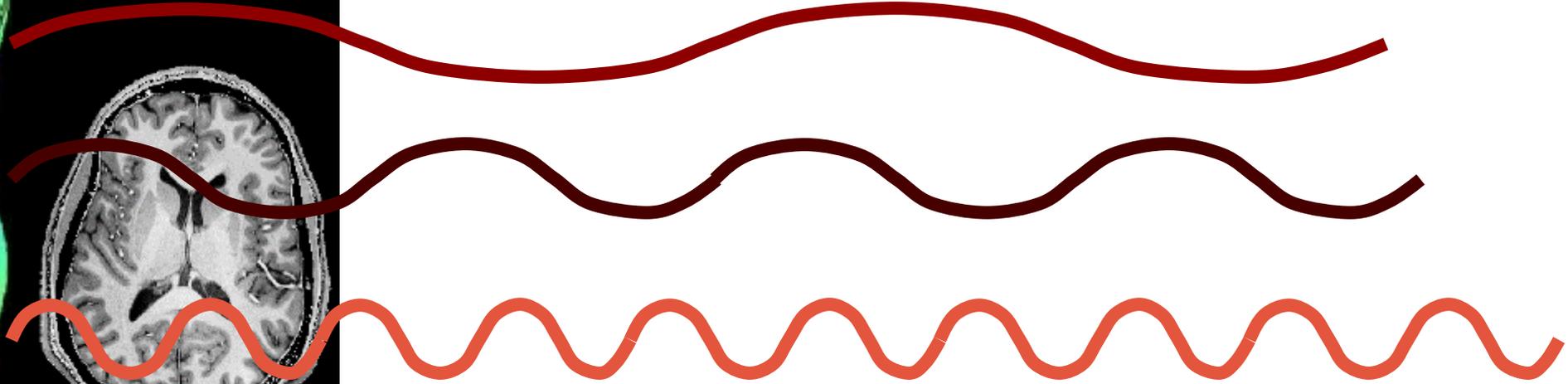
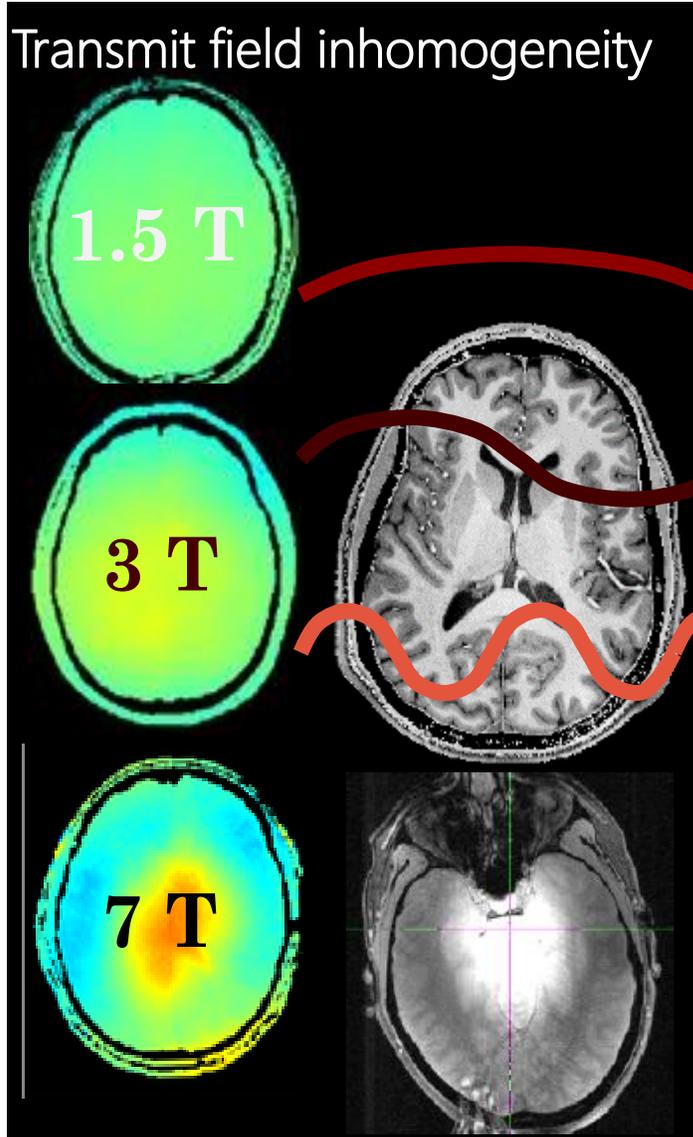
RF inhomogeneity



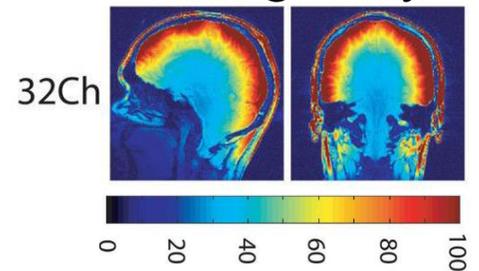
– We all want more signal, the “easy way”: higher B_0

$$\omega \propto B_0$$

$$\lambda \propto \frac{1}{B_0}$$



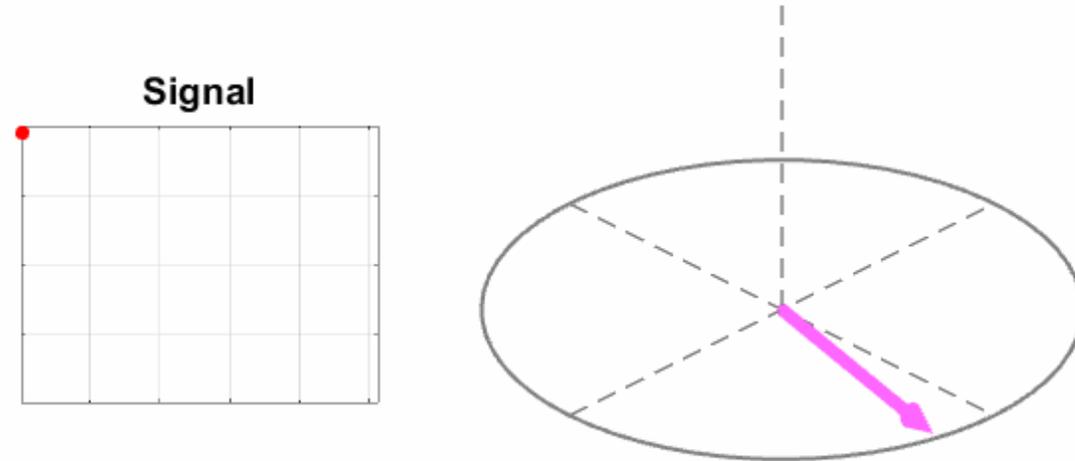
Receive field inhomogeneity



But there is hope...



Quantitative Imaging and Relaxation...



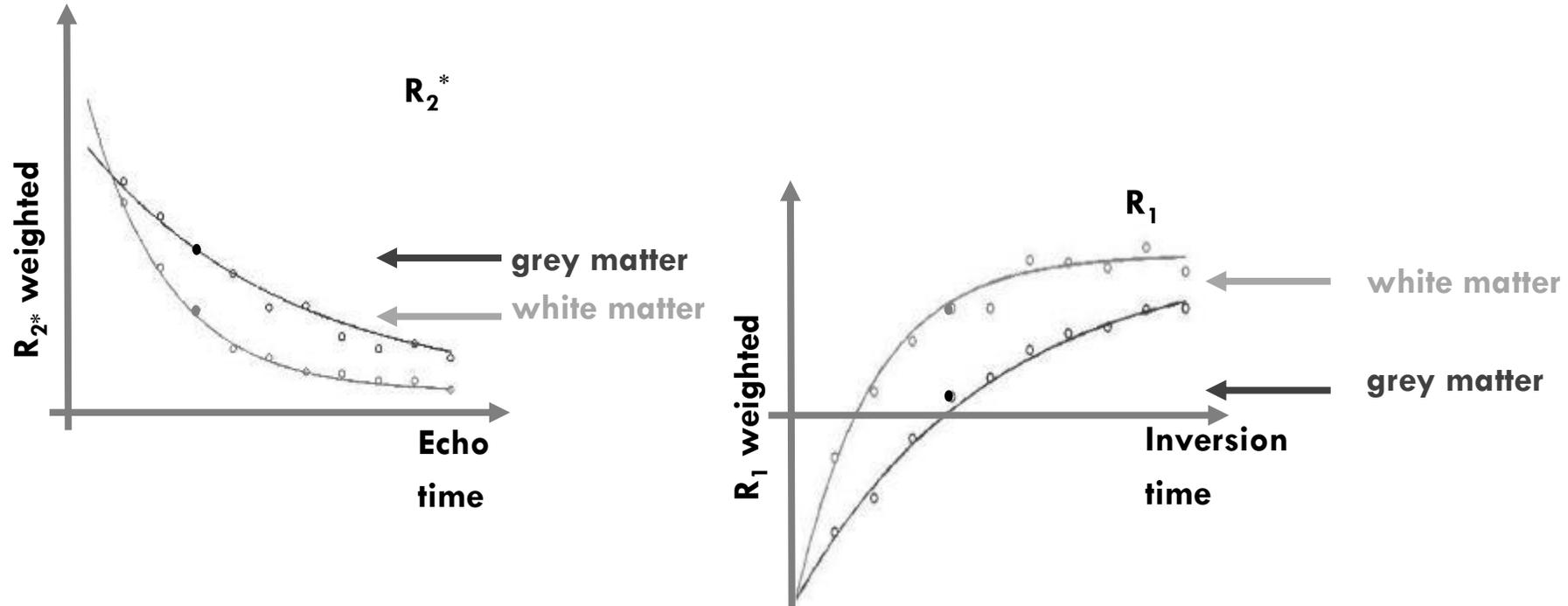
Relaxation restores the thermal **equilibrium** distribution of spins and builds up equilibrium magnetization

$R_2^{(*)}$ (apparent) transverse relaxation rate [s^{-1}]

$$- \{M_x, M_y, M_z\} \equiv \{0, 0, M_0\}.$$

R_1 longitudinal relaxation rate [s^{-1}]

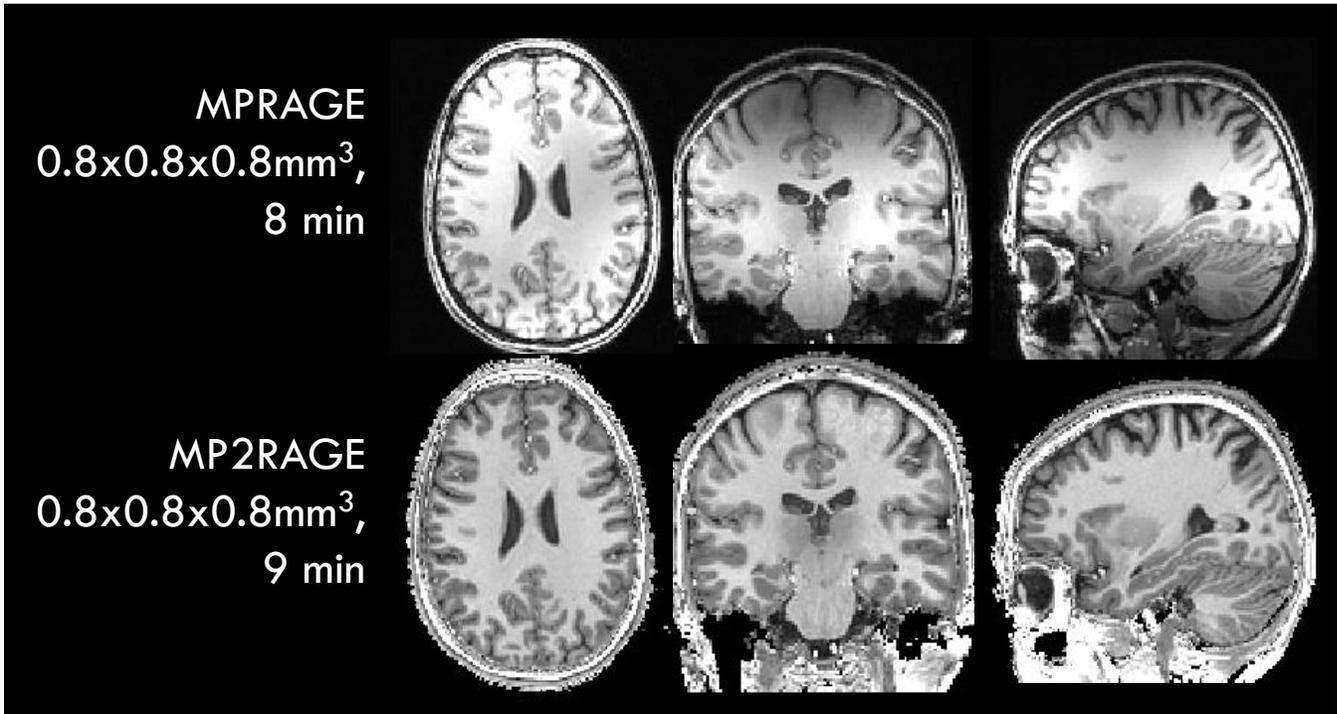
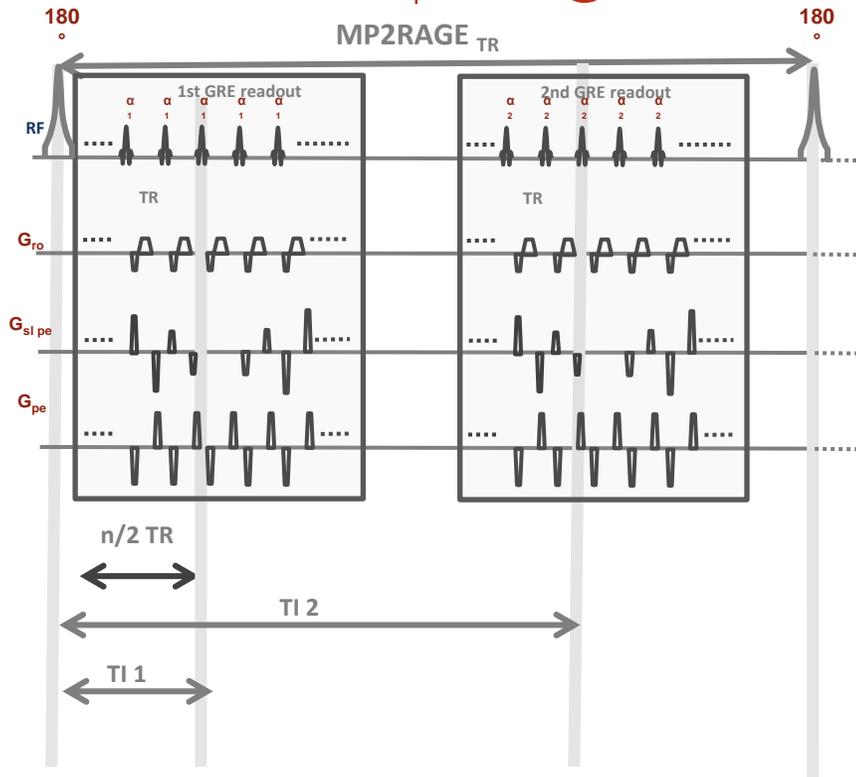
Weighted imaging vs relaxometry



The price:

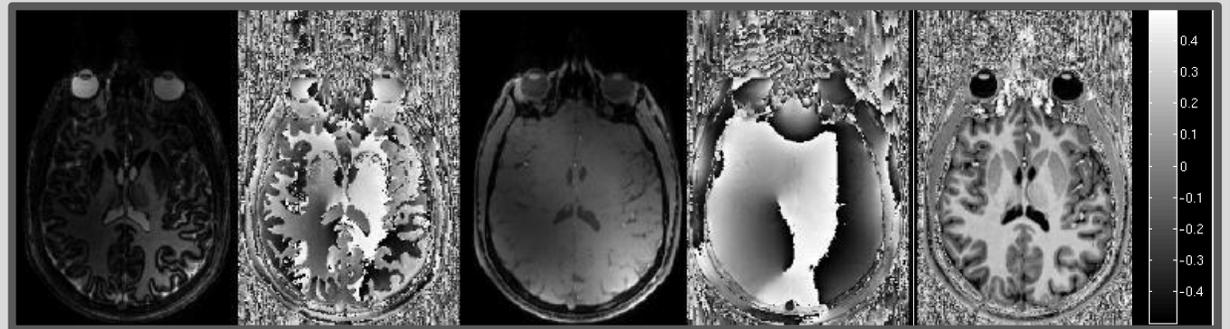
- More data points - > more acquisition time
- If one parameter is to be measured, you have to ensure that the signal does not depend on the remaining relaxation properties -> less efficient
- Non-linear fitting - > can be computationally expensive particularly as multiple parameters are obtained in one acquisition

From T_1 weighted to MP2RAGE and T1 mapping



After the combination of the two images:
 ~~M_0 effects;~~
 ~~T_2^* effects;~~
~~reception B_1^- effects;~~
~~transmission B_1^+ effects (not really);~~
 All we are left is mostly a T_1 dependence... T_1 estimation

7T



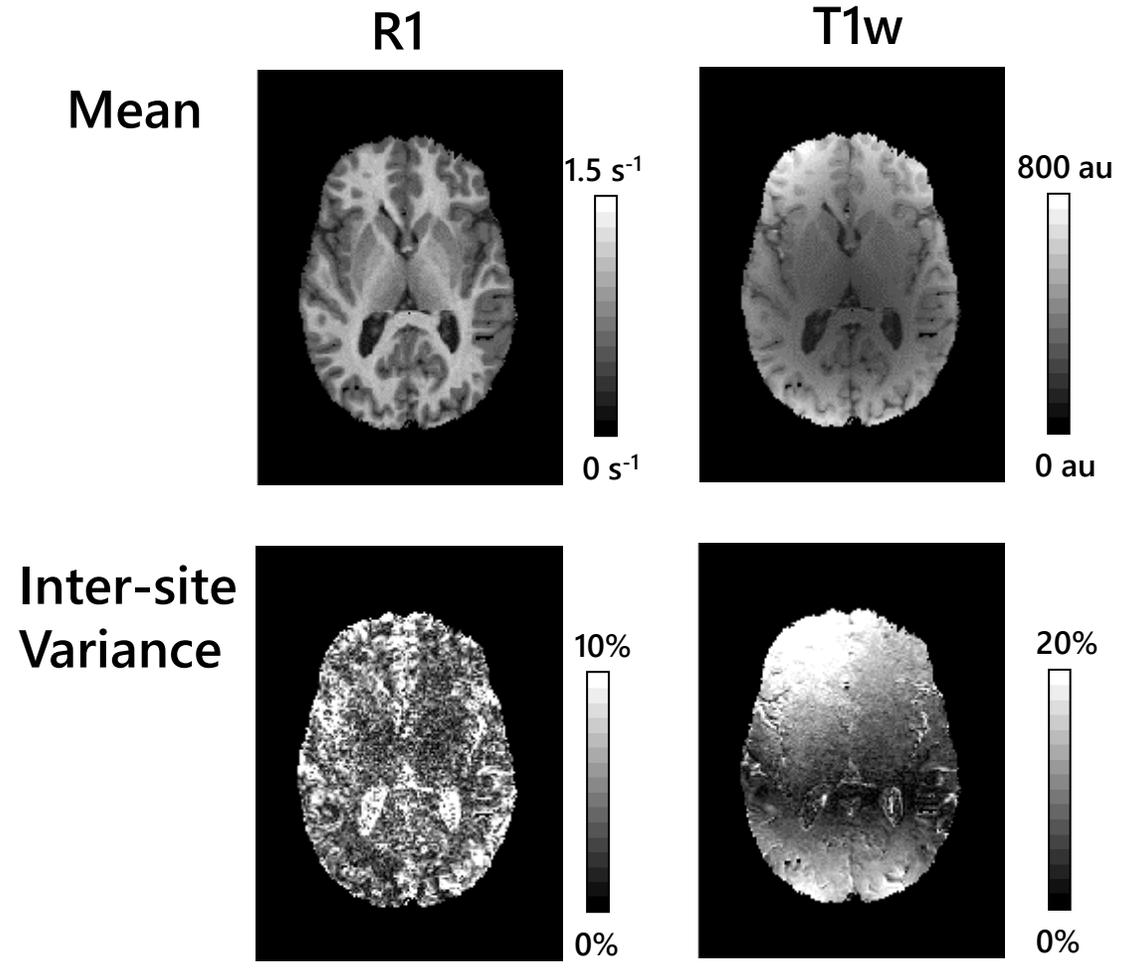
GRE_{T11}

GRE_{T12}

$$S = \frac{GRE_{T11}^* GRE_{T12}}{GRE_{T11}^2 + GRE_{T12}^2}$$



Quantitative imaging facilitates multi-center studies / comparing data



Relaxation rates



$$R_{1/2} = R_{1/2base} + r_{1/2stuff} [stuff]$$

$$R_{1/2} = \frac{1}{T_{1/2}}$$

What is stuff in the brain?



The usual suspects

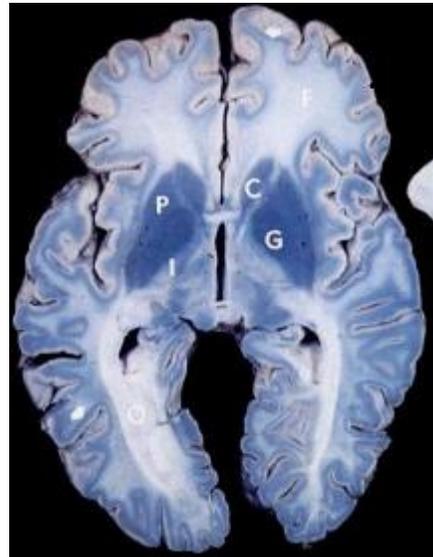
Deoxygenated
Blood



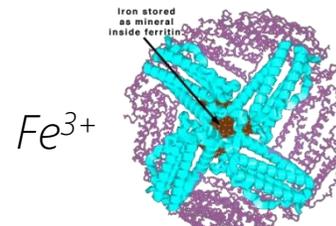
Paramagnetic
 $\chi = +$

Fe^{2+}

Iron
(non-heme)



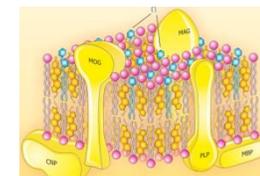
Paramagnetic
 $\chi = +$



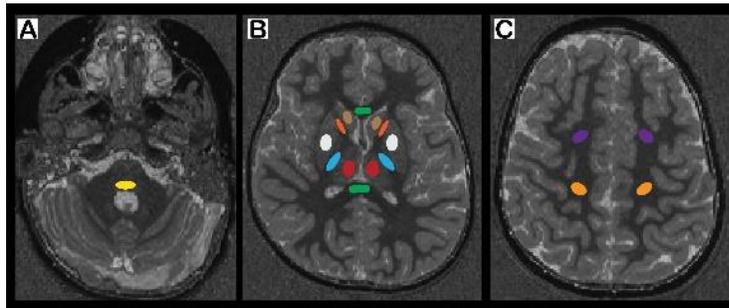
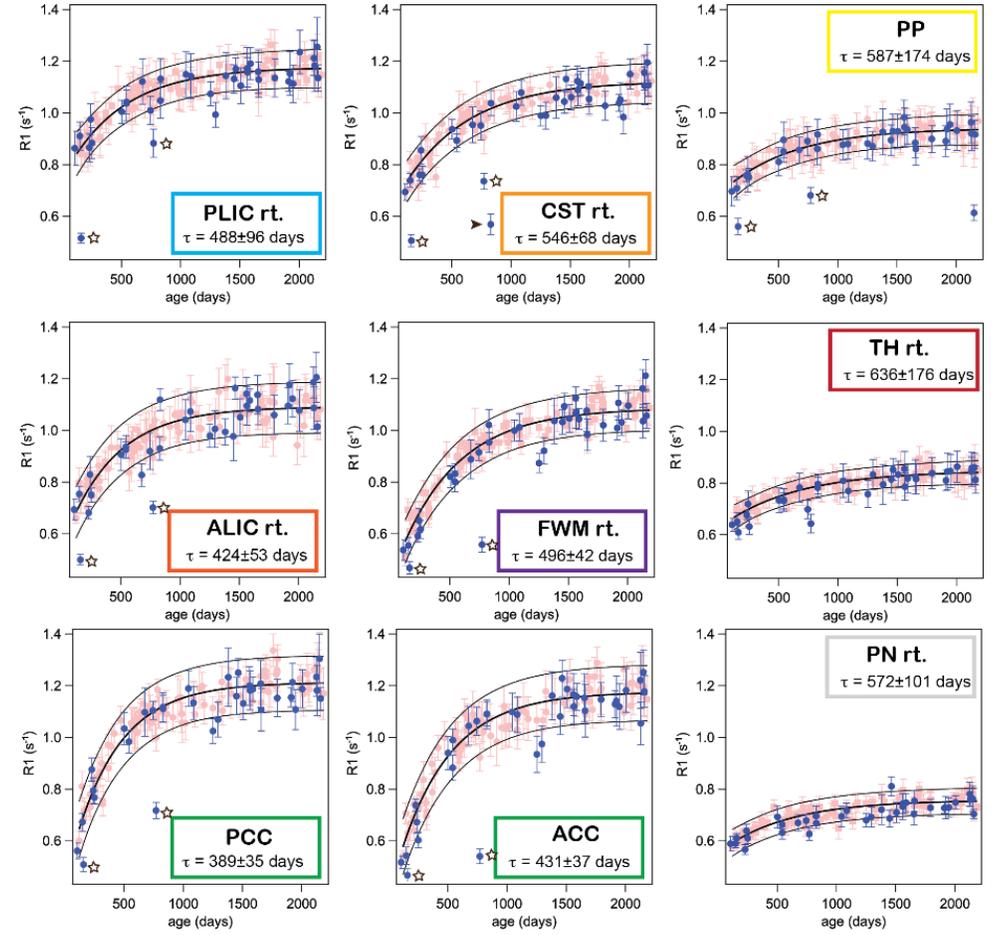
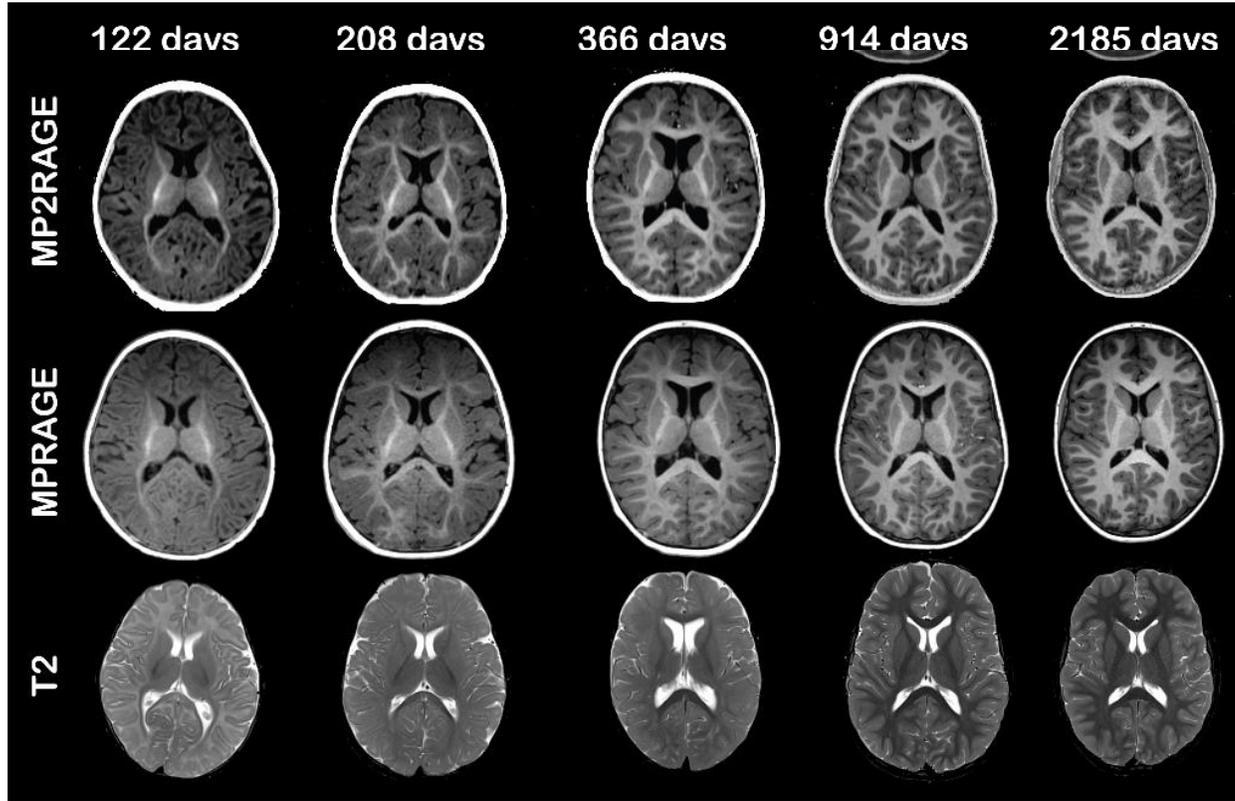
Myelin
density



Diamagnetic
 $\chi = -$



R1 mapping to study brain myelination



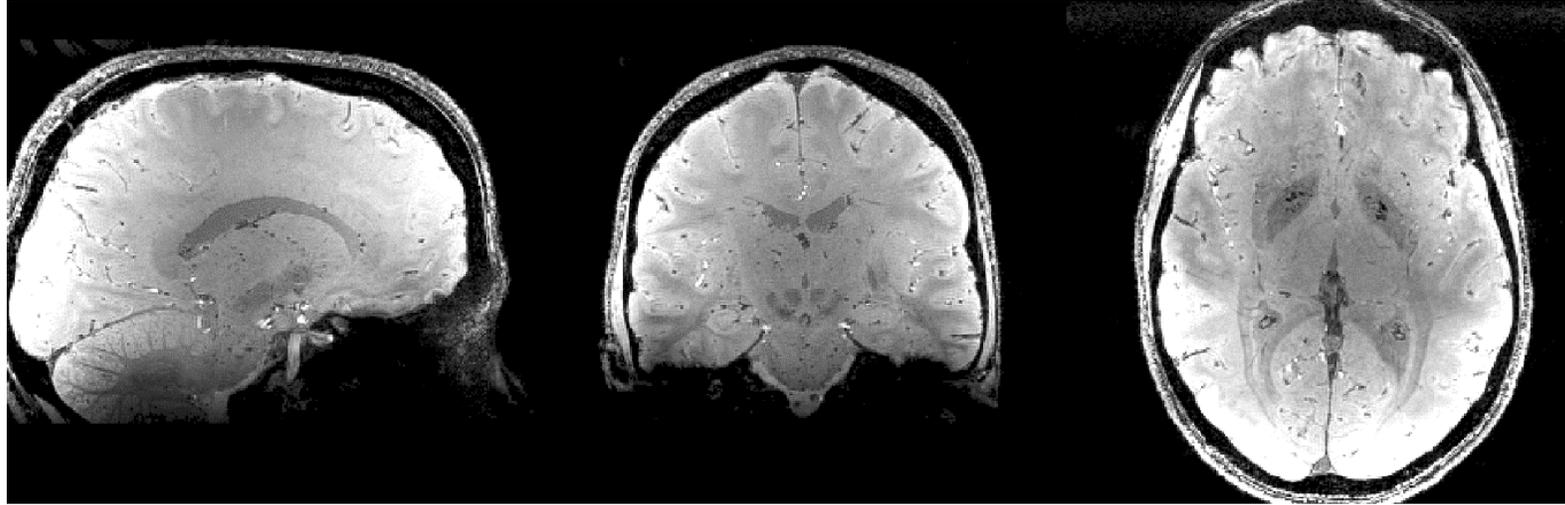
There is more to quantitative imaging than just relaxation



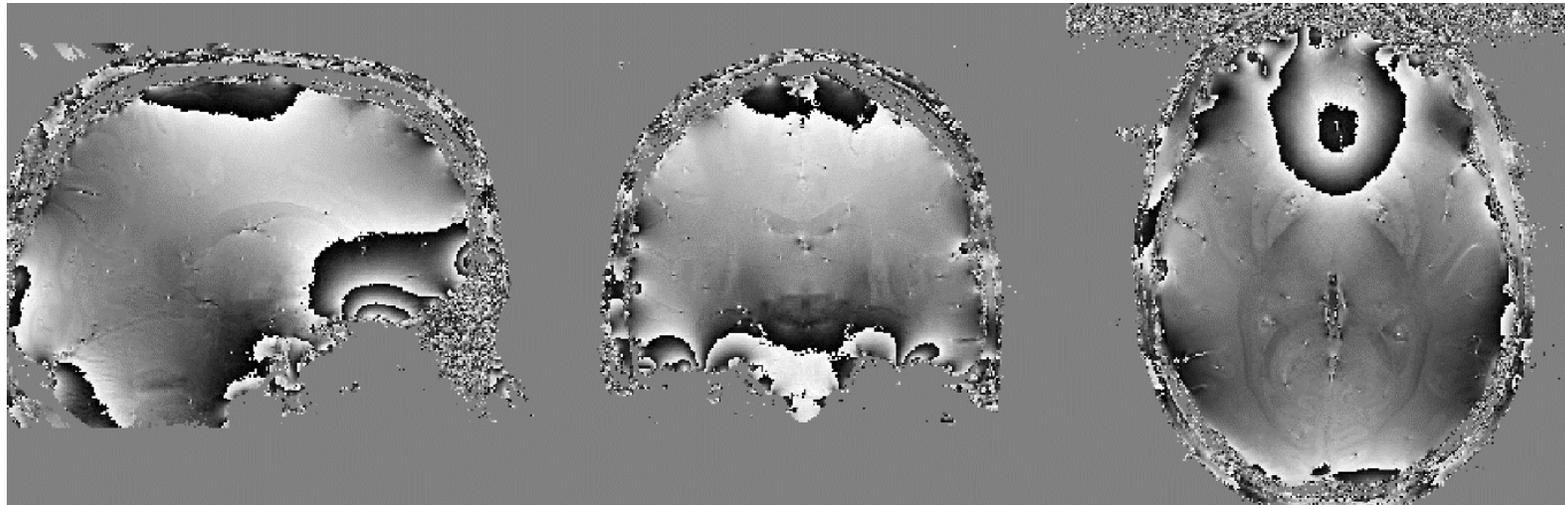
Gradient echo images TE1



Magnitude



Phase



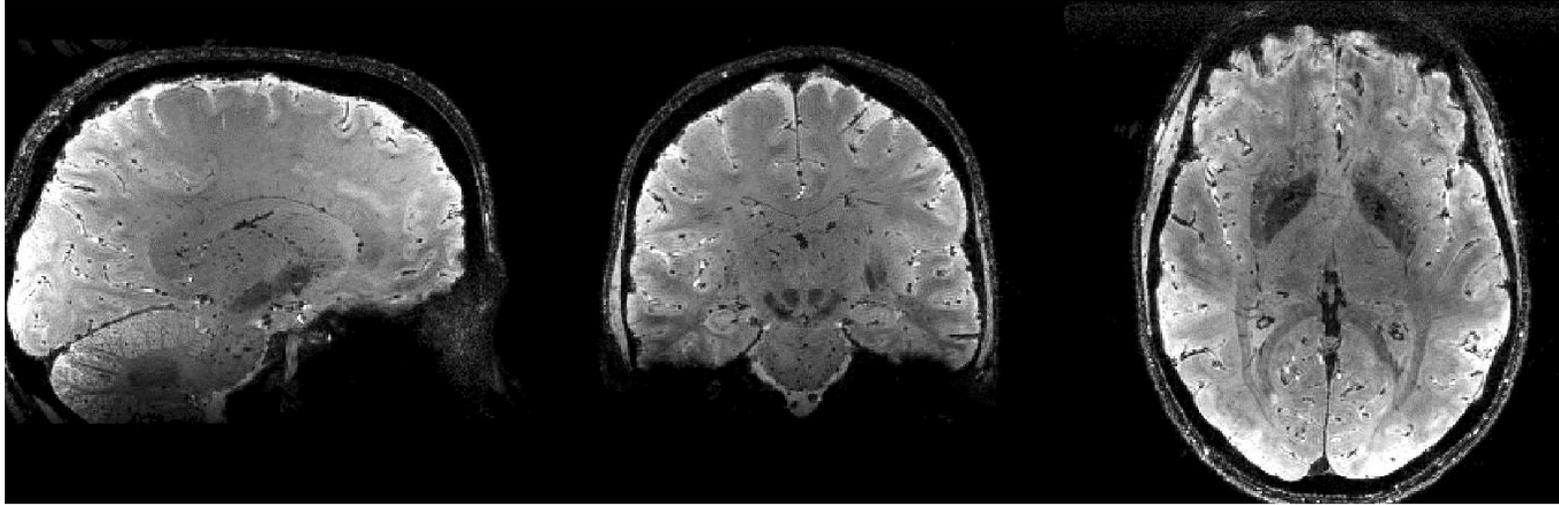
$$S = S_0 \exp\left(\frac{-TE}{T_2^*}\right)$$

$$\phi = \Delta B \gamma T E B_0$$

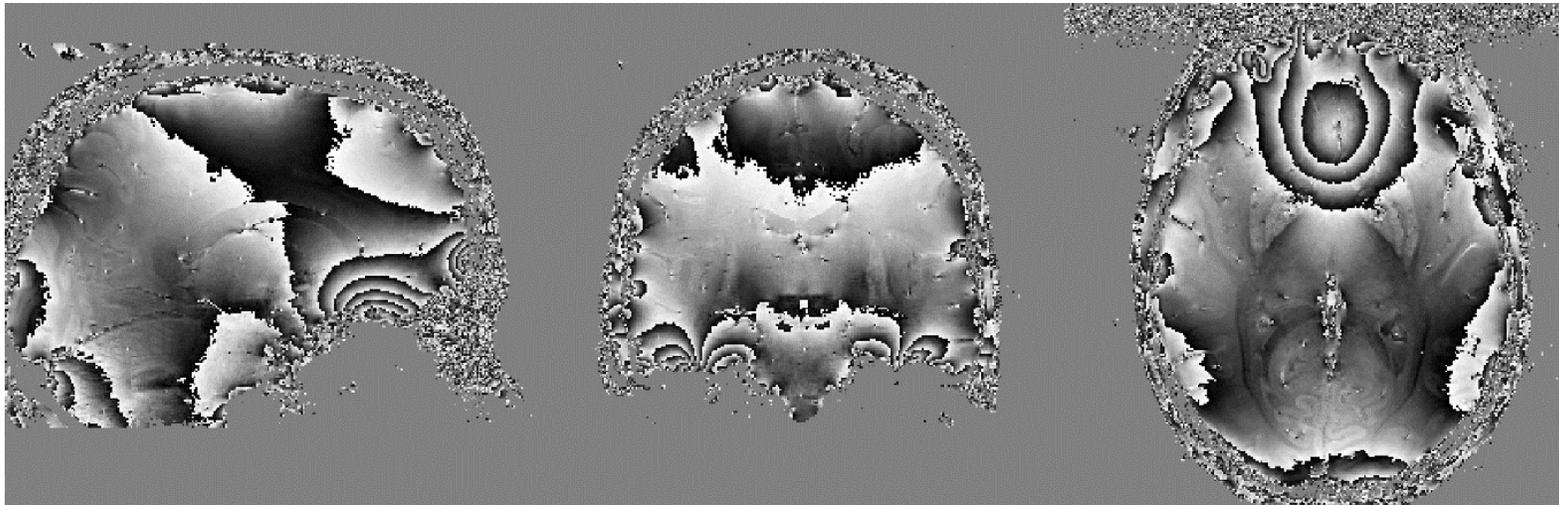
Gradient echo images TE2



Magnitude



Phase



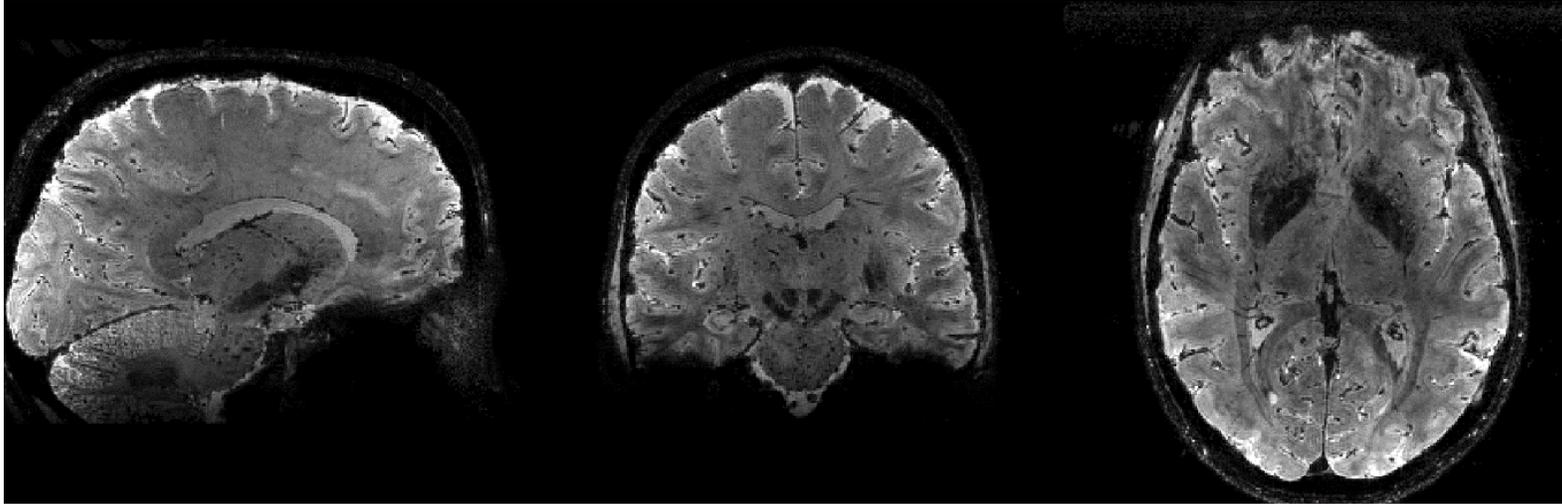
$$S = S_0 \exp\left(\frac{-TE}{T_2^*}\right)$$

$$\phi = \Delta B \gamma T E B_0$$

Gradient echo images TE3

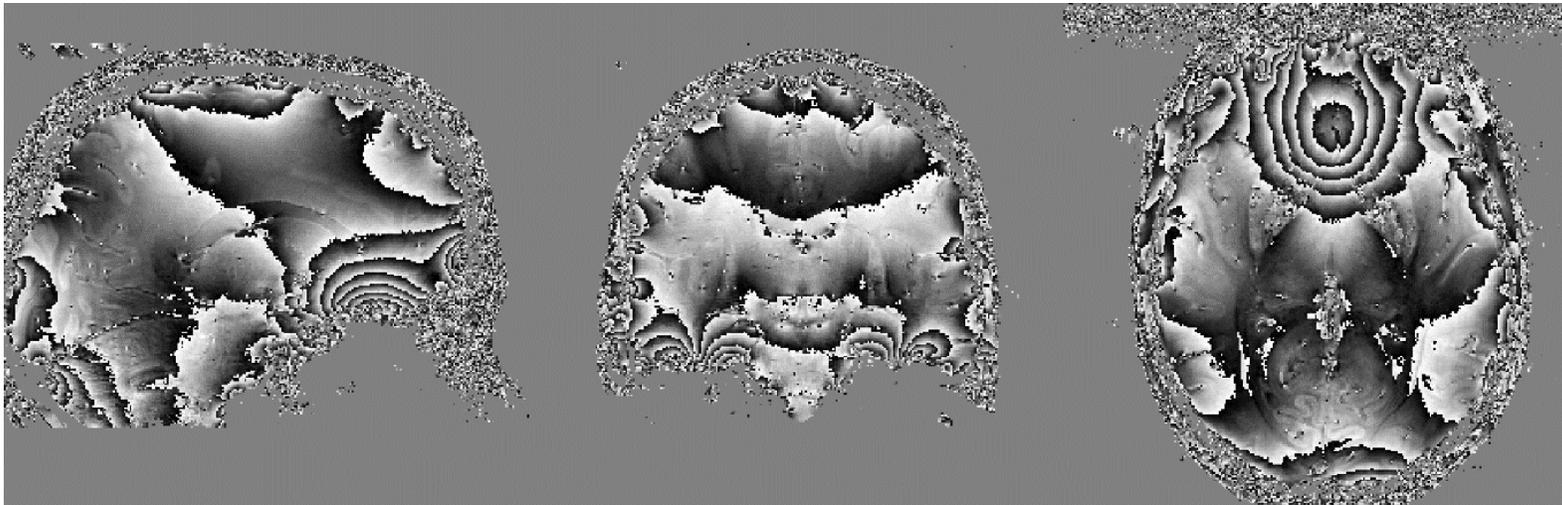


Magnitude



$i\gamma\Delta B_0 TE$

Phase



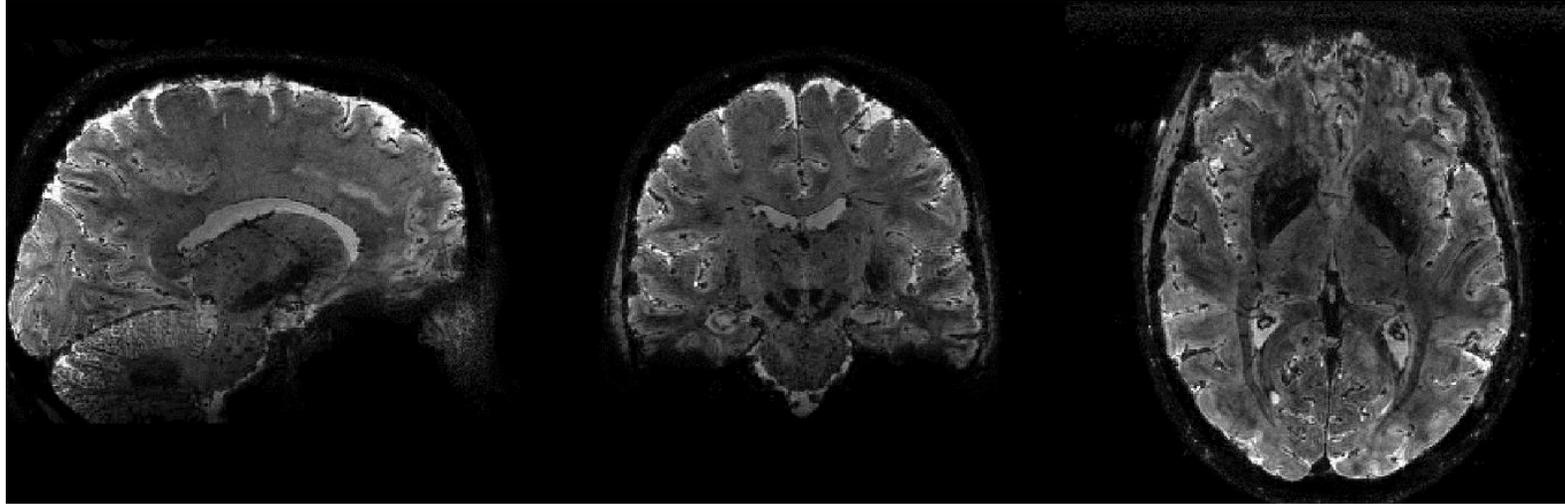
$$S = S_0 \exp\left(\frac{-TE}{T_2^*}\right)$$

$$\phi = \Delta B \gamma TE B_0$$

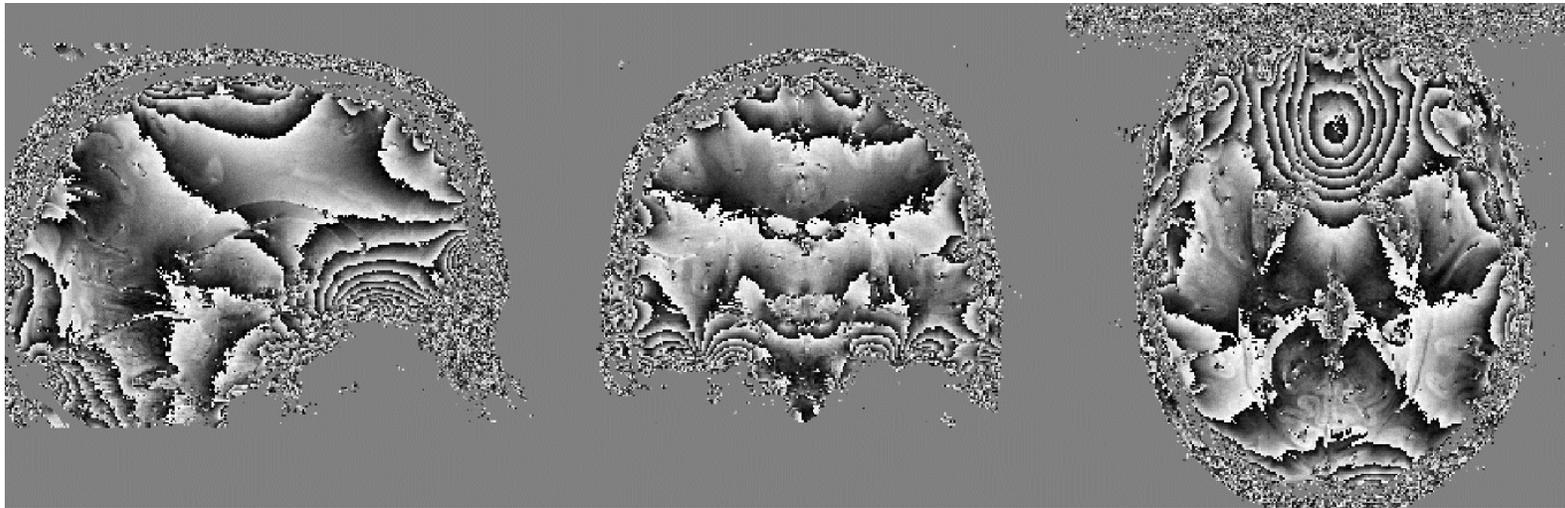
Gradient echo images TE5



Magnitude



Phase



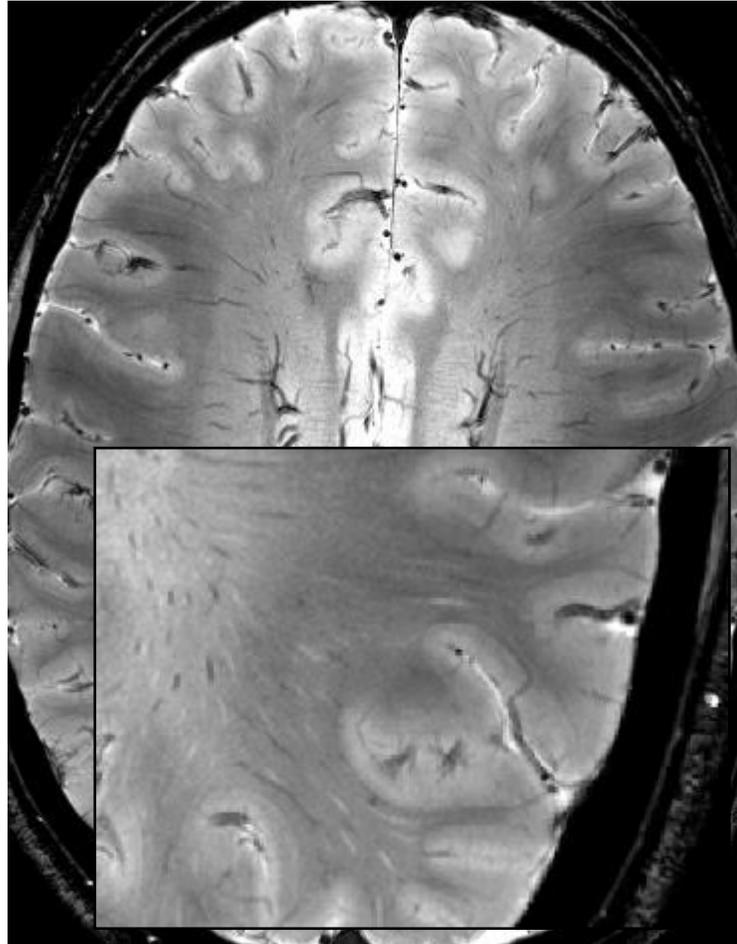
$$S = S_0 \exp\left(\frac{-TE}{T_2^*}\right)$$

$$\phi = \Delta B \gamma T E B_0$$

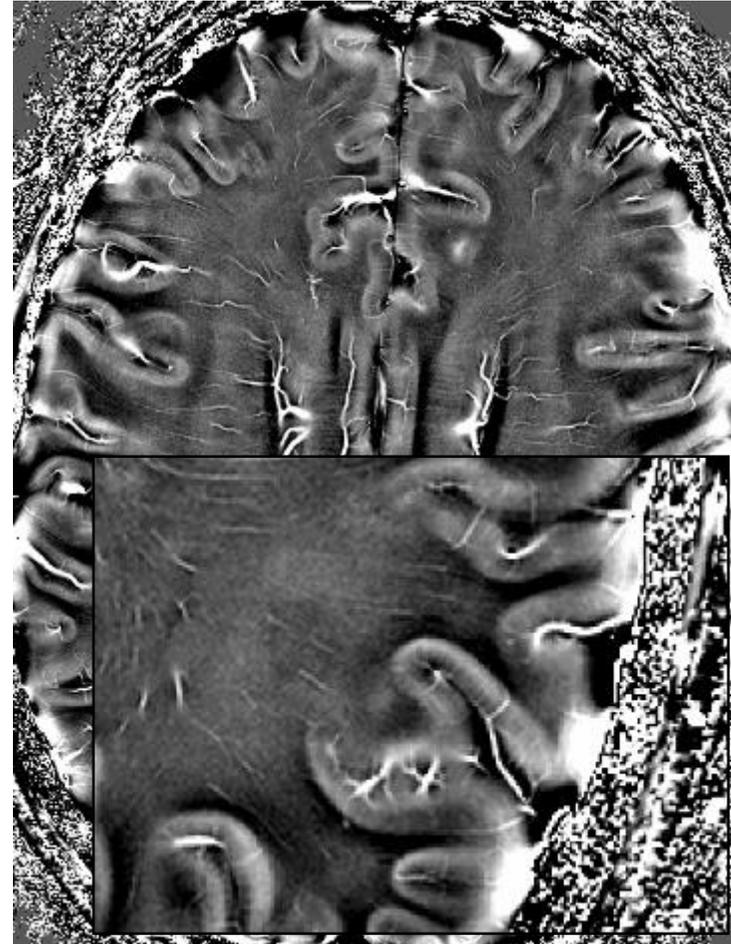
... after background field removal



Magnitude



Phase



$$S = S_0 \exp\left(\frac{-TE}{T_2^*}\right)$$

$$\phi = \Delta B \gamma T E B_0$$

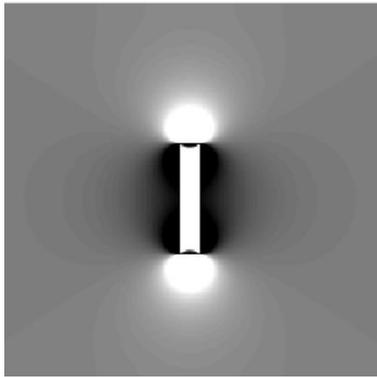
Quantitative Susceptibility Map



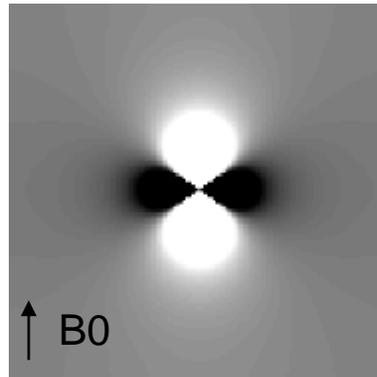
ΔB_z

D

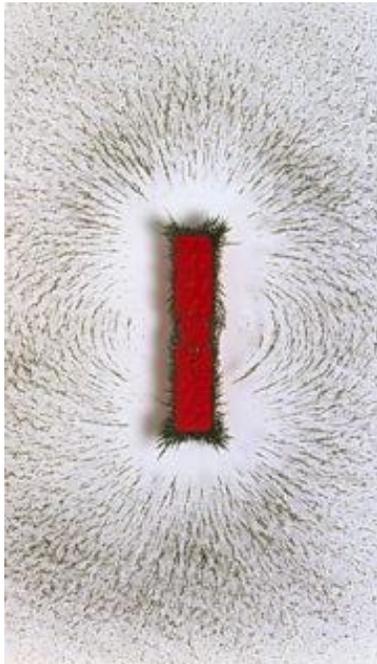
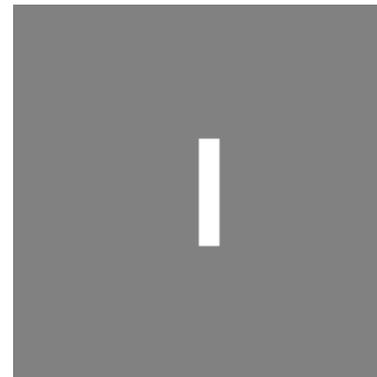
χ



=



⊗



MRI can measure the field perturbation

Quantitative Susceptibility Mapping (QSM) finds χ that could have generated ΔB

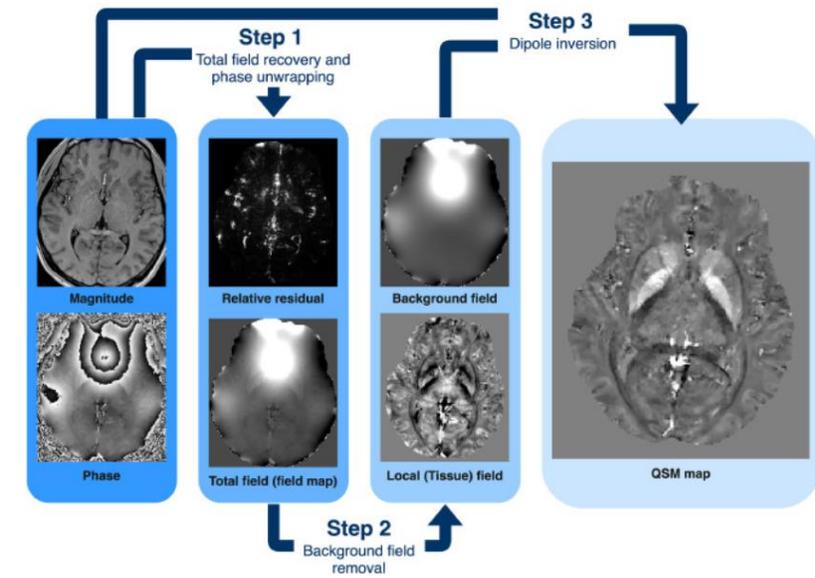
$$\min_{\chi} \|\Delta B - D * \chi\| + \lambda R(\chi)$$



SEPIA—Susceptibility mapping pipeline tool for phase images

Kwok-Shing Chan*, José P. Marques

Donders Institute for Brain, Cognition and Behaviour, Radboud University, Nijmegen, the Netherlands



QSM Challenges & open science



Magnetic Resonance in Medicine 79:1661–1673 (2018)

Quantitative Susceptibility Mapping: Report From the 2016 Reconstruction Challenge

Christian Langkammer¹,² Ferdinand Schweser^{2,3*}, Karin Shmueli⁴,⁵ Christian Kames,⁵ Xu Li,^{6,7} Li Guo,⁸ Carlos Milovic^{9,10}, Jinsuh Kim,¹¹ Hongjiang Wei,¹² Kristian Bredies,¹³ Sagar Buch,¹⁴ Yihao Guo,⁶ Zhe Liu¹⁵, Jakob Meineke,¹⁶ Alexander Rauscher,⁵ José P. Marques,¹⁷ and Berkin Bilgic¹⁸

FULL PAPER

Magnetic Resonance in Medicine

QSM reconstruction challenge 2.0: Design and report of results

QSM Challenge 2.0 Organization Committee | Berkin Bilgic^{1,2,3} | Christian Langkammer⁴ | José P. Marques⁵ | Jakob Meineke⁶ | Carlos Milovic^{7,8,9} | Ferdinand Schweser^{10,11}

¹Athinoula A. Martinos Center for Biomedical Imaging, Charlestown, Massachusetts, USA

²Department of Radiology, Harvard Medical School, Boston, Massachusetts, USA

³Harvard-MIT Health Sciences and Technology, MIT, Cambridge, Massachusetts, USA

⁴Department of Neurology, Medical University of Graz, Graz, Austria

⁵Donders Centre for Cognitive Neuroimaging, Radboud University, Nijmegen, Netherlands

⁶Philips Research, Hamburg, Germany

⁷Department of Electrical Engineering, Pontificia Universidad Catolica de Chile, Santiago, Chile

⁸Biomedical Imaging Center, Pontificia Universidad Catolica de Chile, Santiago, Chile

⁹Department of Medical Physics and Biomedical Engineering, University College London, London, UK

¹⁰Buffalo Neuroimaging Analysis Center, Department of Neurology, Jacobs School of Medicine and Biomedical Sciences, University at Buffalo, The State University of New York, Buffalo, New York, USA

¹¹Center for Biomedical Imaging, Clinical and Translational Science Institute, University at Buffalo, The State University of New York, Buffalo, New York, USA

FULL PAPER

Magnetic Resonance in Medicine

QSM reconstruction challenge 2.0: A realistic in silico head phantom for MRI data simulation and evaluation of susceptibility mapping procedures

José P. Marques¹ | Jakob Meineke² | Carlos Milovic^{3,4,5} | Berkin Bilgic^{6,7,8} | Kwok-Shing Chan¹ | Renaud Hedouin^{1,9} | Wietske van der Zwaag¹⁰ | Christian Langkammer¹¹ | Ferdinand Schweser^{12,13}

¹Donders Institute for Brain, Cognition and Behavior, Radboud University, Nijmegen, the Netherlands

²Philips Research, Hamburg, Germany

³Department of Electrical Engineering, Pontificia Universidad Catolica de Chile, Santiago, Chile

⁴Biomedical Imaging Center, Pontificia Universidad Catolica de Chile, Santiago, Chile

⁵Department of Medical Physics and Biomedical Engineering, University College London, London, United Kingdom

⁶Athinoula A. Martinos Center for Biomedical Imaging, Charlestown, Massachusetts, USA

⁷Department of Radiology, Harvard Medical School, Boston, Massachusetts, USA

⁸Harvard-MIT Health Sciences and Technology, MIT, Cambridge, Massachusetts, USA

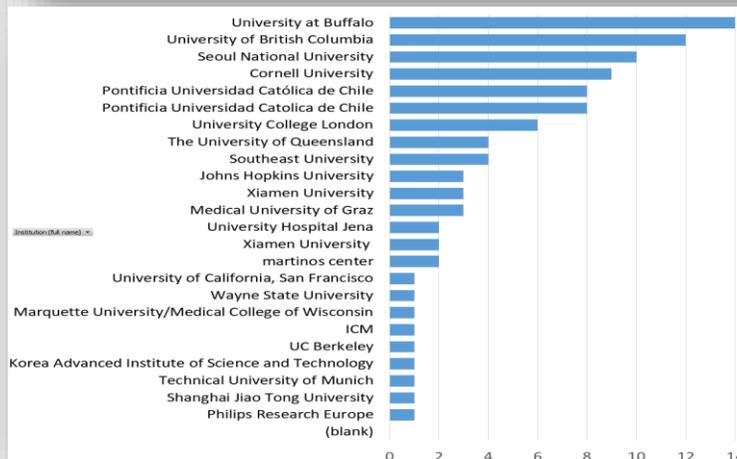
⁹Centre Inria Rennes - Bretagne Atlantique, Rennes, France

¹⁰Spinoza Center for Neuroimaging, Amsterdam, the Netherlands

¹¹Department of Neurology, Medical University of Graz, Graz, Austria

¹²Buffalo Neuroimaging Analysis Center, Department of Neurology, Jacobs School of Medicine and Biomedical Sciences, University at Buffalo, The State University of New York, Buffalo, New York, USA

¹³Center for Biomedical Imaging, Clinical and Translational Science Institute, University at Buffalo, The State University of New York, Buffalo, New York, USA



Make your code and data available...



Data Sharing Collection @ Donders Repository

Quantitative Susceptibility Mapping (QSM) Challenge 2.0

[di.dccn.DSC_3015069.02_542](https://doi.org/10.1155/2021/3015069)

Here we present the creation of a modular and realistic digital brain phantom to serve as a ground-truth to assess the quality of different reconstruction algorithms for Quantitative Susceptibility Mapping (QSM). The phantom is derived from high-resolution, quantitative MRI data of a healthy volunteer, features a realistic morphology including a non piece-wise constant susceptibility distribution.

Files Metadata Manifest History

The files in this collection can be downloaded from https://webdav.data.donders.ru.nl/dccn/DSC_3015069.02_542_v1. To download several files or the entire collection at once, you can use a [WebDAV client](#).

dccn / [DSC_3015069.02_542_v1](#)

Name	Size	Modified
ManuscriptFigures		19 January 2021 10:58:01
Simdata		19 January 2021 10:59:26
data		19 January 2021 10:56:32
func		19 January 2021 10:57:36
DirectoryTree.docx	19.5 KiB	19 January 2021 11:01:17
LICENSE.txt	2.4 KiB	19 January 2021 09:36:11
MANIFEST.txt	27.7 KiB	19 January 2021 11:01:18
MacroAddingMicrostructure.m	3.2 KiB	19 January 2021 11:01:17
MacroCreateQSMpipelineAndCompareHighResLowRes.m	22.2 KiB	19 January 2021 11:01:17
MacroCreateSimulationData.m	5.9 KiB	19 January 2021 11:01:18
MacroCreateSusceptibilityPhantom.m	2.6 KiB	19 January 2021 11:01:18
MacroLoopReconstructionsOfPhantoms.m	8.1 KiB	19 January 2021 11:01:18
MacroProcessInvivoData.m	2.4 KiB	19 January 2021 11:01:18
README.txt	2.2 KiB	19 January 2021 09:36:10

Showing 1 to 14 of 14 entries

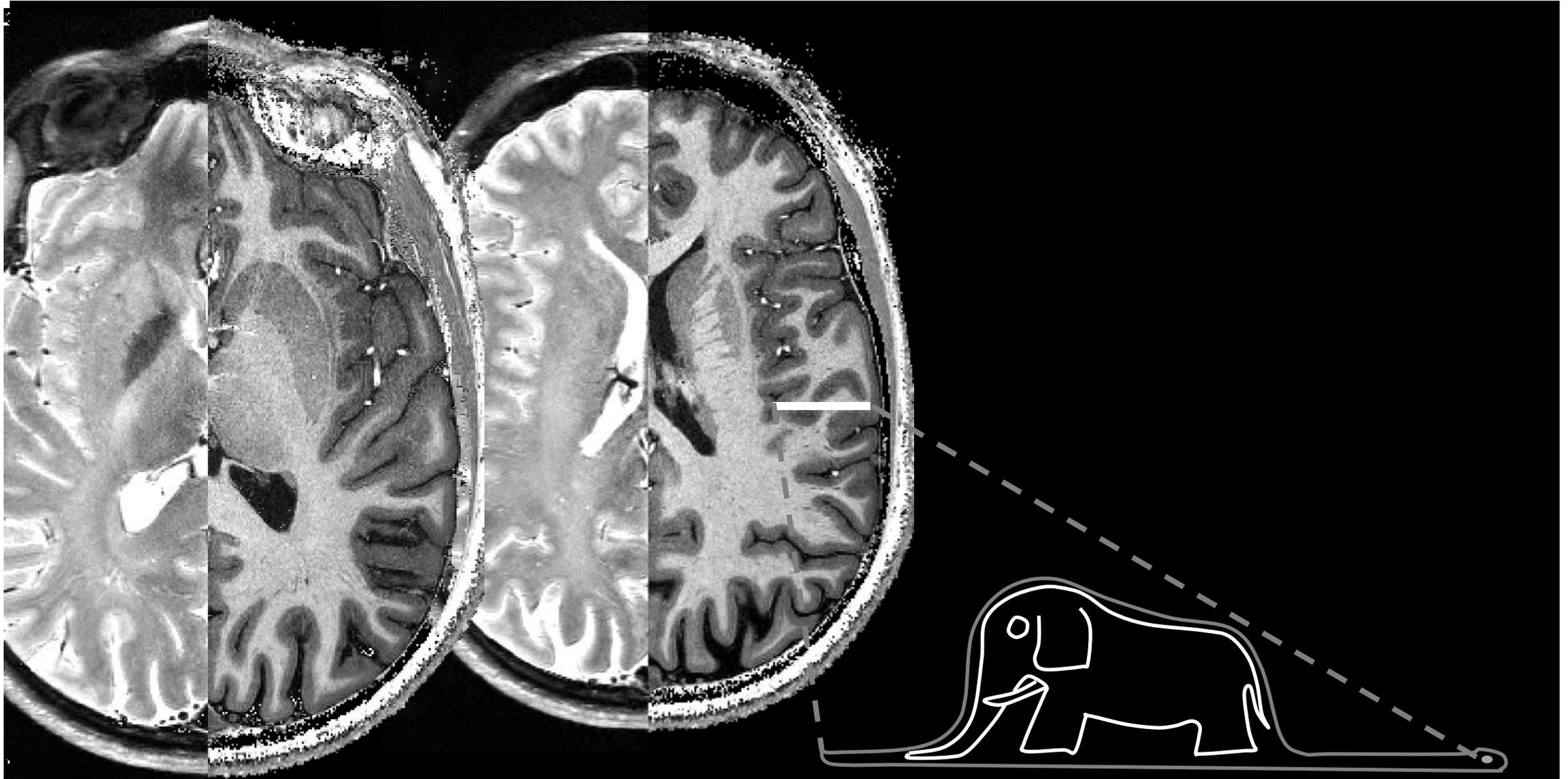
Previous 1 Next

Overview of dataset structure

Collection contains potentially Recognizable Human Data

Scripts used to generate susceptibility phantom (allowing you to modify it)
Scripts to reproduce the paper

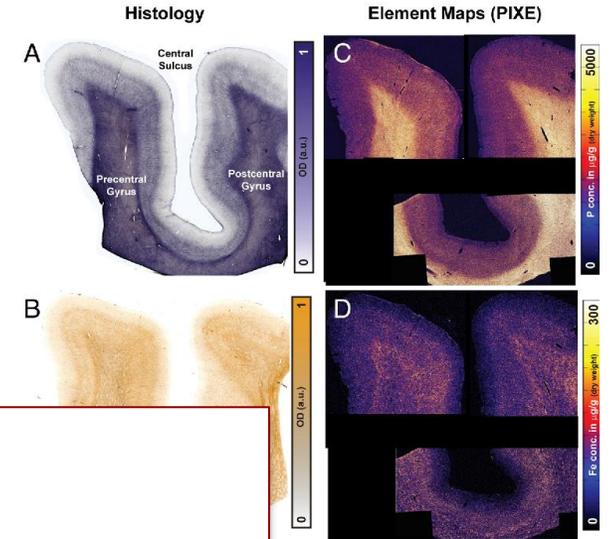
unveiling what is beneath?



Are relaxation rates / times a specific measure of myelin?



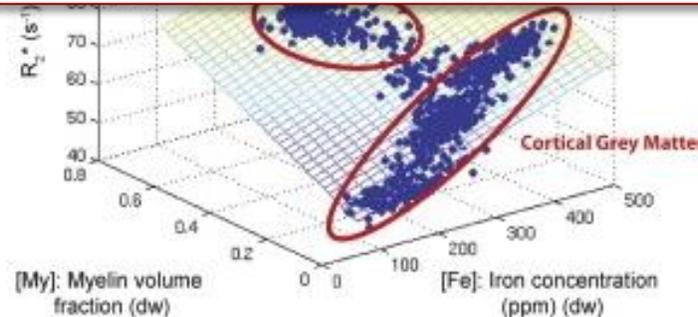
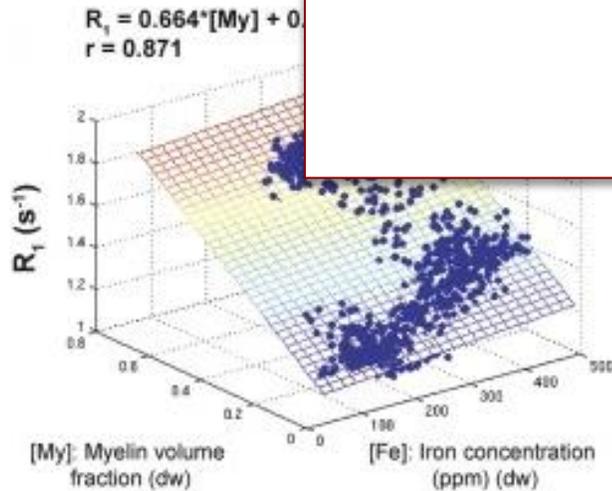
- Myelin affects all relaxation parameters...
but other "stuff" also does



R_1

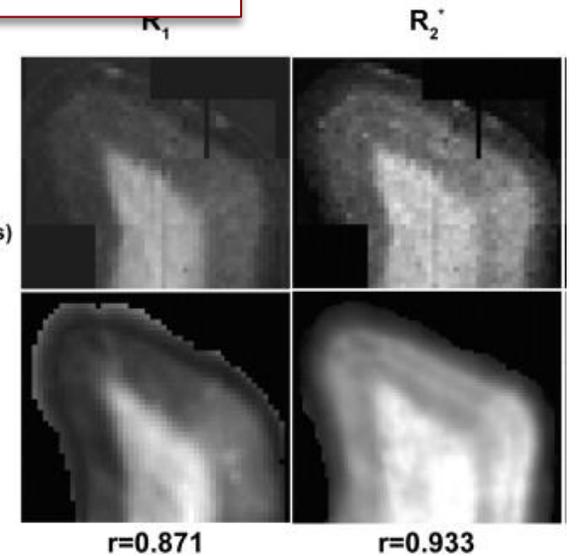
R_2^*

Single compartment models are just too simple...



Simulated MR maps
(Combination of myelin and iron maps)

Measured MR maps





if we want to be more specific
we need to get a better understanding of
how myelin affects the MR signal!

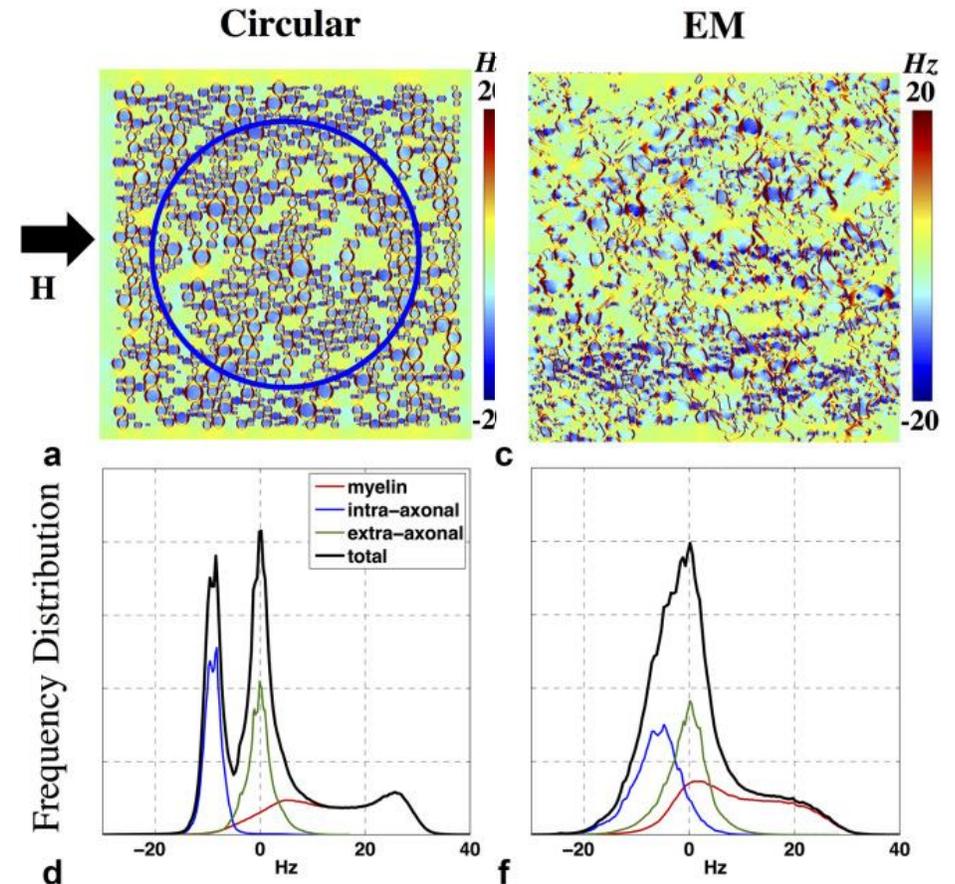
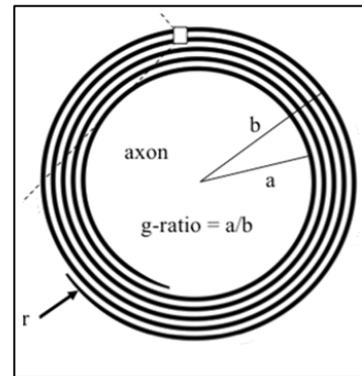
White matter microstructure



Relaxation properties are a too indirect measure of WM microstructure...

What we really want to measure is:

- ❑ Fiber volume fraction
- ❑ g-ratio – conductivity of WM
- ❑ How much myelin there is



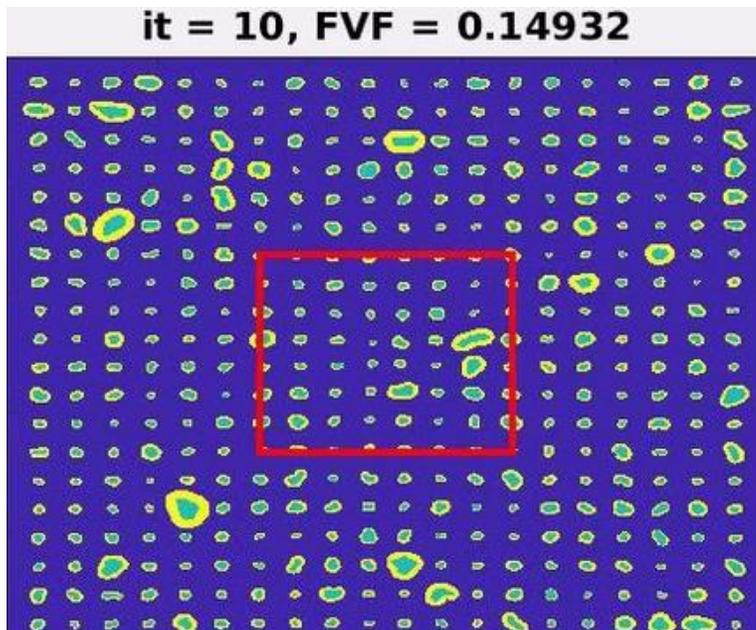
These metrics have an impact in the GRE signal,
And cylinders are not sufficient to describe it..

Creating realistic White Matter models



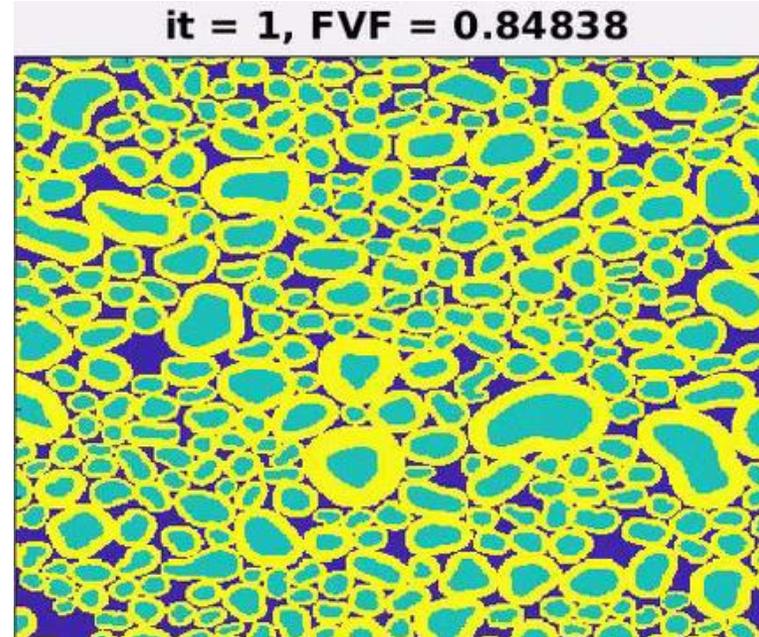
Axon packing

To create realistic WM models

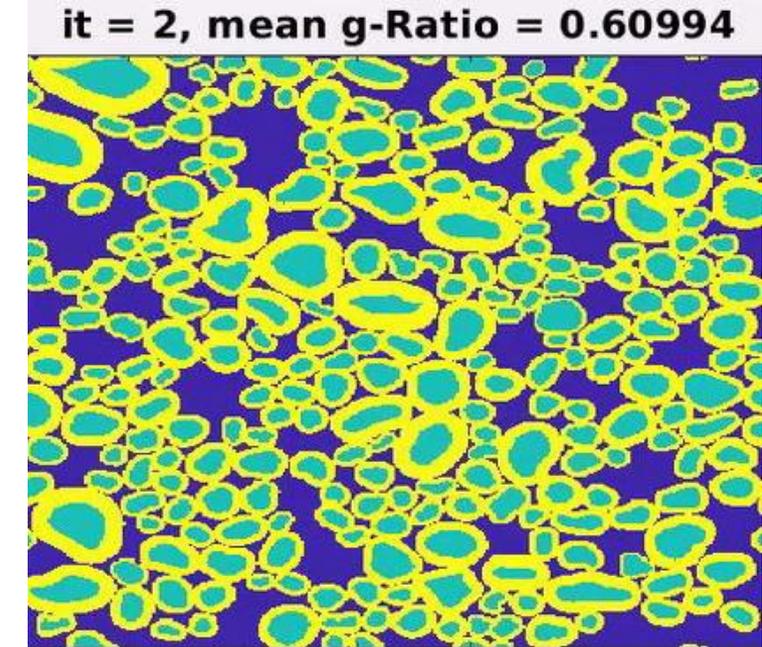


Axon removal

To be able to realistically modulate the FVF



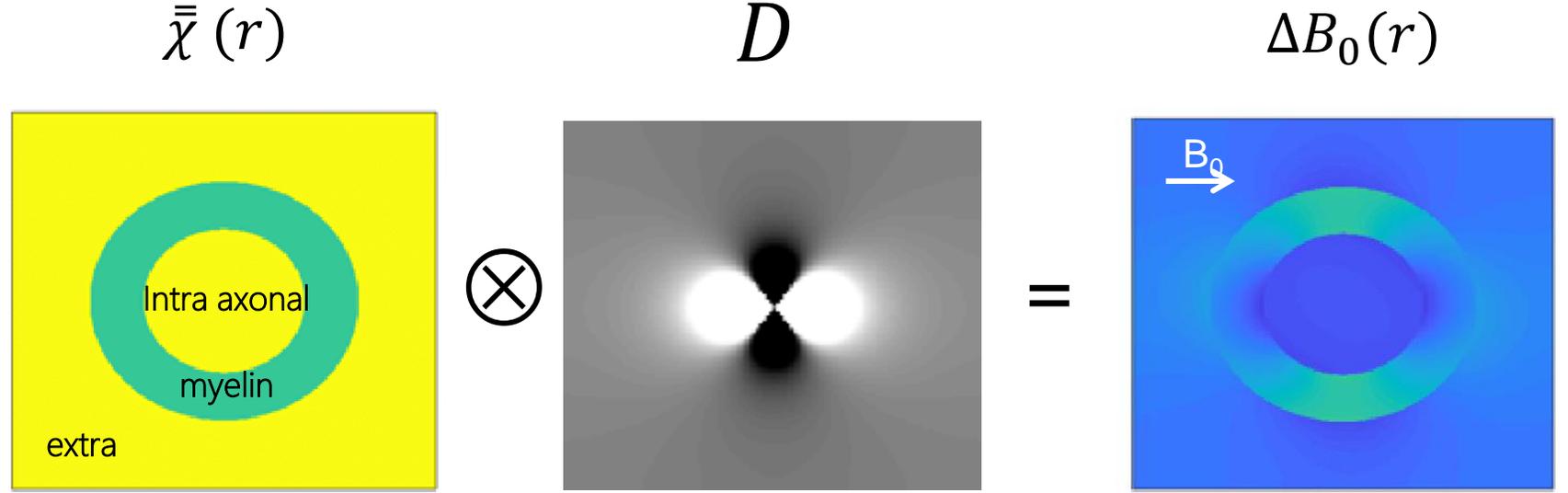
g-factor modulation



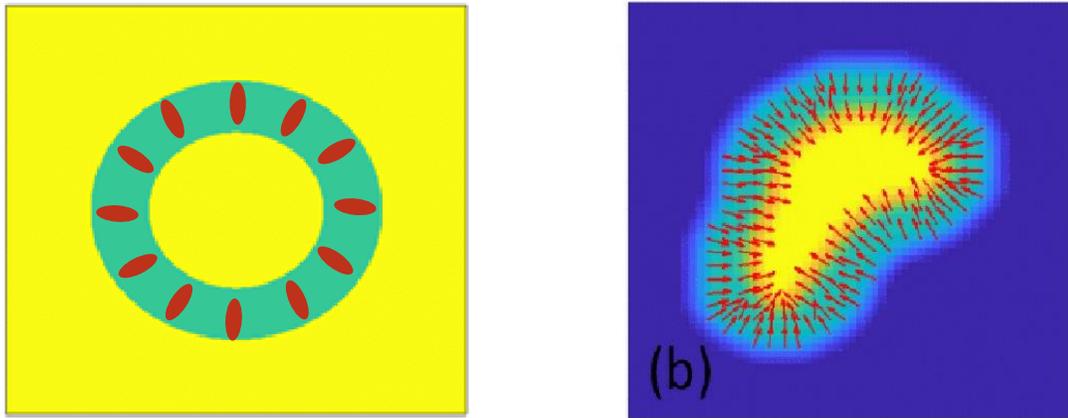
Getting the model right... (enough)



The Hollow cylinder model
Is "very" easy to compute



Yet water is not everywhere, not in the regions of susceptibility



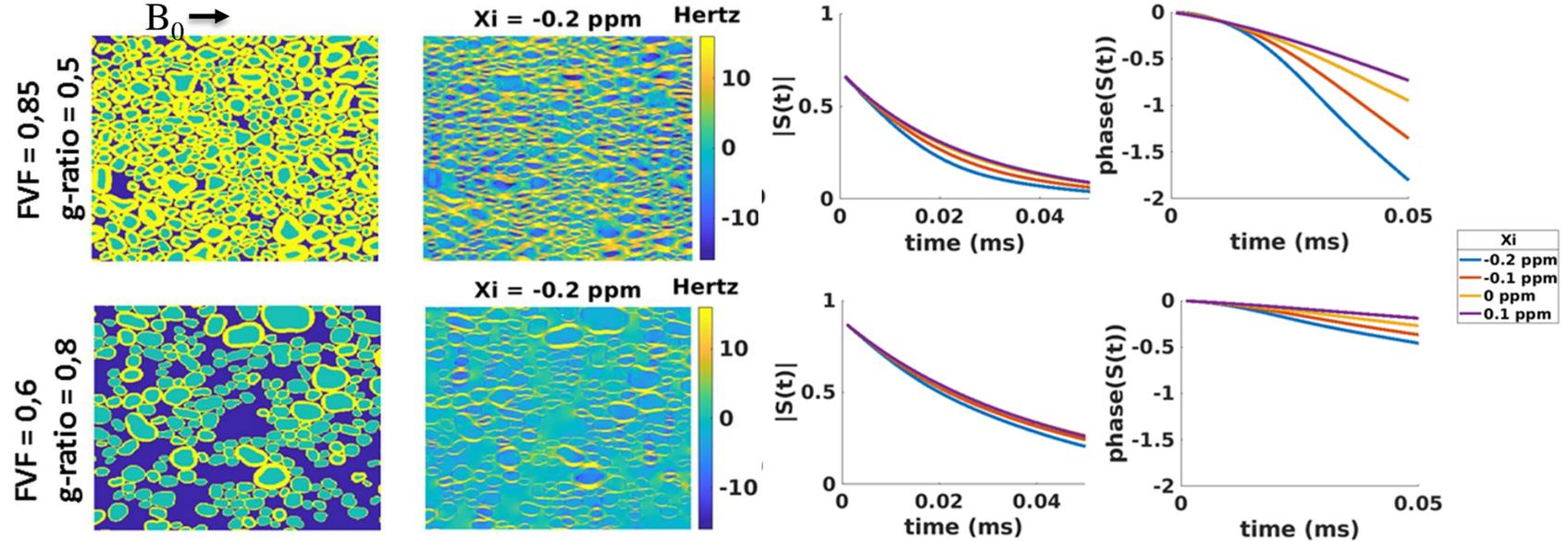
Analytical Lorentzian correction

Axons are not cylinders...

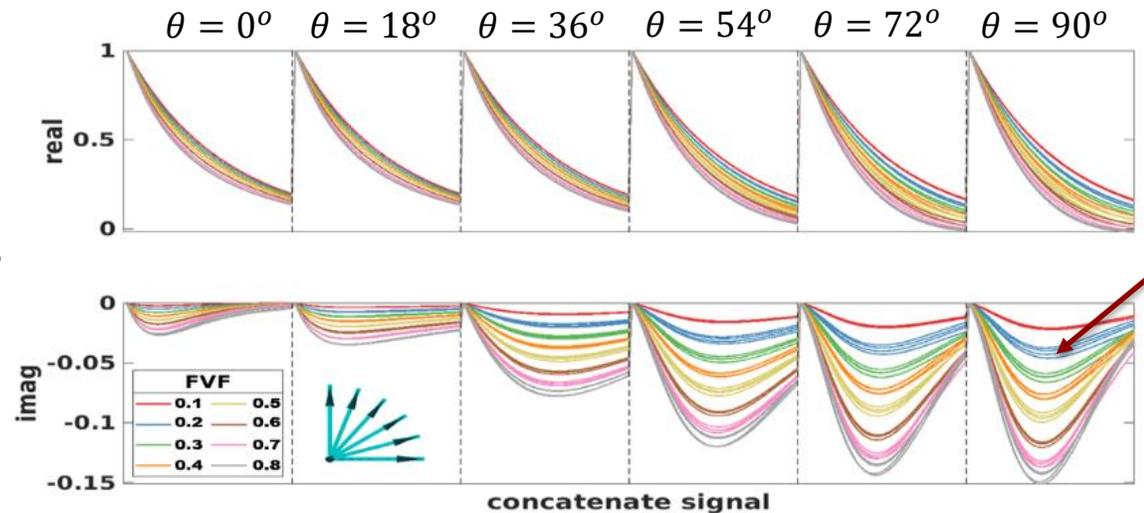
Signal Simulation & Dictionary creation



Different
Microstructure
Parameters
different
Field perturbation
& GRE signal

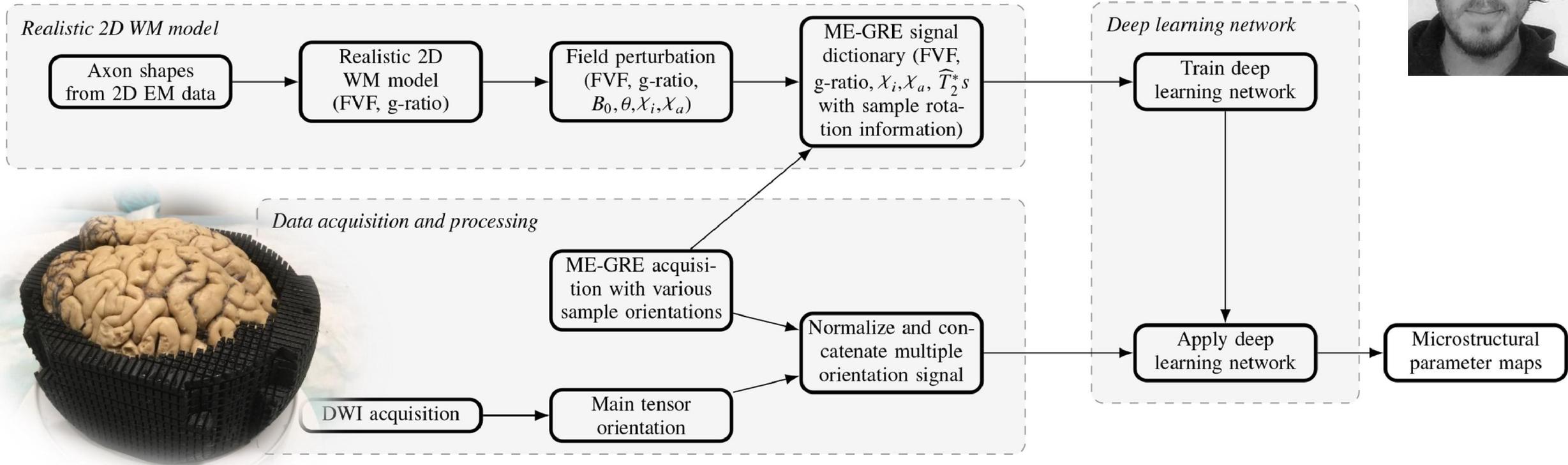


Different white matter models
with same microstructural parameters
Result in similar signals



Different
Realistic
WM models

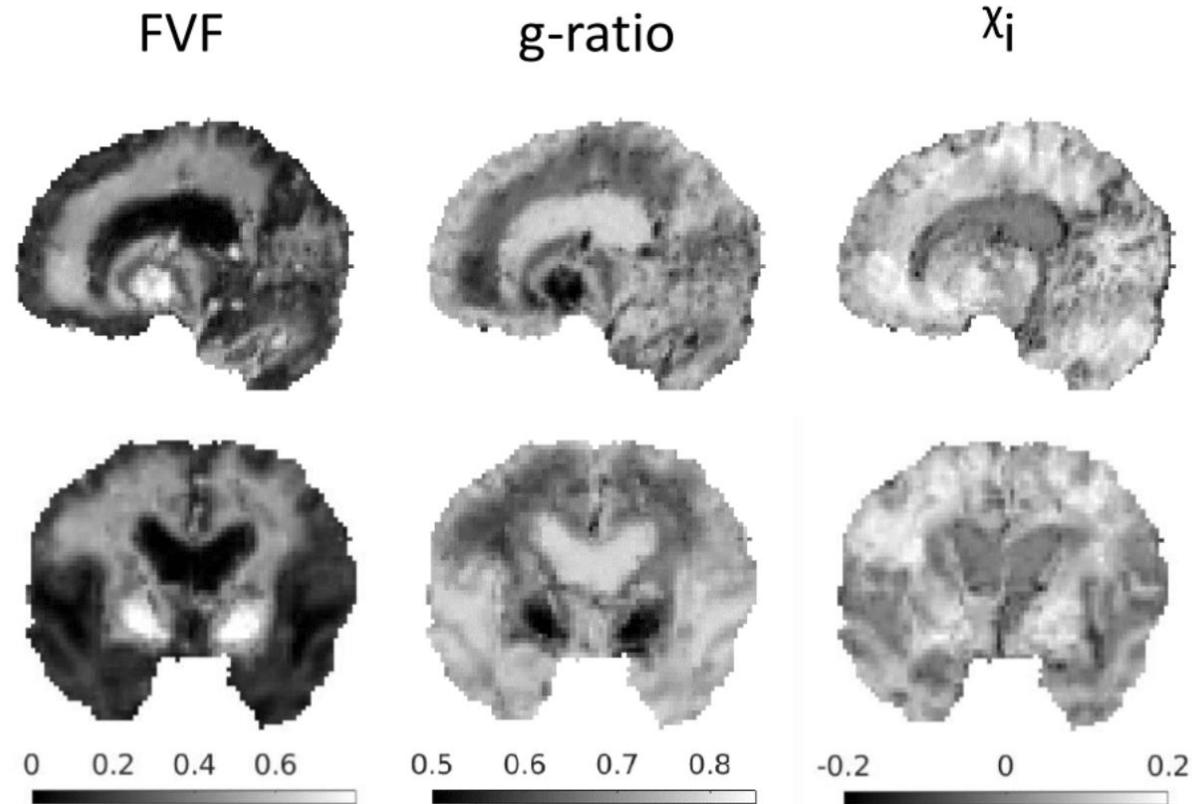
Using Realistic White matter models for decoding microstructure



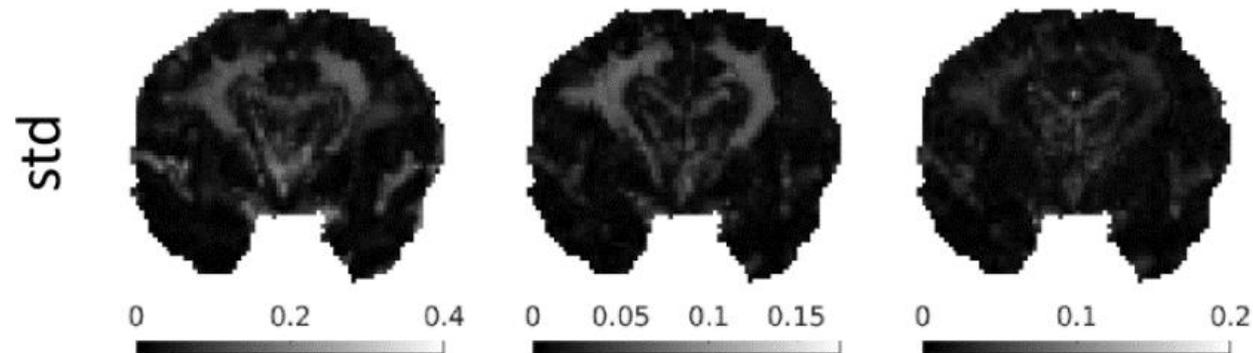
Microstructure property mapping



Whole brain maps
decoded from 9
head positions



Whole brain maps
decoded from 9
head positions
With different T1w



What can an MR Physicist do?



- Understanding how MRI works and the physical interactions in place can take you a long way
- Image reconstruction, motion correction, segmentation and quantitative imaging are being taken over by AI... But AI is better when it knows the right physics!
- Quantitative imaging and biophysical modelling – finding the right complexity balance:
- Share your code, it could help someone else!

Acknowledgements



Co-workers

Kwok-Shing Chan
Renaud Hedouin
David Norris
Christian Licht
Riccardo Mettere
Jeroen Mollink
Rita Gil
Jeni Schultz
... and many more

Collaborators

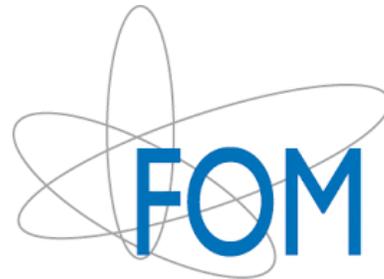
Berkin Bilgic
Christian Langkammer
Richard Bowtell
Ferdinand Schweizer
...

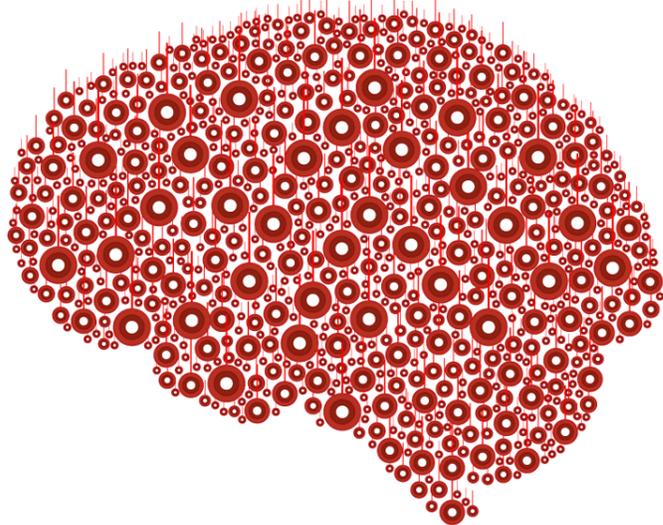
Collaborators in Industry

Tobias Kober
Tom Hilbert

Funding:

" Thinking Inside the Voxel"





Thank you ☺

